Technical Report Documentation Page

1. Report No.	2. Government Acces	ion No. I 3	Recipient's Catalog N	la			
	a. Obvernment Acces	3.	Notified a control of	••			
4. Title and Subtitle		í	Report Dote December 198				
ANTHROPOMETRIC SPECIFI	CATIONS FOR		Performing Organizati				
MID-SIZED MALE DUMMY,							
7 Ad. (3)		8.	Performing Organizati	on Report No.			
7. Author's) D.H. Robbins	•		JMTR1-83-53-	·2			
 Performing Organization Name and Address The University of Mich 	igan	10.	Work Unit No. (TRAI	S)			
Transportation Researc	h Institute	11.	Contract or Grant Na).			
2901 Baxter Road			DTNH22-80-C-	·07502			
Ann Arbor, Michigan 48	109	13.	Type of Report and F	eriod Covered			
12. Sponsoring Agency Name and Address			FINAL REPORT	-			
U.S. Department of Tra		i .	Oct 1980 - Dec 1983				
National Highway Traff	•	ministrationi	14. Sponsoring Agency Code				
Washington, D.C. 20590			sponsoring righting c				
15. Supplementary Notes							
Vol. 1: Development of An an Advanced Adult	thropometric	ally Based Desi	gn Specifica	ations for			
1		· · · · · · · · · · · · · · · · · · ·	·				
Vol. 3: Anthropometric Sp	<u>ecifications</u>	for Small Fema	le & Large M	<u>lale Dummies</u>			
ID. Abstract							
The purpose of th	is report is	to present the	anthropomet	ric			
specifications for a mid-sized male dummy. Data gathered during							
the project as well as							
in formulating these specifications. The analytical techniques							
and procedures used in combining the various data resources are							
described.	•						
This report is pa	rt of a pack	age which also	includes sch	nematic			
drawings and a referen	ce standard	surface form.	The schemati	C			
drawings show front, s	ide, and top	views of the d	ummy form wi	th key			
landmarks and segmenta	oned with respe	ct to the st	andard				
seat coordinate system	seat coordinate system. These three drawing						
front and side full-si	ze drawings	with a superimp	osed skeleta	a l			
i -	ize seated s	urface form is	based on a c	lay			
model.							
	:						
17. Key Words		18. Distribution Statement					
,							
Anthropometry		Unlim	ited				
Crash Test Dummy							
				•			
19. Security Classif. (of this report)	20. Security Clas	if. (of this page)	21- No. of Pages	22. Price			
None	No		134				
			', '				

This document is disseminated under the sponsorship of the Department of Transportation in the interest of information exchange. The United States Government assumes no liability for the contents or the use thereof.

NOTICE

The rights, welfare, and informed consent of the volunteer subjects who participated in this study were observed under guidelines established by the U.S. Department of Health, Education and Welfare Policy (now Health and Human Services) on Protection of Human Subjects and accomplished under medical research design protocol standards approved by the Committee to Review Grants for Clinical Research and Investigation Involving Human Beings, Medical School, The University of Michigan.

VOLUME 2: CONTENTS

LIST	OF TABLES	V
LIST	OF FIGURES	vii
1.0	INTRODUCTION	1
2.0	LANDMARKS USED FOR SUBJECT DEFINITION	_, 5
3.0	DEVELOPMENT OF STANDARD SEAT COORDINATE SYSTEM	11
4.0	SUBJECT DATA TRANSLATED TO STANDARD COORDINATE SYSTEM	15
5.0	SEGMENTATION AND LINKAGE SELECTION	19
6.0	CONSTRUCTION OF SEGMENTATION PLANES	21
	6.1 Head Plane 6.2 Neck Plane 6.3 Thorax Plane 6.4 Abdomen Plane 6.5 Hip Plane: First Attempt 6.6 Hip Plane: Successful Attempt 6.7 Knee Plane 6.8 Ankle Plane 6.9 Shoulder Plane 6.10 Elbow Plane 6.11 Summary	22 22 23 25 27 29 29 29
7.0	DEVELOPMENT OF ANATOMICALLY BASED SEGMENT COORDINATE SYSTEMS	33
	7.1 Head Axis System	39 41 42
8.0	VOLUME, MASS, AND INERTIAL PROPERTIES	51
	8.1 Basic Anthropometric Properties of Each Segment8.2 Volume and Mass Properties8.3 Centers of Gravity in Hip Point and Segment	51 68
	Coordinate Systems	69 72

9.0	A MODEL FOR THE LOCATION OF JOINT CENTERS	87
	9.1 Introduction	87
	9.2 Joint Center Model for the Vertebral Column	91
	9.3 Joint Centers in the Shoulder and Arm	94
	9.4 Joint Centers in Hip, Knee, and Ankle	101
10.0	JOINT PARAMETERS	103
	10.1 Introduction	103
	10.2 Range of Motion at Joint Structures	104
	10.3 Resistance to Motion at Joint Structures	104
11.0	REFERENCES	121

LIST OF TABLES

		Page
1.	List of Surface Landmarks for Segment and Joint Definition (Original Requirements)	8
2.	Landmarks Used in Construction of Segment Anatomical Coordinate Systems	9
3.	Landmarks Used in Constructing Segmentation Planes	10
4.	Skeletal and Surface Landmarks Relative to H-Point	16
5.	Formulation of Segmentation Planes	32
6.	Location of Origins of Segment Anatomical Coordinate Systems	34
7.	Anatomical Axes with Respect to Hip Point Axis System (Cosine Matrix Expressed in Degrees)	35
8.	Anatomical Axes with Respect to Hip Point Axis System (Cosine Matrix)	37
9.	Coordinates of Surface Points on Clay Form	63
10.	Estimated Segment Mass and Volume	69
11.	Location of Estimated Segment Centers of Gravity with Respect to Whole Body Coordinate System	71
12.	Location of Estimated Segment Centers of Gravity with Respect to the Individual Segment Coordinate Systems	71
13.	Anthropometric Variables Used in Principal Moment of Inertia Regression Equations	73
14.	Estimated Segment Principal Moments of Inertia	74
15.	Principal Axes of Inertia with Respect to Anatomical Axes (Cosine Matrix Expressed in Degrees)	78
16.	Principal Axes of Inertia with Respect to Anatomical Axes (Cosine Matrix)	80
17.	Principal Axes of Inertia with Respect to Hip Point Axis System (Cosine Matrix Expressed in Degrees)	82
18.	Principal Axes of Inertia with Respect to Hip Point Axis System (Cosine Matrix)	84

19.	Location of Joint Centers in Whole-Body Coordinates	89
20.	Location of Joint Centers in Segment Coordinates	90
21.	Range-of-Motion Data	107

LIST OF FIGURES

		Page
1.	Schematic of anthropometric specifications for mid-sized male dummy	3
2.	Pelvic coordinate system superimposed on UMTRI lab-based coordinate system	13
3.	Construction of thorax and abdomen segmentation planes .	24
4.	Construction of hip segmentation plane	26
5.	Construction of knee segmentation plane	30
6.	Head anatomical coordinate system	40
7.	Segment axes in thorax for seated posture	54
8.	Side view of clay model with surface profile strips	60
9.	Front view of clay model with surface profile strips	61
10.	Back view of clay model with surface profile strips	62
11.	Construction of C7/T1 joint	93
12.	Construction of thoracic joints	93
13.	Construction of lumbar joints	95
14.	The three joints of the shoulder girdle	97
15.	Range of motion at shoulder joint as a function of degrees of freedom	98
16.	Illustrations of range-of-motion definitions	109
17.	Head resistance to flexion and extension	113
18.	Head resistance to lateral flexion	114
19.	Waist resistance to flexion and extension	115
20.	Shoulder resistance to rotation	116
21.	Elbow resistance to flexion	117
22.	Resistance to hip flexion and extension	118
23.	Resistance to flexion at knees	119

1.0 INTRODUCTION

The purpose of Volume 2 is to present the anthropometric specifications for a mid-sized male dummy. Data gathered during the project as well as data available in the literature were used in formulating these specifications. This volume is organized not only to present the results, but to lead the user through the process of development of a consistent anthropometric description of a seated human.

The first sections concentrate on subject geometric definition based on measured surface landmarks and the construction of a standard seat coordinate system in which all data can be specified. In the next sections, the emphasis shifts to division of the body into discrete segments. This implies at least partial acceptance of the assumption that the human body can be represented as a chain of rigid bodies in dynamic applications. (In the static sense, when the body is not moving, this assumption is valid.) Individual coordinate systems are defined for each segment. Transformations are developed which relate these segment systems to the standard seat coordinate system.

Mathematical formulations follow for the construction of segmentation planes between the various parts of the body. The static anthropometric description is completed by estimation of joint center locations for the seated subject in both standard seat and segment coordinate systems.

A step toward dynamic anthropometric specifications is made in the concluding sections of the report. The limited consistent information available for description of mobility between the various segments of the body is reviewed. The results are assembled into a qualified specification on range of motion to complete the report.

This report is supplemented by full-size blueprints (Nos. MM-101, MM-102, MM-103, MM-104, MM-105) showing side, front, and top views of the following:

- Surface landmarks
- Joints centers
- Segment centers of gravity

- Origins of segment coordinate systemsSurface profile of actual surface form
- Information on anatomical and principal axes
- Information on segmentation planes
- A superimposed skeletal rendering

Figure 1 in this report is a schematic showing a subset of this information.

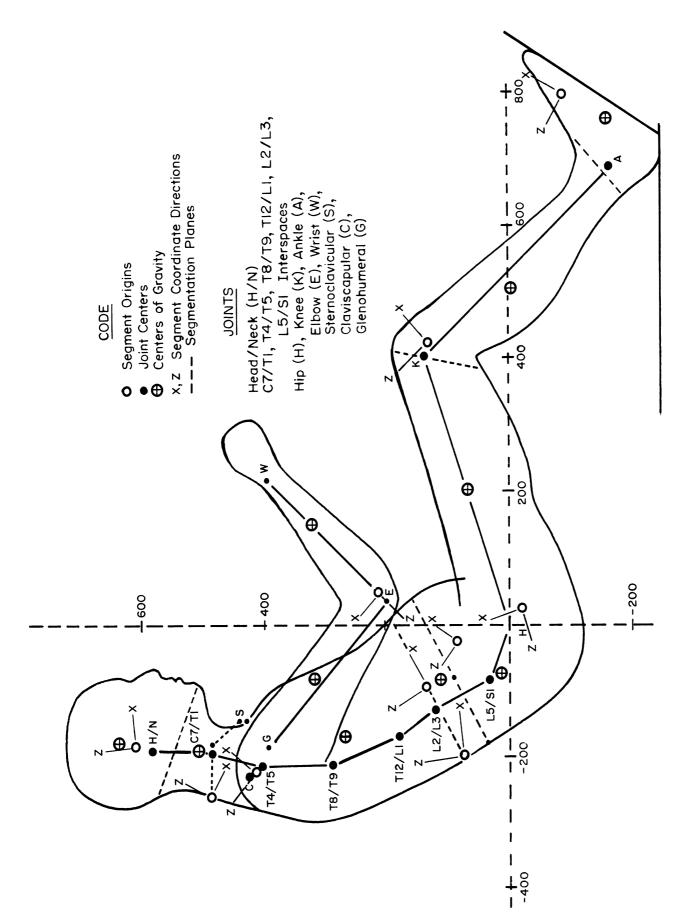


FIGURE 1. Anthropometric specifications for mid-sized male dummy.



2.0 LANDMARKS USED FOR SUBJECT DEFINITION

In order to develop a geometric and mass definition of a person seated in an automobile it is necessary to take into account a variety of issues including:

- Body segmentation scheme
- Sizing of components
- Segment masses
- Segment centers of gravity
- Segment moments of inertia
- Joint locations
- Joint ranges of motion
- Surface geometry
- Orientation of pelvis, vertebral column, skull, and lower extremities in the seated position
- Relation of coordinate systems in anatomical segments to the standard seat coordinate system

Table 1 is the original minimum collection of geometric points estimated to be required. The first thirty-one are minimum requirements for body segmentation, mass property definition, and segment coordinate system construction using the formulae and techniques of McConville et al. (1980). Tables 2 and 3 associate particular skeletal landmarks used in the present analysis with coordinate systems and segmentation planes. The large majority of these agree with the first thirty-one of Table 1. However, a few new points can be identified which are required for the study of seated posture. These include points to define the:

- Thorax and abdomen coordinate system and the thorax segmentation plane: "Intersection point on the back of the surface form of a perpendicular from the center of a line connecting the 10th rib targets to a line connecting the T12 and L5 surface targets."
- Foot coordinate system: "Heel point" (taken directly from the seating buck).
- Abdomen segmentation plane: "Intersection point on the back of the surface form of a perpendicular from the center of a line connecting the iliocristale targets to a line connecting the L2 and L5 surface targets."
- Hip segmentation plane: "Pubotuberosity" and "lateral tuberosity point."

Beyond the first thirty-one, the next three landmarks locate the position of the scapula within the space defined by a shoulder girdle mass, which is separate from the thorax or chest mass defined by McConville et al. Although it has not been possible within the current activity, it is recommended that in future work the cadaver shoulder girdle segmentation scheme and mass data of Dempster (1965) be used to decompose the thorax definition of McConville into rib cage and shoulder girdle segments. The recognition of the separation of rib cage from shoulder girdle will lay the basis for design of more realistic interactions between members of the new dummy family and side door structures as well as frontal restraint devices. A further purpose is to more clearly define the location of the acromio-clavicular and glenohumeral joints so that the best possible estimates of shoulder girdle centers of rotation can be made.

The final five surface landmarks relate to the spinal column. These data are being used as input for procedures reported by Snyder et al. (1972) to define the location of several spinal interface centers with respect to the surface data. These landmarks are important for placing the vertebral column in a correct relationship to the exterior of the surface form.

Four of the surface landmarks in Table 1 require special comment. These are marked by asterisks. The symphysion was replaced in the final list of subject targets by pelvic crest due to the difficulty of target location for photographic data acquisition. In order to compensate, a correction factor was developed to translate pelvic crest landmark to symphysion based on pelvic geometry data of Reynolds et al. (1981). Posterior calcaneus is hidden from view in that the heel is in the driving position in the standard seat buck. However, a close approximation of this point is the heel point reference which is measured directly on the buck.

It was not possible to obtain two points directly. These are nuchale and gluteal furrow. However, nuchale position can be inferred from the surface form and by the fact that its location is given in anatomical coordinates by McConville et al. (1980). Gluteal furrow point is in contact with the seat and hence is invisible. No attempt to

develop this point was made because of tissue shifts between standing seated posture. The subject is discussed further in Sections 5 and 6.

TABLE 1

LIST OF SURFACE LANDMARKS FOR SEGMENT AND JOINT DEFINITION (Original Requirements)

- 1. Cervicale*
- 2. Acromion
- 3. Trochanterion (skeletal reconstruction)
- 4. Infraorbitale
- 5. Tragion
- 6. Suprasternale
- 7. Lateral Humeral Epicondyle
- 8. Ulnar Styloid
- 9. Anterior-Superior Iliac Spine
- 10. Symphysion**
- 11. Lateral Femoral Epicondyle
- 12. Lateral Malleolus
- 13. Clavicale
- 14. Mid-Spine, 10th Rib Level
- 15. Lateral 10th Rib
- 16. Medial Humeral Epicondyle
- 17. Radiale
- 18. Stylion
- 19. Medial Femoral Epicondyle
- 20. Tibiale
- 21. Sphyrion
- 22. Metatarsal/Phalangeal |
- 23. Metatarsal/Phalangeal V
- 24. Posterior Calcaneus**
- 25. Tip of Digit II (Toe)
- 26. Gonion
- 27. Iliocristale
- 28. Anterior Scye
- 29. Olecranon
- 30. Nuchale**
- 31. Gluteal Furrow (most inferior point) **
- 32. Superior Margin Scapula
- 33. Inferior Margin Scapula
- 34. Acromio-Clavicular Articulation
- 35. T4 Surface
- 36. T8 Surface
- 37. Tl2 Surface
- 38. L2 Surface
- 39. L5 Surface

^{*}See Section 3.0 in Volume 1 for definitions.

^{**}Landmarks modified or deleted from final list.

TABLE 2

LANDMARKS USED IN CONSTRUCTION OF SEGMENT ANATOMICAL COORDINATE SYSTEMS

Segment	Landmarks
Head	Tragion (L and R) Infraorbitale (L)
Neck	Clavicale (L and R) Cervicale
Thorax	Cervicale 10th rib (L and R) Intersection point on back of surface form of a perpendicular from the center of a line connecting the 10th rib targets to a line connecting the T12 and L5 surface targets T12 L5
Abdomen	10th rib (L and R) Intersection point on back of surface form of a perpendicular from the center of a line connecting the 10th rib targets to a line connecting the T12 and L5 surface targets T12 L5
Pelvis	Anterior-Superior Iliac Spines (L and R) Symphysion
Upper Arms	Acromion (L and R) Medial Humeral Epicondyle (L and R) Lateral Humeral Epicondyle (L and R)
Lower Arms and Hands	Radiale (L and R) Ulnar Styloid Process, Distal End (L and R) Radial Styloid Process, Distal End (L and R)
Upper Legs	Trochanterion, reconstructed (L and R) Lateral Femoral Epicondyle (L and R) Medial Femoral Epicondyle (L and R)
Lower Legs	Tibiale (L and R) Sphyrion (L and R) Lateral Malleolus (L and R)
Feet	Metatarsal/Phalangeal I (L and R) Metatarsal/Phalangeal V (L and R) Heel Point (L and R)

TABLE 3

LANDMARKS USED IN CONSTRUCTING SEGMENTATION PLANES

Segmentation Plane	Landmarks
Head	Gonion (L and R) Nuchale
Neck	Clavicale Cervicale
Thorax	10th Rib (L and R) Intersection point on back of surface form of a perpendicular from the center of a line connecting the 10th rib targets to a line connecting the T12 and L5 surface targets
Abdomen	Iliocristale (L and R) Intersection point on back of surface form of a perpendicular from the center of a line connecting the iliocristale targets to a line connecting the T12 and L5 surface targets
Нір	Anterior-Superior Iliac Spine (L and R)* Pubotuberosity (L and R)* Lateral Tuberosity Point (L and R)*
Knee	Lateral Femoral Epicondyle (L and R)
Ankle	Sphyrion (L and R)
Shoulder	Acromion (L and R) Anterior Scye (L and R) Posterior Scye (L and R)
Elbow	Olecranon Medial Humeral Epicondyle Lateral Humeral Epicondyle

^{*}These skeletal landmarks are derived from the position in space of the average pelvis (Reynolds et al. 1981).

3.0 DEVELOPMENT OF STANDARD SEAT COORDINATE SYSTEM

The selection of a standard seat coordinate system was made between two candidates: (1) traditional H-point, and (2) seat-based coordinate system. The traditional H-point represents a point on the H-point machine associated with the human hip joint. Seat-based coordinate systems often reflect the intersection point between seat back and seat cushion lines. The continuous curvature of the seat back and cushion of the average standard seat developed on this project prevented development of any clear definition of seat back and seat cushion lines. Hence, it was decided that the traditional H-point concept offered the better alternative.

The surface landmarks for right and left anterior-superior iliac spines as well as pelvic crest were obtained in this study (see Volume 1, Section 3.8). These were used to determine the orientation of the pelvis in three-dimensional coordinates. In order to define the H-point it was necessary to estimate tissue thicknesses of the surface landmarks over the skeletal landmarks. These data also being available, it was then possible to orient the pelvis if an appropriate average structure could be found.

The pelvic data of Reynolds et al. (1981) are based on a subject group similar in average stature and weight to those measured during the current UMTRI study as shown below.

Body Measurement	UMTR! 1983	Reynolds et al. 1981
Weight (1b)	168.8	165.7
Stature (cm)	175.1	173.6

These data were accepted for the pelvic reconstruction, location of the standard seat coordinate system at the center of a line connecting the H-points, location of the center of rotation of the two hip joints, and location of the lumbar-sacral (L5/S1) joint center.

The direction of Reynolds' coordinate system was superimposed upon the UMTRI data for anterior-superior iliac spine (ilio-spinale summum) and pubic symphysis (Figure 2). The direction of 54.07 degrees between the two allowed conversion of any of the Reynolds et al. data points into a system parallel to the UMTRI lab system with an origin at the center point of the anterior-superior iliac spines using the simple transformation:

$$X_L = X_R \cos \theta - Z_R \sin \theta$$

 $Z_L = X_R \sin \theta + Z_R \cos \theta$

where the subscript R identifies the Reynolds et al. coordinate values and L refers to the lab system. The following points were transformed as needed for use in construction of joint centers, segmentation planes, anatomical segment axis construction, estimation of tissue depths, etc.:

- H-points
- Pubic symphysis
- Inferior symphyseal pole
- Superior pole, pubic symphysis
- Ilio-spinale summum
- Ilio-cristale summum
- Inferior tuberosity point
- Posterior point on 1st sacral vertebral body
- Promontorion
- Lateral point on 1st sacral vertebral body
- Pubotuberosity
- Lateral tuberosity point

The key points for development of a standard seat coordinate system were the H-points which have the following coordinates in the UMTRI laboratory reference system (defined by the subscript L):

H-Point	X _L (mm)	Y _L (mm)	Z _L (mm)
Left	657	701	422
Right	657 657	537	422

The Y-shift from the body centerline was ± 82 mm as reported by Reynolds et al. The center of the line connecting these two points is located at: $X_L=657$, $Y_L=619$, $Z_L=422$. This point is selected as the origin of the standard seat coordinate system. All further data in this report are

related to this point on the body centerline. The subscript for all data quantities referred to in this new coordinate system based on the H-point will have the subscript H.

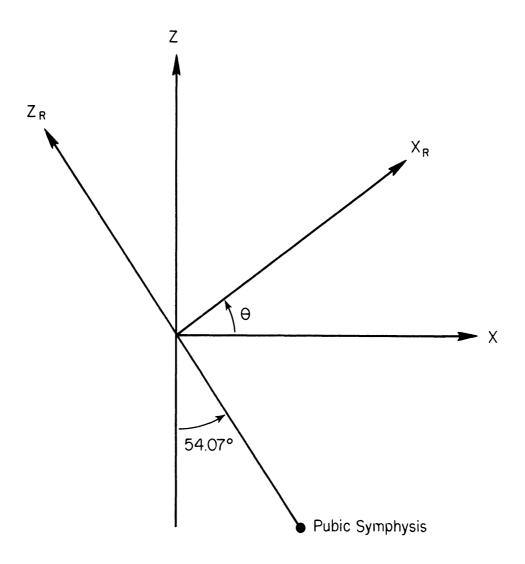


FIGURE 2. Pelvic coordinate system superimposed on UMTRI lab-based coordinate system.



4.0 SUBJECT DATA TRANSLATED TO STANDARD COORDINATE SYSTEM

Table 4 presents all skeletal and surface landmarks used in the development of the anthropometric specifications for the mid-sized male dummy and are incorporated in the surface form. The origin of coordinates is the center of a line connecting the H-points. These data are derived from the original data given in Volume 1 of this report. The subscript H is used throughout the report for all quantities given with respect to this origin.

TABLE 4

SKELETAL AND SURFACE LANDMARKS RELATIVE TO H-POINT (mm)

	Surface		Skeletal			
Body Segment and Landmark		YH	z _H	ХН	YH	z _H
HEAD Glabella	- 80	0	651		0	651
Infraorbitale (L) Infraorbitale (R) Tragion (L) Tragion (R) Gonion (L) Gonion (R) Gnathion Nuchale*	- 96 - 96 - 185 - 185 - 173 - 101 - 262	70 - 70	620 614 614 544 511 579	- 99 -185 -185 -173	76 - 76 67	620 614 614 549 549 517
VERTEBRAL COLUMN						
C7 T4 T8 T12 L2 L5 Mid-Spine 10th Rib Superior Margin Scapula (L) Superior Margin Scapula (R) Inferior Margin Scapula (R)	-266 -293 -284 -246 -217 -174 -242 -296 -296 -276	0 0 0 0 0 0 79 - 79 126 -126	380 253 146 87 13	-240 -212 -169 -242 -285 -285 -269	0 0 0 0 0 79 - 79 126 -126	489 380 253 146 87 13 138 392 274 274
Intersection point on back of surface form of a perpendicular from center of line connecting 10th rib targets to line connecting T12 and L5 surface targets*	-209	0	71			
Intersection point on back of surface form of a perpendicular from center of line connecting iliocristale targets to line connecting T12 and L5 surface targets*	-188	0	35			
TORSO						
Suprasternale Mesosternale Substernale Bimammary, midline Nipple (L) Nipple (R) 10th Rib, Anterior, Midline Umbilicus	-139 - 98 - 72 - 52 - 52 - 52 - 53 35	0 0 0 0 113 -113 0	385 336 281 290	-140 -101 - 75	0 0 0	431 385 336

TABLE 4
SKELETAL AND SURFACE LANDMARKS RELATIVE TO H-POINT (Continued)

Body Segment and Landmark		Surface			Skeletal		
body Segment and Landmark	ХН	YH	z _H	Х _Н	Y _H	z _H	
TORSO (Contd.) Maximum Abdominal Protrusion 10th Rib (L) 10th Rib (R)	56 - 93 - 93			- 93 - 93		133	
Trochanterion (L) (UMTRI photo) Trochanterion (R) (UMTRI photo) Iliocristale (L) Iliocristale (R) Anterior-Superior Iliac Spine (L) Anterior-Superior Iliac Spine (R) Pubic Symphysis Thigh/Abdominal Junction (L) Thigh/Abdominal Junction (R) Trochanterion (skeletal reconstruction)* H-Point Pubic Symphysis Inferior Symphyseal Pole Left Superior Pole, Pubic Symphysis Ilio-Spinale Summum Iliocristale Summum Inferior Tuberosity Point Posterior Point 1st Sacral Vertical Body Promontorion Lateral Point 1st Sacral Vertical Body Pubotuberosity Lateral Tuberosity	- 33 - 33 - 80 - 80 - 25 - 25 51 21 20	161 -161 116 -116 0 122 -122	28 28 93 83 83 81 81 - 20	- 33 - 80 - 80 - 25 - 25 - 44 0 38 42 33 - 25 - 102 37 - 98 - 89 - 89 34	-148 131 -131 116 -116 0 ± 82 0 ± 5 ±119 ± 39 0	28 93 78 78 28 0 32 - 7 25 78 74 - 61 33 37	
SHOULDER Clavicale (L) Clavicale (R) Acromio-Clavicular Articulation (L) Acromio-Clavicular Articulation (R) Greater Tubercle Humerus (L) Greater Tubercle Humerus (R) Acromion (L) Acromion (R) Anterior Scye (L) Anterior Scye (R) Posterior Scye (R)	-145 -145 -215 -215 -173 -173 -224 -224 -97 -97 -214	- 23 182 -182 218 -218 203 -203 154 -154 197	443 443 443 421 421 419	-147 -147 -215 -215 -183 -183 -224	- 23 182 -182 197 -197 199	439 437 437 400 400 417	

TABLE 4
SKELETAL AND SURFACE LANDMARKS RELATIVE TO H-POINT (Continued)

Body Segment and Landmark	Surface			Skeletal		
Body Segment and Landmark	Х _Н	YH	z _H	ХН	YH	z _H
ARM						
Lateral Humeral Epicondyle (L) Lateral Humeral Epicondyle (R) Radiale (L) Radiale (R) Medial Humeral Epicondyle (L) Medial Humeral Epicondyle (R) Olecranon (L) Olecranon (R) Ulnar Styloid (L) Ulnar Styloid (R) Stylion (L) Stylion (R)	32 46 46 32 32 53 226 226 211 211	242 -242 243 -243 -173 -173 210 -210 -191 -191 135 -135	224 224 209 209 199 186 186 387 387 399 399	32 46 46 32 53 53 226 226 209	240 -240 176 -176 210	221 221 205 205 202 202 189 189 388 388 397
LEG AND FOOT						
Lateral Femoral Epicondyle (L) Lateral Femoral Epicondyle (R) Medial Femoral Epicondyle (L) Medial Femoral Epicondyle (R) Tibiale (L) Tibiale (R) Patella (L) Patella (R) Sphyrion (L) Sphyrion (R) Metatarsal/Phalangeal I (L) Metatarsal/Phalangeal I (R) Digit II (L) Digit II (R) Metatarsal/Phalangeal V (L) Metatarsal/Phalangeal V (R) Lateral Malleolus (R)	404 407 407 424 449 484 484 684 796 839 7850 680	88 - 88 - 150 - 150 - 61 - 61 - 84 - 84 - 147 - 147 - 174 - 174	- 37 - 37 -124	404 407 407 424 424 684 796 839 785 786 680	63 - 63 86 - 86 147 -147 173 -173	129 142 142 128 128 128 -149 - 86 - 43 - 124 - 124 - 181 - 181

 $[\]star$ Landmark location determined by construction.

5.0 SEGMENTATION AND LINKAGE SELECTION

The traditional segmentation of the human body for use in developing crash test device linkages is as follows:

Head Two Lower Legs

Neck Two Feet

Thorax Two Upper Arms
Abdomen Two Lower Arms
Pelvis Two Hands

Two Upper Legs

Although substantial mobility in the shoulder girdle has been known for years (see Dempster 1965, Dempster and Gaughran 1967, and Snyder et al. 1972), only minimal data are available for the description of its mass and inertial properties. Dempster (1965) reports a center of gravity, mass, and inertial properties around the side-to-side axis (Y-axis) for the masses associated with scapula, clavicle, and soft tissues exterior to most of the bony thorax. No shoulder girdle data are given in the more recent work of McConville et al. (1980) and Reynolds et al. (1975). As a result, it was concluded that insufficient consistent data are available from the literature to construct a separate shoulder girdle within the scope of the current activity.

A non-traditional segmentation scheme is recommended for the eventual advanced dummy family that includes a separate, mobile shoulder girdle link and the associated mass. Sufficient surface landmarks are available in the UMTRI data (scapula, clavicale, extent of rib cage) to define this segmentation. Mass, center of gravity, and inertial properties could be measured directly from a solid casting of the surface form shoulder girdle after separation from the thorax. Also, it is expected that a related mathematical procedure could be used to separate thorax from shoulder in the McConville et al. (1980) data.

In conclusion, the traditional segmentation and linkage system has been adopted as the only one feasible based on available data. It has been simplified slightly by coupling hand and lower arm masses, although the location of the wrist joint is specified. This linkage arrangement will be assumed throughout the remainder of the report.



6.0 CONSTRUCTION OF SEGMENTATION PLANES

The construction of segmentation planes is based largely upon the scheme used by McConville et al. (1980) in their determination of anthropometric relationships of body and body segment moments of inertia. The constructions are modified somewhat to account for differences between body segment relationships in the seated and standing postures.

6.1 Head Plane

The head plane is defined to pass through the left and right gonial points and the nuchale for a standing subject. As head orientation is very similar for both standing and seated posture, it is assumed that the procedure can be directly adopted. The gonial points are available from UMTRI measurements. However, the nuchale was estimated from values given in the McConville et al. report. To accomplish this, nuchale coordinates in the head anatomical coordinate system were rotated and translated into the UMTRI standard seat coordinate system. The three points defining the head segmentation plane are therefore:

Point ————	X _H (mm)	Y _H (mm)	Z _H (mm)
Nuchale	-279	0	579
Gonion (L)	-173	70	544
Gonion (R)	-173	- 70	544

The formula for this plane is:

$$.31354X_{H} + .94958Z_{H} - 462.33 = 0$$

It should be noted that formulae for segmentation planes can be used to determine the intersection of the plane with the surface form at points other than surface landmarks used in the definitions.

6.2 Neck Plane

The neck segmentation consists of two planes. The first plane is parallel to the floor and anterior to cervicale. The second plane originates at the clavicale and tilts up and back at a 45-degree angle until it intersects with the horizontal plane. Because the orientation of head and neck are similar in the seated and standing postures, this procedure was adopted directly from McConville et al. The points used for the construction were:

Point ————	X _H (mm)	Y _H (mm)	Z _H (mm)	
Cervicale	-266	0	489	
Clavicale	-145	± 23	443	

The two planes were found to intersect along the line defined by $X_H=191$, $Z_H=489$. The formula for the first plane anterior to the cervicale is:

$$Z_{H} = 489$$
 for $X_{H} \le -191$.

The formula for the second plane is:

$$.70710X_{H} + .70710Z_{H} - 210.72 = 0$$
 for $X_{H} \ge -191$.

6.3 Thorax Plane

The McConville et al. definition specifies that the plane originates at the 10th rib mid-spine landmark and passes through the torso parallel with the standing surface. In order to approximate this plane in the seated posture, a line was constructed from the 10th rib landmark which was perpendicular to a line connecting the T12 and L5 surface landmarks. This line, which is roughly perpendicular to the body centerline, is intended to separate the thorax which has a bony skeletal periphery from the abdomen which has a soft tissue periphery. In dynamic applications, thorax and abdomen will have very different stiffnesses and are coupled very differently to the bony skeleton. The points used in construction of the plane are:

Point	X _H (mm)	Y _H (mm)	Z _H (mm)
R10/Back Perpendicular	-209	0	71
R10	- 93	±156	133

The formula for the thorax plane is:

$$.47138X_{H} - .88194Z_{H} + 161.14 = 0$$

It should be noted that the L2 surface landmark is approximately 17 mm from the plane and the L2/L3 joint center falls less than 10 mm above the plane (see Figure 3).

6.4 Abdomen Plane

The McConville et al. definition specifies that the plane "originates at the iliocristale landmarks and passes through the torso parallel with the standing surface." This plane presents a dilemma even more complex than the thorax. Because of the spinal tilt due to the seated posture, it would seem logical to develop a segmentation scheme similar to that used for the thorax.

However, on the basis of the physical nature of the abdomen mentioned in Section 6.3, it would make more sense to define a scheme which better delineates the extent of the soft abdomen. A pair of new planes can be proposed, the first of which angles backward from the iliocristale landmarks perpendicular to the same line connecting the T12 and L5 surface landmarks which was used in constructing the thorax plane (see Figure 3). The second plane is horizontal and extends from the iliocristale target to the front of the body. The region of maximum abdominal protrusion is included in this definition. This planes passes just above the anterior-superior iliac spine targets and about 50 mm above pubic symphysis.

Two more observations on the McConville et al. data conclude the information required for making a final decision on the abdomen segmentation plane. The first is that the distance between the thorax and abdomen planes, which are parallel, is similar to the distance from the iliocristale landmark to the thorax segmentation plane developed from the UMTRI data. The second is that the data which are available for mass and inertial properties apply only to the parallel planes through the iliocristale and 10th rib landmarks.

CODE

JOINTS (TI2/LI, L2/L3, L5/SI, HIP)

TI2 - TI2 LANDMARK

L2 - L2 LANDMARK

RIO1 - POINT ON SURFACE FROM RIO

I 1 - POINT ON SURFACE FROM ILIOCRISTALE

L5 - L5 LANDMARK

RIO - IOth RIB LANDMARK

I - ILIOCRISTALE LANDMARK

U - UMBILICUS LANDMARK

M - MAXIMUM ABDOMINAL PROTRUSION

ASIS - ANTERIOR SUPERIOR ILIAC SPINE

TH - THORAX SEGMENTATION PLANE

AB - ABDOMEN SEGMENTATION PLANE

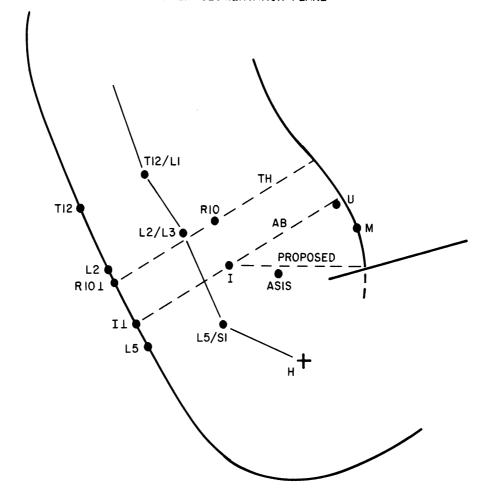


FIGURE 3. Construction of thorax and abdomen segmentation plane.

The conclusion was to present data based on a segmentation plane parallel to the thorax plane and recommend that new inertial and mass properties be developed based on the proposed definition given above and illustrated in Figure 3. The points used in the construction of the plane are:

Point	X _H (mm)	Y _H (mm)	Z _H (mm)
	-188	0	35
	- 80	±161	93

The formula for the segmentation is:

$$.47312X_{H} - .88098Z_{H} + 119.78 = 0$$

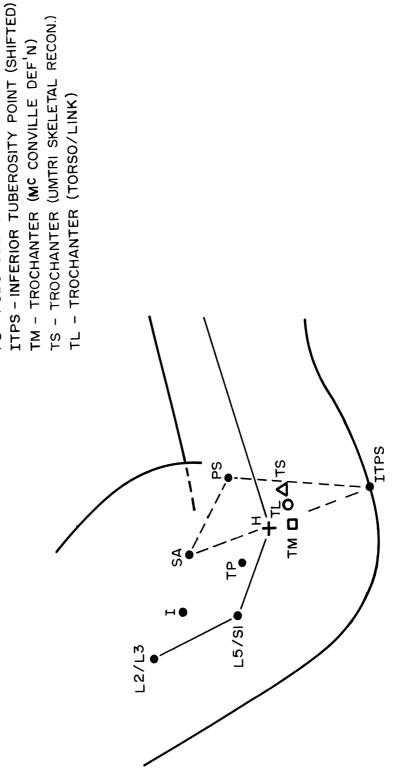
The recommendation, then, is to use this formula until mass, center of gravity, and inertial properties can be measured directly from a solid casting of the surface form abdomen with the additional material from the pelvic region. Similar measurements would be required for the new pelvic region.

6.5 Hip Plane: First Attempt

The McConville et al. definition specifies that the plane "originates at the center of the crotch and passes laterally midway between the anterior-superior iliac spine and trochanter landmarks along the lines of the right and left inguinal ligaments." Construction of these planes thereby requires information on several features of the anatomy of the subject population.

From plots of data (Figure 4) and a review of pelvis and femur internal geometry, it appeared that a comparison should be made between the UMTRI trochanterion surface landmark obtained photographically and similar data obtained by other investigators. The torso-link data of Snyder et al. (1972) was gathered from a somewhat similar population (weight=175 pounds, height=70 inches). Seated measurements on these subjects show:

- Seat back to trochanter = 14.06 cm
- Seat surface to trochanter = 8.84 cm



PS - PUBOTUBEROSITY SHIFTED

I - ILIOCRISTALE SA - SHIFTED ASIS

JOINTS (L2/L3, L5/SI, HIP)

CODE

FIGURE 4. Construction of hip segmentation plane.

From the drawing of our somewhat more slumped subject and estimates of seat cushion and seat back lines, the trochanter landmark from photographic measurements yielded the following data using a similar measurement scheme:

- Seat back to trochanter = 12.1 cm
- Seat surface (deepest point) = 14.7 cm
 to trochanter

In order to obtain a further check on the location of this point, a mid-sized-male femur matching the average femur length of subjects in the UMTRI sample was set up in the lab to locate the pivot center in the acetabulum. The femur was oriented in space using the medial and lateral epicondyle point data and the center of the head of the femur (H-point). Using the McConville et al. definition of the trochanter landmark based on the most superior point (determined from the orientation of the femur in a standing subject), the trochanter landmark was found to be 5 mm forward and 25 mm down from the H-point. Using the present project definition of most lateral point, the trochanter landmark was found to be 35 mm forward and 12 mm down. The four versions are shown in Figure 4. The point estimate from the torso-link study falls between the values obtained from the skeletal reconstruction. In conclusion, a new point is defined called trochanterion (skeletal reconstruction) with the coordinates $X_{H}=20$, $Y_{\mu}=\pm 203$, $Z_{\mu}=-20$. This will be used in all analyses which follow.

Although a point on the inguinal ligament line is well represented by the thigh/abdominal junction point $(21, \pm 122, 81)$, it was not found possible to obtain realistic selection of a point representing the center of the crotch. Because three non-colinear points are required to construct a plane in three dimensions, the original hip plane concept used by McConville et al. was dropped.

6.6 Hip Plane: Successful Attempt

The objective of hip segmentation plane is to separate the upper leg region from the bony pelvis. The procedure used by Clauser et al. (1969) extended the plane "from the level of the iliac crest inferiorly along the external shelf of the ilium, cutting the rim of the

acetabulum and severing the ischial tuberosity (posteriorly at the level of the attachment of m. semimembranous, anteriorly at the mid-point of the ascending ramus of the ischium)." That procedure yields a plane which approximately bisects the H-point and removes as little of the bony pelvis as possible.

A procedure which defines a plane based on available data and which avoids cutting into the pelvic bone mass uses the four bony landmarks quantified by Reynolds et al. (1981):

Point	X _H (mm)	Y _H (mm)	Z _H (mm)
Anterior-Superior Iliac Spines Pubotuberosity	-25 34	±116 ± 25	78 29
Lateral Tuberosity Point	20	± 67	-55
Inferior Tuberosity Point	37	± 39	-61

To define a pelvic mass which is separate from the upper leg mass, a segmentation plane is proposed which does not intersect the average pelvis but which maintains the relation to the inguinal ligaments, is very similar to the other procedures, and can be quantified in three-dimensional coordinates.

To present pubotuberosity, a point 35 mm lateral to the pubic symphysis on (or near) the dummy surface has been selected. Likewise, for the anterior-superior iliac spine, a lateral shift of 10 mm from the surface marker is selected. The final point, which in some sense represents the bottom of the crotch, is selected as 10 mm lateral to and projected vertically to the seat surface from the inferior tuberosity point. These three points are:

Point	X _H (mm)	Y _H (mm)	Z _H (mm)
Pubotuberosity Surface	51	± 35	41
Shifted ASIS	-25	±126	83
Shifted Inferior Tuberosity	37	± 49	-107

The formula for the segmentation is:

$$-.76487X_{H} \pm .64407Y_{H} + .01143Z_{H} + 61.082 = 0$$

where the positive sign on Y_H is the right side of the body. This segmentation plane passes 8 mm lateral (oblique) to the H-point joint center and less than 2 mm from the lateral tuberosity.

6.7 Knee Plane

The McConville et al. definition specifies that the plane "passes through the lateral femoral epicondyle landmark parallel to the standing surface." Because of the difference between the standing and seated postures, this definition is not realistic. As an alternative, which is designed to separate the upper and lower leg masses, it is proposed to pass the plane through the lateral femoral epicondyles bisecting the angle in the $X_H Z_H$ plane made by the lines connecting the upper and lower leg links. The plane is assumed to be parallel to the Y_H coordinate axis and has an angle of 14.56 degrees with respect to the vertical (Figure 5). Its formula is:

$$-.96788X_{H} + .25139Z_{H} + 358.59 = 0$$

The plane passes within 0.2 mm of the knee joint center.

6.8 Ankle Plane

The McConville et al. definition specifies that the plane "originates at the sphyrion landmark and passes through the ankle parallel to the standing surface." This plane is maintained fairly well by constructing a plane through the sphyrion, parallel to the Y_H axis, and perpendicular to a line connecting the knee and ankle joints projected into the $X_H^2Z_H$ plane. Its angle with the vertical is 42.35 degrees and the formula is:

$$.73904X_{H} - .67366Z_{H} - 605.88 = 0$$

6.9 Shoulder Plane

The McConville et al. definition specifies that the plane "originates at the acromion landmark and passes downward through the anterior and posterior scye creases at the level of the axilla." This

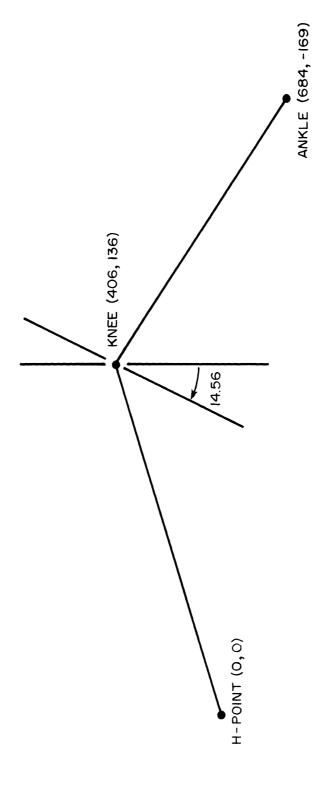


FIGURE 5. Construction of knee segmentation plane.

segmentation plane appears to be similar for both the standing and seated postures. The three points needed for its definition are:

Point	X _H (mm)	Y _H (mm)	Z _H (mm)
Acromion	-224	±203	419
Anterior Scye	- 97	±154	380
Posterior Scye	-214	±197	306

The formula for this segmentation is:

$$.35502X_{H} \pm .93466Y_{H} - .01821Z_{H} - 102.58 = 0$$

where the plus sign on Y_H refers to the left side of the body. The distance of this plane from the glenohumeral joint center is estimated to be proximal by 14 mm while the distance to the claviscapular joint is estimated to be even larger at 35 mm. It is recommended that this segmentation procedure be evaluated carefully during an overall review of the definition of the entire shoulder girdle (Section 9).

6.10 Elbow Plane

The McConville et al. definition specifies that the plane "originates at the olecranon landmark and passes through the medial and lateral humeral epicondyle landmarks." This definition appears to be satisfactory. The three points needed for definition are:

Point	X _H (mm)	Y _H (mm)	Z _H (mm)
Olecranon	53	±210	186
Medial Humeral Epicondyle	32	±173	199
Lateral Humeral Epicondyle	32	<u>+</u> 242	224

The formula for the segmentation is:

$$-.96349X_{H} \pm .22Y_{H} - .60719Z_{H} + 107.2 = 0$$

where the plus sign on $Y_{\mbox{\scriptsize H}}$ refers to the left side of the body. The plane passes about 3 mm from the estimated joint center for the seated posture.

6.11 <u>Summary</u>

A summary of the formulation of the segmentation planes is given in Table $5. \,$

TABLE 5
FORMULATION OF SEGMENTATION PLANES

Head:	.31354x _H + .94958z _H - 462.33 = 0
Neck:	$.70710X_{H} + .70711Z_{H} - 210.72 = 0$
	(for all X _H ≥ -191)
Thorax:	$.47138x_{H}88194z_{H} + 161.14 = 0$
Abdomen:	$.47312X_{H}88098Z_{H} + 119.78 = 0$
Hip:	$76487X_{H} \pm .64407Y_{H} + .01143Z_{H} + 61.082 = 0$
	(+ sign on Y _H for right side of body)
Knee:	$96788x_{H} + .25139Z_{H} + 358.59 = 0$
Ankle:	$.73904x_{H}67366z_{H} - 605.88 = 0$
Shoulder:	$.35502X_{H} \pm .93466Y_{H}01821Z_{H} - 102.58 = 0$
	(+ sign on Y _H for left side of body)
Elbow:	$76349X_{H} \pm .22Y_{H}60719Z_{H} + 107.2 = 0$
	(+ sign on Y for left side of body)

7.0 DEVELOPMENT OF ANATOMICALLY BASED SEGMENT COORDINATE SYSTEMS

This section shows the development of anatomically based coordinate systems for each of the various segments of the body. The coordinate systems which have been constructed are the same, or very similar to, those which have been reported by McConville et al. (1980) in developing anthropometric relationships of body and body segment moments of inertia. As such, they will be used directly in the presentation of center of mass and inertial data and will provide the linkage between the coordinate systems defining the principal axes of inertia and the standard coordinate system at the H-point center.

In order to construct coordinate systems and relate them to the standard system, it is necessary to know three points in the segment. For most of the present analyses, this is done by selecting one point at the origin, a second point on an axis, and the third point in one of the orthogonal planes. The sub-sections that follow identify the points required, discuss necessary details of the construction, and present results as direction cosine matrices for transforming from anatomical to standard coordinates.

The subscript A is used to denote anatomical coordinate systems. It should be noted that there is a different anatomical coordinate system for each segment and more subscripts could be added to represent each specific anatomical system. However, it is felt that this additional cumbersome notation is unnecessary due to the context in which the symbols are used.

7.1 Head Axis System

The McConville et al. definition for the head axis system is as follows:

- \bullet $X_{\underline{A}}Y_{\underline{A}}$ Plane: Right and left tragion and right infraorbitale
- $Y_{\Delta}Z_{\Delta}$ Plane: Right and left tragion
- X_AZ_A Plane: Sellion

Coordinates for the three points for the head axis system are:

Point	X _H (mm)	Y _H (mm)	Z _H (mm)
Infraorbitale (R)	- 96	- 34	620
Tragion (L)	-185	83	614
Tragion (R)	-185	- 83	614

The origin of the coordinate system is at the center of a line connecting the tragions. In lab coordinates the point is:

$$X_{H} = -185, Y_{H} = 0, Z_{H} = 614$$

The origins of all segment coordinate systems are summarized in Table 6. The direction cosine matrix for the transformation from laboratory into head segment coordinates is given in Table 7 (degrees) and Table 8 (cosine of angle).

TABLE 6

LOCATION OF ORIGINS OF SEGMENT ANATOMICAL COORDINATE SYSTEMS

Segment	X _H (mm)	Y _H (mm)	Z _H (mm)
Head	-185	0	614
Neck	-266	0	489
Thorax	-209	0	71
Abdomen	- 93	0	133
Pelvis	- 25	0	83
Upper Arms	-224	+203*	419
Lower Arms	46	±243	209
Upper Legs	20	±203	- 20
Lower Legs	424	± 88	128
Feet	796	±126	- 96

*The positive sign on $\boldsymbol{Y}_{\boldsymbol{H}}$ refers to the left side of the body.

TABLE 7

ANATOMICAL AXES WITH RESPECT TO HIP POINT AXIS SYSTEM (Cosine Matrix Expressed in Degrees)

Segment		X _H	YH	z _H
Head	X	3.86	90.	86.14
	Y A	90.	0.	90.
	Z A	93.86	90.	3.86
Neck	X Y Z A	20.8 90. 69.2	90. 0. 90.	110.8 90. 20.8
Thorax	X	7.8	90.	82.2
	Y A	90.	0.	90.
	Z A	97.8	90.	7.8
Abdomen	X Y Z A	28.1 90. 118.1	90. 0. 90.	61.9 90. 28.1
Pelvis	X	61.05	90.	28.96
	Y A	90.	0.	90.
	Z A	151.04	90.	61.05
Upper Arm (L)	X	52.5	105.7	41.8
	Y A	85.8	17.2	73.3
	Z A	142.2	96.9	53.0
Upper Arm (R)	X	52.5	74.3	41.8
	Y A	94.2	17.2	106.7
	Z A	142.2	83.1	53.0
Lower Arm with Hand (L)	X	128.2	71.4	44.1
	Y A	68.6	22.2	95.6
	Z A	134.1	78.4	133.5
Lower Arm with Hand (R)	X	128.2	108.6	44.1
	Y A	111.4	22.2	84.4
	Z A	134.1	101.6	133.5
Upper Leg (L)	X Y Z A	110.9 86.0 158.8	83.8 6.3 88.1	21.9 95.1 111.2
Upper Leg (R)	X Y Z Z	110.9 94.0 158.8	96.2 6.3 91.9	21.9 84.9 111.2

TABLE 7
ANATOMICAL AXES WITH RESPECT TO HIP POINT AXIS SYSTEM (Cosine Matrix Expressed in Degrees, Continued)

Segment		Х _Н	YH	z _H
Lower Leg (L)	X Y Z A	46.2 103.5 133.1	67.6 22.9 85.9	52.2 108.0 43.3
Lower Leg (R)	X Y Z A	46.2 76.5 133.1	112.4 22.9 94.1	52.2 72.0 43.3
Foot (L)	X Y Z A	59.9 90. 149.9	78.4 13.4 83.3	32.7 103.4 60.8
Foot (R)	X Y Z A	59.9 90. 149.9	101.6 13.4 96.7	32.7 76.6 60.8

TABLE 8

ANATOMICAL AXES WITH RESPECT TO HIP POINT AXIS SYSTEM (Cosine Matrix)

Segment		x _H	YH	z _H
Head	X Y A Z A	.998 0. 0673	0. 1. 0.	.0673 0. .998
Neck	X Y A Z A	.935 0. .355	0. 1. 0.	355 0. .935
Thorax	X Y A Z A	.991 0. 136	0. 1. 0.	.136 0. .991
Abdomen	X Y A Z A	.882 0. 471	0. 1. 0.	.471 0. .882
Pelvis	X Y Z A	.484 0. 875	0. 1. 0.	.875 0. .484
Upper Arm (L)	X Y Z A	.609 .0728 790	-0.270 0.955 -0.120	.746 .287 .602
Upper Arm (R)	X Y Z A	.609 0728 790	0.270 0.955 0.120	.746 .287 .602
Lower Arm with Hand (L)	X Y Z A	618 .365 697	0.319 0.926 0.201	.718 0982 689
Lower Arm with Hand (R)	X Y Z A	618 365 697	-0.319 0.926 -0.201	.718 .0982 689
Upper Leg (L)	X Y A Z A	356 .0705 932	0.108 0.994 0.0340	.928 0884 362
Upper Leg (R)	X Y A Z A	356 0705 932	-0.108 0.994 -0.0340	.928 .0884 362

TABLE 8

ANATOMICAL AXES WITH RESPECT TO HIP POINT AXIS SYSTEM (Cosine Matrix, Continued)

Segment		x _H	YH	z _H
Lower Leg (L)	X A Y A Z A	.692 234 683	0.382 0.922 0.0709	.612 310 .727
Lower Leg (R)	X A Y A Z A	.692 .234 683	-0.382 0.922 -0.0709	.612 .310 .727
Foot (L)	XA YA ZA	.501 0. 865	0.200 0.973 0.116	.842 232 .487
Foot (R)	X A Y A Z A	.501 0. 865	-0.200 0.973 -0.116	.842 .232 .487

It is now possible to compare McConville et al. surface landmark locations reported in segment coordinates with similar surface landmarks measured at UMTRI. The X_A distance from tragion to infraorbitale is 72.3 mm for McConville et al. and 89 mm for UMTRI which is clearly a large discrepancy. A check of Churchill and Truett (1957) data show subtracting "external canthus to wall" from "tragion to wall" yields 63 mm. That value is comparable to the McConville et al. data. To further study the issue, head-size data such as length and circumference were checked and found very comparable as shown below:

Point	McConville et al. 1980	UMTRI 1983
Head Length (mm)	199.3	197.4
Head Circumference (mm)	572.7	570.6

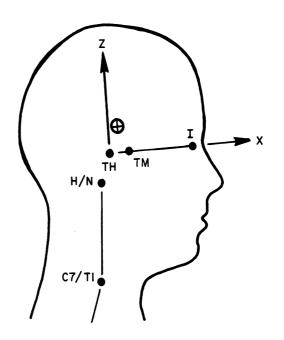
Because of this similarity, the discrepancy is assumed to be in tragion location. The origin of coordinates is selected to be between the UMTRI tragions as indicated previously.

Figure 6 shows the head anatomical coordinate system. The McConville et al. coordinate system is superimposed with the infraorbitales coincident and the tragions located along the X_A axis. In this presentation, the center of volume, as specified in the McConville et al. system, lies 8.5 mm behind and 31.3 mm above the McConville et al. origin and at the same time is 8.4 mm in front of and 31 mm above the UMTRI origin. The relationship of origin to center of volume in the UMTRI definition is closer to that of Beier et al. (1980). Because of the overall head dimensional similarity (e.g., length, breadth, circumference), it is felt that the above analysis is a reasonable approximation for the various data resources.

7.2 Neck Axis System

The McConville et al. definition for the neck axis system is as follows:

- \bullet $X_A Z_A$ Plane: Adam's apple, cervicale, suprasternale
- \bullet $~X_A{}^Y_A$ Plane: Including a line in the $X_H{}^Z_H$ plane connecting the cervicale with the midpoint of a line connecting the clavicales
- YAZA Plane: Cervicale



CODE

JOINTS (H/N, C7/TI)

- HEAD CENTER OF GRAVITY

I - INFRAORBITALE (UMTRI AND MCCONVILLE SUPERIMPOSED)

TM - MCCONVILLE TRAGION

TH - UMTRI TRAGION

FIGURE 6. Head anatomical coordinate system.

The three points required are:

Point	X _H (mm)	Y _H (mm)	Z _H (mm)	
Cervicale Clavicale (L)	-266 -145	0 23	489 443	
Clavicale (R)	-145	- 23	443	

Because of the symmetry assumption, it is not necessary to provide coordinates for Adam's apple or suprasternale. The origin of the coordinate system is at the cervicale:

$$X_{H} = -266, Y_{H} = 0, Z_{H} = 489$$

The direction cosine matrix for the transformation is given in Tables 7 and 8.

7.3 Thorax Axis System

The McConville et al. definition of the thorax axis system is as follows:

• X_AZ_A Plane: Suprasternale, cervicale, and mid-spine at level of 10th rib

 \bullet Y_AZ_A Plane: Cervicale and 10th rib level at mid-spine

 \bullet $X_A Y_A$ Plane: 10th rib level at mid-spine

The symmetry assumption reduces the requirements to the points defining the Y_AZ_A and X_AY_A planes. The "l0th rib level at mid-spine" point is not applicable to the seated position (see Section 6.3). In order to approximate this point for a seated posture, a line was constructed from the l0th rib landmark which was perpendicular to a line connecting the T12 and L5 surface landmarks. In other words, a line was constructed which was perpendicular to an approximation of the seat back line. The point which was selected to replace the McConville et al. point is called the R10/back perpendicular point and is the intersection of the perpendicular line with the line connecting the T12 and L5 surface

landmarks. The points needed for constructing the transformation are thus:

Point	X _H (mm)	Y _H (mm)	Z _H (mm)
Cervicale	-266	0	489
R10/Back Perpendicular	-209	0	71

The origin of coordinates is at the R10/back perpendicular point and the direction matrix for the transformation is given in Tables 7 and 8.

7.4 Abdomen Axis System

The McConville et al. definition for the abdomen axis system is as follows:

• XAYA Plane: Right and left 10th rib and at mid-spine at level of 10th rib

• $Y_{\Delta}Z_{\Delta}$ Plane: Right and left 10th rib

• $X_{\Delta}Z_{\Delta}$ Plane: 10th rib mid-spine

Again the "mid-spine at level of 10th rib" point is not applicable to the seated posture. The R10/back perpendicular point, discussed in Section 7.3, is again used as a substitute. The points needed for construction of the transformation are:

Point	X _H (mm)	Y _H (mm)	Z _H (mm)
R10/Back Perpendicular	-209	0	71
10th Rib (L)	- 93	156	133
10th Rib (R)	- 93	-156	133

The origin of coordinates is at the center of a line connecting the right and left 10th rib surface landmarks:

$$X_{H} = -93, Y_{H} = 0, Z_{H} = 133.$$

The direction cosine matrix for the transformation is given in Tables 7 and 8.

7.5 Pelvis Axis System

The McConville et al. definition of the pelvis axis system is as follows:

- YAZA Plane: Right left anterior-superior iliac spines and and symphysion
- $X_{\Delta}Y_{\Delta}$ Plane: Right and left anterior-superior iliac spines
- XAZA Plane: Mid-spine at level of posterior-superior iliac spine

The body symmetry assumption eliminates the need for the mid-spine at level of posterior-superior iliac spine point. Remaining are definitions of symphysion and anterior-superior iliac spine. Four different axis systems for the pelvis are used at various places in this report. The first is the laboratory system based on the standard seat. The second is that of McConville et al. which is used for mass and inertial property definition. The third is that of Reynolds et al., used in the study of the spatial geometry of the pelvic bone, and the fourth is the UMTRI pelvis segment axis system. As a result, three sets of definitions should be compared, those of McConville et al. (1980), Reynolds et al. (1981), and the present UMTRI study. They are:

Symphysion

McConville et al. 1980: "The lowest point on the superior border of the pubic symphysis, the anterior juncture of the pelvic bones."

Reynolds et al. 1981: "The midpoint of a line between point 180, right superior pole, pubic symphysis, and point 183, left superior pole, pubic symphysis..." Point 180 is "at the intersection of the longitudinal midline axis of the pubic symphysis with the superior margin of the symphyseal face of the right innominate bone."

UMTRI 1983: "The superior margin of the pubic symphysis in the midline" (i.e. pelvic crest).

Anterior-Superior Iliac Spine

McConville et al. 1980: "The most prominent point on the anterior-superior spine of the ilium."

Reynolds et al. 1981: "Left iliospinale, summum, 201-203: The left innominate rests on its medial surface with the iliac blade and pubic symphysis in contact with the horizontal surface of an osteometric board. Move the bone into the right angle corner of the board in such a way that the superior border of the iliac crest in contact with the vertical plate ..."

UMTRI 1983: "The most prominent point on the anterior-superior spine of the left ilium."

With respect to both points, the McConville et al. and UMTRI definitions refer to surface landmarks while Reynolds et al. refers directly to the skeleton. In comparing the definitions, the attempt was made to visualize the Reynolds et al. quantities as if tissue were in place over the bone. From this point of view, the symphysion targets of UMTRI and Reynolds et al. appear to be directed at approximately the same point while the McConville et al. definition is a bit more anterior. It is estimated that the difference is less than one centimeter. For the anterior-superior iliac spines, the McConville et al. and UMTRI definitions are identical. The Reynolds et al. definition, which is more precise in an absolute measurement sense, appears to define a very similar point to the other two.

The origin of coordinates in the three segment coordinate systems is based on the midpoint of a line connecting the anterior-superior iliac spines. As these points are defined to be nearly the same (assuming the tissue thickness shift for the Reynolds et al. system is valid), then the origins are assumed to coincide (with the Reynolds et al. system based on the related skeletal landmarks under the surface of the skin). The symphysion is used to construct an axis direction in the three cases. The slight difference in the McConville et al. definition is believed to be within the error bounds of the measurements but should ultimately be evaluated using the concepts suggested by Robbins (1977) in a brief study of errors in definition of an anatomically based coordinate system using anthropometric data.

The previous discussion shows a procedure for merging the data bases of UMTRI, McConville et al., and Reynolds et al. The results have already been used in establishment of a standard seat coordinate system (Section 4). They were used in Section 9 to locate the hip and lumbar-spinal (L5/S1) joints based on Reynolds et al. work. They are used here to obtain a transformation to segment coordinates in order to utilize the pelvic mass and inertial data of McConville et al.

The three points needed for construction of the transformation are:

Po	int X _H (mm)	Y _H (mm)	Z _H (mm)
ASIS		116	83
ASIS Symph		-116 0	83 41

The origin of the anatomical system is at:

$$X_{H} = -25, Y_{H} = 0, Z_{H} = 83$$

The direction cosine matrix for the transformation is given in Tables 7 and 8.

7.6 Upper Arm Axis System

The McConville et al. definition for the upper arm axis system is as follows:

ullet Y $_{A}$ Z Plane: Acromion as well as medial and lateral humeral epicondyles

 \bullet $X_A Z_A$ Plane: Lateral humeral epicondyle and acromion

• X_ΔY_Δ Plane: Acromion

This axis system is not consistent with body mobility as the acromion is not part of the arm link. The axis system migrates as the arm rotates. With respect to the standing position, in which the McConville et al. data were developed, the anatomical long axis is approximately along the axis of the humerus. In forward reach, however, the axis from acromion to humeral epicondyles is above the axis of the humerus.

In the case of the seated occupant shown in Figure 1, it is seen that the upper arm is rotated less than 20 degrees from the torso long

axis. Therefore, for the present estimates of center of mass and inertial properties, the McConville et al. definition is assumed to be adequate. These basic properties probably will not vary much with arm rotation whereas the anatomical axis definition is totally inadequate for arm mobility studies.

The points needed for construction of the transformations are:

Point	X _H (mm)	Y _H (mm)	Z _H (mm)
Acromion (L and R) Lateral Humeral Epicondyle (L and R) Medial Humeral Epicondyle (L and R)	-224	±203	419
	32	±242	224
	32	±173	199

The origins of coordinates for the two segments are at the acromions:

$$X_{H} = -224$$
, $Y_{H} = \pm 203$, $Z_{H} = 419$

where the positive sign on Y_H refers to the left side of the body. The direction cosine matrices for both left and right upper arms are given in Tables 7 and 8.

7.7 Lower Arm Axis System (Hands Included)

The McConville et al. definition for the lower arm axis system is as follows:

• YAZA Plane: Distal end of ulnar and radial styloid processes and radiale

 \bullet X_AZ_A Plane: Distal end of ulnar styloid process and radiale

• XAYA Plane: Radiale

The points needed for construction of the transformations are:

Point	X _H (mm)	Y _H (mm)	Z _H (mm)
Radiale (L and R)	46	±243	209
Ulnar Styloid (L and R)	226	±191	387
Radial Styloid (L and R)	211	±135	399

The origins of coordinates for the two segments are at the radiales as given. The direction cosine matrices for both left and right lower arms are given in Tables 7 and 8.

7.8 Upper Leg (Complete Up to Pelvis) Axis Systems

The McConville et al. definition for the upper leg axis system is as follows:

 \bullet $\text{Y}_{\text{A}}\text{Z}_{\text{A}}$ Plane: Trochanterion as well as right and left lateral femoral epicondyles

 \bullet $X_{\Delta}Z_{\Delta}$ Plane: Lateral femoral epicondyles and trochanterion

• $X_{\Delta}Y_{\Delta}$ Plane: Trochanterion

The points needed for construction of the transformation are:

Point	X _H (mm)	Y _H (mm)	Z _H (mm)
Trochanterion (skeletal reconstruction, L and R)	20	±203	- 20
Lateral Femoral Epicondyle (L and R)	404	±189	127
Medial Femoral Epicondyle (L and R)	407	± 87	142

The point trochanterion (skeletal reconstruction) was defined and developed in Section 6.5 of this report. The origins of coordinates for the two segments are at trochanterions (skeletal reconstruction) as given. The direction cosine matrices for both left and right upper legs are given in Tables 7 and 8.

In order to compare the geometry of the upper legs using the McConville et al. and UMTRI data bases, the distance from trochanterion to femoral epicondyles was computed. The UMTRI leg appeared to be about 20 mm short. However, the two studies palpated different points on the trochanter (Section 6.5). When this is taken into account, there is only about 10 mm difference between the two studies which is estimated to be quite reasonable given the experimental difficulties with trochanterion.

7.9 Lower Leg Axis Systems

The McConville et al. definition for the lower leg axis system is as follows:

• $Y_{\Delta}Z_{\Delta}$ Plane: Tibiale, sphyrion, lateral malleolus

• $X_{\Delta}Z_{\Delta}$ Plane: Sphyrion and tibiale

• X_AY_A Plane: Tibiale

The points needed for construction of the transformation are:

Point	X _H (mm)	Y _H (mm)	Z _H (mm)
Tibiale (L and R)	424	± 88	128
Sphyrion (L and R)	684	±61	-149
Lateral Malleolus (L and R)	680	±126	-185

The origins of coordinates for the two segments are at tibiale as given above. The direction cosine matrices for both left and right lower legs are given in Tables 7 and 8.

7.10 Feet Axis Systems

The McConville et al. definition for the feet axis systems is as follows:

 X_AY_A Plane: Metatarsal/phalangeal I and V landmarks and posterior calcaneus

• $X_{\Delta}Z_{\Delta}$ Plane: Tip of digit II and posterior calcaneus

• $Y_A Z_A$ Plane: Metatarsal/phalangeal I

The posterior calcaneus is estimated to coincide with the heel point on the standard seat buck. Using the data of McConville et al. and the relationship between the four points required for construction of the system, an anatomical origin was computed. This point was combined with two others, as follows, to construct the transformation:

Point	X _H (mm)	Y _H (mm)	Z _H (mm)
Constructed Origin (L and R) Metatarsal/Phalangeal I (L and R) Heel Point (L and R)	796	±126	- 96
	796	± 84	-86
	705	± 94	-250

The direction cosine matrices for both left and right feet are given in Tables 7 and $8. \,$



8.0 VOLUME, MASS, AND INERTIAL PROPERTIES

The volume, mass, and inertial properties are based on the results of McConville et al. 1980. For each of the segments the following data are provided:

- Anthropometry of segment (means)
- Volume (mean values and regression equations using anthropometric measures)
- Center of volume from anatomical axis origin
- Principal moments of inertia (mean values and regression equations using anthropometric measures)
- Principal axes of inertia with respect to anatomical axes

The following four subsections of this report compare the basic anthropometric properties of the UMTRI-seated and Air-Force-standing populations, develop the volume and mass properties of the body segments, present centers of gravity based on center of volume, and tabulate the inertial properties and principal axes.

8.1 Basic Anthropometric Properties of Each Segment

For each body segment a variety of anthropometric measurements were taken in both the McConville et al. study and the present one at UMTRI. One of the uses of these data is in regression equations for segment volume and inertial properties. As such, they will be discussed and compared in some detail. The measurements made at UMTRI were taken in the vehicle seated posture, where possible, whereas the standard standing position was used in the previous work. The following text compares the anthropometry and discusses the effects that differences might have on segment shape. It should be noted that the comparable statures and weights are:

Quantity	McConville et al. (1980)	<u>UMTR I</u>
Stature (mm)	1774.9	1751.4
Weight (lbs)	170.4	168.8

For the <u>head</u>, data from the two studies are as follows:

	Quantity	McConville et al. (1980)	<u>UMTR I</u>
Head	Length	199.3	197.4
	Breadth	153.2	158.0
Head	Circumference	572.7	570.6
Head	Height	166.5	230.9

These measurements are very comparable, except for head height, and can be used directly in regression equations. In the original data it was defined as the difference between stature and mastoid heights while at UMTRI it was taken as the distance from the bottom of the chin to the highest point on the top of the head.

For the <u>neck</u>, data from the two studies are as follows:

	Quantity	McConville et al. (1980)	<u>UMTR I</u>
Neck	Circumference	376.7	388.2
	Breadth	122.9	118.0
	Length	81.8	84.8

These measurements are very comparable. The UMTRI breadth and circumference data are based on the average of measurements taken at two heights along the neck.

For the thorax, data from the two studies are as follows:

Quantity	McConville et al. (1980)	UMTRI <u>Standing</u>	UMTRI Seated
Chest Circumference	965.1	961	1009.6
Chest Breadth	331.9		348.7
Thorax Length	403.1		(355, 390, 415)
10th Rib Breadth	298.5		
10th Rib Circumference	821.5		909.4

The basic data demonstrate a considerable difference between the seated and standing postures. The segmentation plane at the neck is horizontal for both postures whereas the front of the thorax segmentation plane has

been tilted upward to maintain an orientation approximately perpendicular to the seatback. The three numbers given for UMTRI (seated) thorax length were determined as follows:

- Vertical distance from neck segmentation plane to 10th rib landmark
- Direct distance from cervicale to 10th rib landmark
- Vertical distance from neck segmentation plane to 10th rib perpendicular intersection with seat back

That this redirection of the thorax segmentation plane and compressing of the abdominal and lower thoracic contents actually takes place appears to be verified by the increased chest circumference and breadth in the seated posture. The measure of thorax length in the standing posture (403.1 mm) is not too different from the distance along the seated spinal linkage from cervicale to the 10th rib landmark (390 mm). The curving of the spine in the seated posture does tend to compress the frontal abdominal and thorax region as indicated by the shorter thorax length obtained by using a parallel through the 10th rib landmark (355 mm). This will tend to move the center of gravity forward in the thorax as the seated posture is assumed. Because the curving of the spine tends to move the thorax segment Z_Δ axis further toward the front of the body than is the case with the McConville et al. axis, it will be assumed that this tends to compensate. (This can be visualized by connecting cervicale and R10/back perpendicular landmarks as has been done in Figure 7.) It should also be noted that the thorax segment X_{A} axis is placed further below the abdomen segmentation plane than in the McConville et al. case. This should tend to compensate for spreading of tissue toward the bottom of the thorax. The term "compensation" is used to reflect that the center of gravity will be moved around in the segment depending on the placement of segment coordinate axes.

In conclusion, the center of mass location will be conditionally accepted. In order to improve upon these data, a casting of the thorax segment should be made so that improved center-of-gravity and inertial properties can be measured directly as there is no easy computational procedure except for the photographic and analytical methods reported by McConville et al.

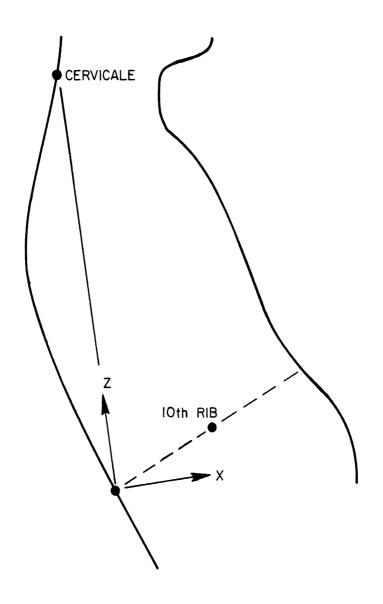


FIGURE 7. Segment axes in thorax for seated posture.

For the abdomen, data from the two studies are as follows:

Quantity	McConville et al. (1980)	UMTRI Standing	UMTRI Seated
Abdomen Length Waist Circumference 10th Rib Breadth	50.1 857.0 298.5	859.0	42.0 903.8
10th Rib Circumference Waist Breadth Suprailiac Skinfold	821.5 312.3 152.4	210.9	909.4 313.5

The major feature of this comparison is that the abdominal segment is thinner and has a greater circumference. This is caused by the curving of the spine as the pelvis rotates upward toward the rib cage during the process of sitting down in a car seat. A qualitative pilot study at UMTRI involving a targeted subject in both seated and standing postures yielded this same conclusion regarding the narrowing of the abdominal area. Section 6.4 of this report presented a recommendation for a different segmentation and delineation of the abdominal area which better defines the extent of the soft abdomen. Although data based on McConville et al. are being used in this volume, it is strongly recommended, as was done for the thorax, that castings of the proposed abdominal segment be made so that revised mass and inertial properties can be directly determined.

For the pelvis, data from the two studies are as follows:

Quantity	McConville et al. (1980)	UMTRI Standing	UMTRI <u>Seated</u>
Buttock Circumference	952.9	944.4	
Buttock Depth	240.8		220-255
Bispinous Breadth	222.9	224.6	
Pelvic Length	258.3		235
Hip Breadth (maximum)	346.2		384.7
Suprailiac Skinfold	152.4	210.9	

There are several differences between the data which appear to be related to postural differences. The UMTRI measure reported as buttock circumference is hip circumference (maximum). Representative buttock

depths can be selected by measuring the perpendicular distance to the seat back from anatomical landmarks. These distances range from about 220 mm at the pubic symphysis to about 255 mm at the point of maximum abdominal protrusion. It is therefore assumed that the McConville et al. value (240.8) is a rough measure of this quantity. Pelvic length is defined by McConville et al. as the difference between gluteal furrow height and iliocristale height. An UMTRI estimate for this quantity is the perpendicular distance from iliocristale to the seat surface. This perpendicular line is essentially parallel to the seat back. The pelvic length, although not strictly comparable, is smaller for the seated subject perhaps due to the compression of tissue during the seating process. Also, the seated hip breadth is larger as would be expected from tissue being displaced toward the side of the subject/seat interface during the seating process. Because the pelvic mass is to a great extent determined by the shape and extent of the bony pelvis, the mass and inertial properties will be computed based on the McConville et al. data. Some corrections are suggested by using the UMTRI modified anthropometric constructions just presented. If the proposed new segmentation plane for the abdomen is accepted, then it is recommended that a casting be made of the new pelvic mass in order to obtain data for revised properties.

For the upper arms, data from the two studies are as follows:

Quantity	McConville et al. (1980)	UMTRI Standing	UMTRI Seated
Axilla Arm Circumference	319.1		
Biceps Circumference Relaxed	299.7	298.6	
Biceps Circumference Flexed	321.0	-	314.6
Acromion-Radiale Length	333.9	329.0	
Elbow Circumference	265.7		285.3
Biceps Depth Relaxed	108.3		108.
Elbow Breadth	70.7		80.2
Biceps Skinfold	37.4		
Triceps Skinfold	94.4	100.4	
Axilla Arm Depth	124.9		

These measures are quite similar with the exceptions of elbow circumference which becomes larger as the elbow flexes and elbow breadth

which was measured across soft tissue for the UMTRI subjects. In the regression equations, the biceps circumference flexed data from UMTRI are substituted for axilla arm circumference in that the biceps are not flexed much in the driving posture. Also, the McConville et al. data for axilla arm depth are used.

For the <u>lower arms</u> (hands included), data from the two studies are as follows:

Quantity	McConville et al. (1980)	UMTRI <u>Standing</u>	UMTRI <u>Seated</u>
Elbow Circumference	265.7		285.3
Midforearm Breadth	79.5		82.0
Midforearm Circumference	234.2	253.7	182.5-275.3
Wrist Circumference	169.9		168.7
Hand Length	189.4	187.2	·
Hand Breadth	86.4	85.3	
Hand Circumference	208.7		
Forearm-Hand Length	459.8	474.0	

In most of the cases, similar, but not precisely the same, measurements were available for the two groups of subjects. The elbow circumference is larger due to flexion in the seated position. There was no equivalent measurement for midforearm circumference as UMTRI reported the minimum and maximum values given in the table. The forearm-hand length was measured with the arm flexed at 90 degrees for the UMTRI subjects while McConville et al. added radiale-stylion length to hand length.

For the upper legs, data from the two studies are as follows:

Quantity	McConville et al. (1980)	UMTRI <u>Standing</u>	UMTRI Seate
Thigh Length	465.5	435.3	447.
Upper Thigh Circumference	570.2		578.6
Mid Thigh Circumference	529.0	515.1	503.
Mid Thigh Depth	174.0		148.
Knee Circumference	374.1		392.2
Knee Breadth	96.1		101.
Gluteal Furrow Depth	193.8		184.

Thigh length is represented differently in the two studies. UMTRI uses trochanterion to lateral femoral epicondyle while McConville et al. reports tibiale to trochanterion. As the femoral epicondyle is a landmark associated with the upper leg link and closely correlated with the knee joint center, the UMTRI values will be used. Mid thigh depth is estimated as the distance from the top of the thigh to the seat surface and thus is smaller for the UMTRI sample. The knee measurements are undoubtedly larger based on the movement of tendons during knee flexion. All in all, the data appear sufficiently alike to warrant use of the McConville et al. data base. In summary, the overall shape changed surprisingly little.

For the <u>lower legs</u>, data from the two studies are as follows:

Quantity	McConville et al. (1980)	UMTRI <u>Standing</u>	UMTRI <u>Seated</u>
Calf Length	407.4	401.8	
Calf Circumference	376.8	367.4	372.9
Ankle Circumference	224.3		229.5
Knee Circumference	374.1		392.2
Ankle Breadth	59.0		72.7 (61.2
Knee Breadth	96.1		101.3
Calf Depth	120.2		117.7

These data are very similar. The knee circumference is larger for the UMTRI subjects due to flexion. The reason for the large difference in ankle breadths is unknown. UMTRI measurements include a minimum ankle breadth of 61.2.

For the feet, data from the two studies are as follows:

Quantity	McConville et al. (1980)	UMTRI <u>Standing</u>	UMTRI Seated
Foot Length	266.1	264.0	
Foot Breadth	104.9	95.7	
Sphyrion Height	70.7		80.0
Ankle Circumference	224.3		229.5
Arch Circumference	260.1		
Ball of Foot Circumference	257.3		

These data are fairly similar. Sphyrion height is defined to be the perpendicular distance from toeboard to sphyrion. It is believed this value is larger for the seated case because very little force is exerted on the foot in a normal seated position.

As a supplement to the study of the basic geometric properties of the body, a series of surface profile measurements was made on the original clay version of the surface form shortly before castings were made. Thin strips of paper were laid on the surface of the form to represent "tops, bottoms, and sides" of the various regions of the body. Figures 8, 9, and 10 show side, front, and back views of the clay form with strips attached. Points along these strips were digitized in three dimensions using a mechanical measurement frame. The coordinates of these surface points are included in Table 9. These points have been used in Figure 1 of this report and the full-size drawings (Blueprint Nos. MM-101, MM-102, MM-103, MM-104, and MM-105). Also, they have been used as an aid in reconstructing some of the non-standard anthropometry discussed in this section of the report.

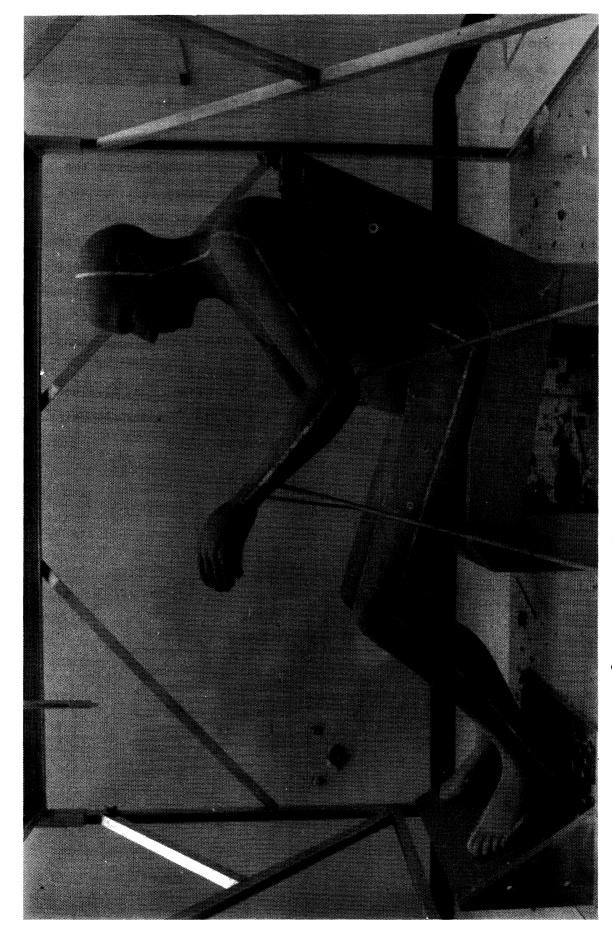


FIGURE 8. Side view of clay model with surface profile strips.

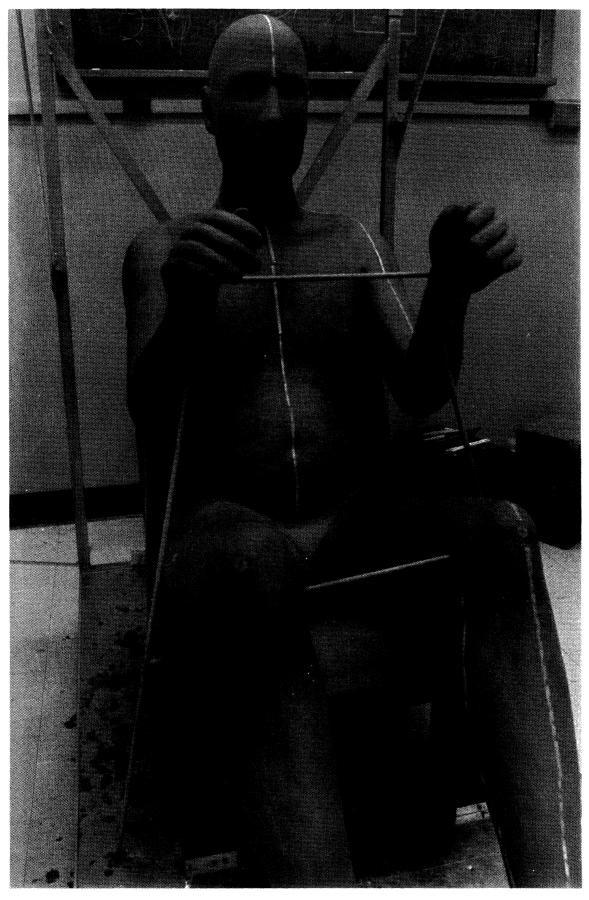


FIGURE 9. Front view of clay model with surface profile strips.

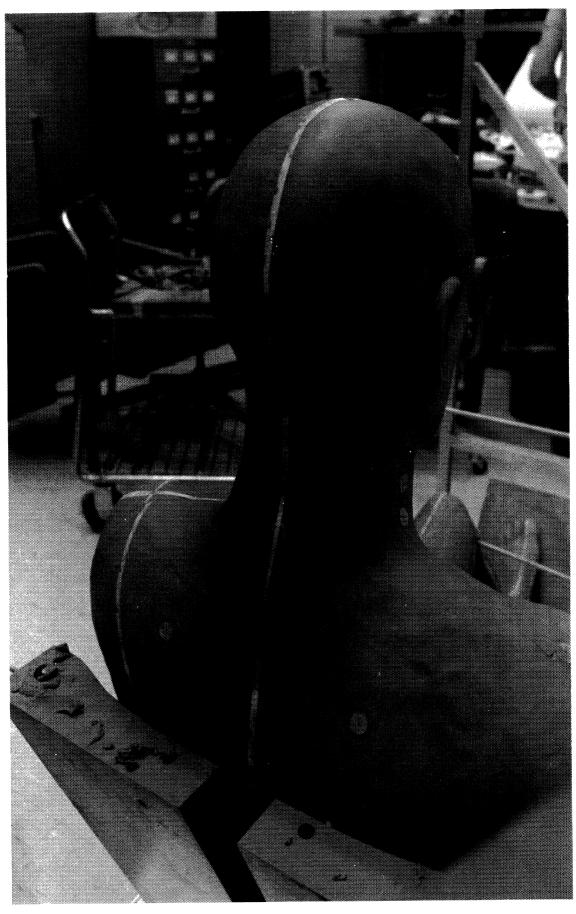


FIGURE 10. Back view of clay model with surface profile strips.

TABLE 9

COORDINATES OF SURFACE POINTS ON CLAY FORM (mm)

Surface Point	X _H	YH	z _H
Body center from crotch up front of body, over head, down back to seat intersection	62 62 54 31 - 31 - 76 - 127 - 139 - 143 - 120 - 144 - 129 - 164 -		5 9 9 1 3 7 0 1 0 1 0 1 0 1 0 1 0 1 0 1 0 1 0 1 0

TABLE 9
COORDINATES OF SURFACE POINTS ON CLAY FORM (Continued)

Surface Point	Х _Н	YH	z _H
Line from posterior scye up back, over shoulder, and down top of arm to hand	-297 -292 -275 -262 -240 -224 -209 -190 -160 -126 - 84 - 27 31 37 69 110 133 163 201 219 228 237 254 274	112 131 141 146 156 161 168 176 188 195 204 205 200 194 188 175 164 156 141 132 124	336 392 419 449 449 449 432 405 327 274 308 317 328 341 346 468
Line from top of head to lateral point on shoulder	-185 -182 -178 -175 -174 -175 -182 -192 -204 -208 -213 -215 -213 -216 -196	0 29 57 74 79 74 69 57 61 71 116 170 202 222 231	735 730 711 679 642 588 552 524 491 473 456 447 431 407 378
Line from lateral point on shoulder down outside of arm to ulnar styloid process	-154 - 97 - 42 33 66	236 235 236 241 244 232	352 313 272 223 245 284

TABLE 9
COORDINATES OF SURFACE POINTS ON CLAY FORM (Continued)

Surface Point	хн	Y _H	Z _H
Line from lateral point on shoulder down outside of arm to ulnar styloid process (Continued)	152 188 207 222	211 197 191 191	321 354 373 388
Line down side of torso from posterior scye to seat surface	-217 -190 -166 -144 -120 - 98 - 82 - 64 - 47 - 36 - 26	189 179 169 157 169 162 157 182 196 198	294 250 204 164 119 81 54 23 - 5 - 22 - 37
Outside of left leg from hip to little toe	- 31 36 133 237 322 379 405 429 469 511 553 590 627 655 694 719 752 784	200 204 204 206 200 194 188 186 187 180 168 148 131 122 129 149 171	- 21 33 70 97 113 129 94 45 - 7 - 89 -122 -149 -185 -210 -165 -123 - 98
Jnderside of leg from seat front to heel	311 360 403 417 453 512 566 617 650 667	129 129 138 134 123 113 100 93 91	- 1 31 57 25 - 45 - 93 -126 -162 -205 -229

TABLE 9
COORDINATES OF SURFACE POINTS ON CLAY FORM (Continued)

Surface Point	X _H	YH	z _H
Top of leg from thigh-abdominal junction to tips of second toe (tips of all toes included)	18 63 167 244 318 412 449 478 572 641 676 701 729 764 801 840 843 827 814	123 125 134 132 145 151 151 146 139 116 102 103 108 117 129 150 164 172	79 88 116 140 162 190 170 127 82 0 - 79 -107 -114 -109 - 89 - 68 - 36 - 42 - 59 - 76 - 92
Inside of leg from crotch to metatarsal/phalangeal	190 235 293 355 395 424 445 467 490 518 579 640 673 713 703 736 777 796 823 840	30 48 64 75 85 91 89 82 77 76 80 74 67 71 82 87 88 103	16 33 58 95 134 130 92 58 22 - 20 - 72 - 121 - 144 - 175 - 140 - 123 - 95 - 84 - 59 - 44

TABLE 9
COORDINATES OF SURFACE POINTS ON CLAY FORM (Continued)

Surface Point	Х _Н	YH	z _H
Inside of arm from scye to fingers	- 28 14 38 80 117 165 202	151 160 166 153 147 142 138	276 231 205 237 275 336 381
Line on underside of arm from level of scye to wrist	-208 -155 - 99 13 42 94 144 183 222 240 262 281 303	191 194 196 197 199 194 181 175 167 174 184 191	302 283 248 191 182 211 259 309 355 378 385 398 409

8.2 Volume and Mass Properties

To compute the segment volumes, the regression equations given in McConville et al. (1980) were used. The following list indicates which anthropometric variables were included for each segment:

Segment	Variables
Head	Head circumference and length
Neck	Subject weight, neck circumference and breadth
Thorax	Subject weight, chest circumference, thorax length
Abdomen	Subject weight, abdomen length, waist circumference
Pelvis	Buttock circumference, suprailiac skinfold
Upper Arms	Subject weight, biceps circumference flexed, Acromion-radiale length
Lower Arms	Subject weight, elbow breadth,
(with Hands)	Mid-forearm circumference
Upper Legs	Subject weight, mid-thigh circumference, stature
Lower Legs	Stature, weight
Feet	Ankle circumference, stature, sphyrion height

The predicted volumes and the sum of volumes for the whole body are given in the first column of Table 10. The values obtained from the left and right sides of the body have been averaged. These volume calculations are based on a density assumption of 1.0 g/cm^3 . Using this value for density, the resulting body weight would be 176.9 pounds, an overestimate of about 4.6 percent. Because of this apparent overestimation of volume, a correction factor was developed as follows:

Volume Correction Factor =
$$\frac{\text{Average Subject Mass}}{\text{Initial Prediction}} = 0.954$$

Scaled volumes and estimated masses are given in the final two columns of Table 10.

It should be noted that an overestimation of volume was expected and is a subject of continuing investigation by the McConville et al. team as indicated in their report. The correction factor is similar to their 5 percent figure. Also, it should be noted that the human body does not have a constant density within each segment. For example, if a value of less than 1.0 is used for the thorax as has been suggested by Dempster (1955a), the necessary correction can be reduced considerably.

TABLE 10
ESTIMATED SEGMENT MASS AND VOLUME

Segment	Predicted Volume (cm ³)	Scaled Volume (cm ³)	Estimated Mass (gm)
Head Neck Thorax Abdomen Pelvis Right Upper Arm Left Upper Arm Right Lower Arm with Hand Left Lower Arm with Hand Right Upper Leg Left Upper Leg Right Lower Leg Left Lower Leg Left Lower Leg Right Foot Left Foot	4,337 1,012 24,909 2,479 11,964 1,854 1,854 2,120 2,120 9,029 9,029 3,760 3,760 1,028 1,028	4,137 965 23,763 2,365 11,414 1,769 1,769 2,022 2,022 8,614 8,614 3,587 3,587 981 981	4,137 965 23,763 2,365 11,414 1,769 1,769 2,022 2,022 8,614 8,614 3,587 3,587 981 981
TOTAL	80,254	76,562	76,562

Using his value of 0.92, thorax mass predicted from the regression equation is 22916 gm. This reduces thorax weight (predicted using density=1.0 gm/cm³) from 54.9 pounds to 50.5 pounds. Using this adjusted thorax value in computing total body weight, the correction factor is reduced to 2.1 percent. Clearly a considerable amount of work is required before final mass and inertial data can be recommended with confidence.

8.3 <u>Centers of Gravity in Hip Point</u> <u>and Segment Coordinate Systems</u>

McConville et al. (1980) give data on center of volume for the various segments of the body. The assumption is made for the current project that center of mass and center of volume are coincident. It is known that this assumption is not completely correct because of density variations within segments. Clauser et al. (1969) note that mid-volume of limb segments are proximal to centers of mass. The differences.

however, are small and believed to be insignificant in comparison with other possible errors. The greatest of these is the mobility of soft tissues with respect to the bony skeleton as the body moves either voluntarily or especially under impact loading. For the current static case of seated posture, and for applications where the assumption of an articulated linkage of rigid masses is valid, the forestated assumption is believed to be adequate. However, if these data are to be used for dynamic applications where there is loose coupling between soft tissue and bony skeleton, the assumption should be rejected and substitute data gathered. To the knowledge of the present author, there are no substantive published data available to address this issue for automotive applications.

Table 11 gives the location of estimated centers of gravity with respect to the whole-body coordinate system. These were derived from the data in Table 12, which locate the points in segment coordinates through the use of the transformations presented in Section 7 of this report. Average values are shown for the left and right sides of the body.

It should be noted that the head center-of-gravity is given with respect to the UMTRI definition of the origin. The placement is thus in front of, and above, the origin as discussed in detail in Section 7.1.

In the case of the neck, the center of mass is a few millimeters in front of a line connecting the estimated head/neck and neck/thorax joints (see Figure 1 and Section 9 for graphics and details of joint locations).

The thorax center-of-gravity lies approximately 40 mm in front of and 20 mm below the reconstructed T8/T9 joint centers. This is a somewhat larger value than that reported by Chandler and Young (1981) in their recent link man analysis. It is believed that the forward migration of soft tissue during the process of sitting down may well account for the shift.

The center of gravity of the abdomen mass is in the center of the mass as projected in the X_H^ZH plane shown in Figure 1. It is located about 2 cm in front of the spinal linkage. If, at a later time,

TABLE 11

LOCATION OF ESTIMATED SEGMENT CENTERS OF GRAVITY
WITH RESPECT TO WHOLE-BODY COORDINATE SYSTEM

Segment	X _H (mm)	Y _H (mm)	Z _H (mm)
Head	-179	0	646
Neck	- 195	0	515
Thorax	-177	0	267
Abdomen	- 85	0	110
Pelvis	- 74	0	17
Upper Arms	- 80	±191*	319
Lower Arms with Hands	149	±174	320
Upper Legs	200	±131	64
Lower Legs	504	±125	- 5
Feet	763	±110	-164

*The positive sign on $\boldsymbol{Y}_{\boldsymbol{H}}$ refers to the left side of the body.

TABLE 12

LOCATION OF ESTIMATED SEGMENT CENTERS OF GRAVITY WITH RESPECT
TO THE INDIVIDUAL SEGMENT COORDINATE SYSTEMS*

Segment	X _A (mm)	Y _A (mm)	Z _A (mm)
Head Neck Thorax Abdomen Pelvis Upper Arm (R) Upper Arm (L) Lower Arm with Hand (R) Lower Arm with Hand (L) Upper Leg (R) Upper Leg (R) Upper Leg (R) Lower Leg (R) Lower Leg (L) Foot (R) Foot (L)	8.4 57.2 58. - 4. -81.8 16.5 16.5 -10. -10. 6. 6. -11.9 -76.9 -76.9	0. 0. 0. 0. 30. -30. 35. -35. 66. -66. -57. 57. - 0.6	31. 49.8 190. - 24.2 10.7 -172. -166. -166. -200. -200. -149. -149. - 6.2 - 6.2

*Recall that there is a different (X_A , Y_A , Z_A) system for each segment.

the abdomen segmentation plane proposed earlier in this report is used, the center of gravity will be shifted even further toward the front of the body. This mass element is believed to be very mobile and loosely coupled to the remainder of the body linkage system.

For the pelvis, the center of gravity is nearly on the line of the spinal column projected into the pelvic region. It lies approximately 2 cm below the L5/S1 joint and 75 mm behind and 17 mm above the hip pivot point. It is not surprising that this mass is far toward the back in that the soft tissue surrounding the head of the femur has been attached to the upper leg segments.

The values for the upper arms, lower arms including hands, upper legs, lower legs, and feet are averaged for the right and left sides of the body. The centers of gravity for the lower arms and upper legs lie virtually on the line connecting the proximal and distal joint centers. The center of gravity of the upper arm lies above the similar line while for the lower leg the center of gravity is below it. This probably reflects the location of major muscle masses (biceps brachii and triceps surae).

8.4 <u>Inertial Properties and Principal Axes</u>

To compute the segment principal moments of inertia, the regression equations given in McConville et al. (1980) were used. These equations predict each of the three principal moments of inertia (I_x , I_y , I_z) for each segment as a linear function of anthropometric variables. Table 13 lists the anthropometric variables used in computing each quantity. The predicted segment inertial properties are given in the first three columns of Table 14. Values from the left and right sides of the body have been averaged. The principal axes (X_p , Y_p , Z_p) for each segment have their origin at the center of gravity (assumed to be coincident with the center of volume). The orientation of these axes is dependent on the geometric form of each individual segment and represents yet another group of coordinate systems.

It appears that the magnitudes of both volume and inertial properties are overestimated by the McConville et al. formulae. In a simplistic sense, the overall composition of a moment of inertia is the

TABLE 13

ANTHROPOMETRIC VARIABLES USED IN PRINCIPAL MOMENT OF INERTIA REGRESSION EQUATIONS

Segment	Moment	Anthropometric Variables
Head	I X I Y I Z	Head circumference, head breadth Head circumference Head circumference, head length
Neck	I X I Y I Z	Neck breadth, neck length Weight, neck circumference, neck breadth Weight, neck circumference, neck breadth
Thorax	I X I Y I Z	Weight, thorax length, chest breadth Weight, stature, thorax length Weight, chest circumference, thorax length
Abdomen	X	Abdomen length, waist circumference, suprailiac skinfold 10th rib circumference, abdomen length, suprailiac skinfold Waist circumference, abdomen length, suprailiac skinfold
Pelvis	I X	Buttock circumference, suprailiac skinfold, buttock depth Buttock depth Buttock depth, weight, suprailiac skinfold
Upper Arms	l X	Weight, acromion-radiale length, biceps circumference (flexed) Weight, triceps skinfold, axilla arm depth Biceps circumference (flexed), axilla arm circumference, acromion-radiale length
Lower Arms (with hands)	I X I Y I Z	Forearm-hand length, wrist and hand circumferences Forearm-hand length, wrist and hand circumferences Elbow and mid-forearm circumferences, weight
Upper Legs	X I Y I Z	Weight, mid-thigh circumference, thigh length Stature, mid-thigh circumference, thigh length Weight, mid-thigh and upper-thigh circumferences
Lower Legs	I X I Y I Z	Stature, calf depth, ankle circumference Stature, calf depth, ankle circumference Weight, calf length, calf circumference
Feet	X X Y Z	Ankle circumference, sphyrion height, stature Foot length, sphyrion height, ankle circumference Foot length, ankle circumference, sphyrion height

TABLE 14

ESTIMATED SEGMENT PINCIPAL MOMENTS OF INERTIA

Coment	Predicted (gm cm ²)			Scaled (gm cm ²)		n ²)
Segment	I X	I _Y	l Z	I _X	Ι _Υ	l _Z
Abdomen Pelvis Up. Arm (L) Up. Arm (R) Low. Arm & Hand (L) Low. Arm & Hand (R) Up. Leg (L)	206,678 15,271 4,712,487 172,973 1,048,233 116,065 116,065 320,711 320,711	109,969 972,524 126,446 126,446 319,145 319,145 1,343,179 1,343,179 545,245 545,245	149,176 23,643 3,112,360 262,991 1,222,598 23,854 23,854 20,793 20,793 378,863 378,863 62,629 62,629	200,271 14,798 4,566,400 167,611 1,015,738 112,467 112,467 310,769 310,769 1,230,899 1,230,899 520,397 520,397	221,546 18,463 3,222,558 106,560 942,376 122,526 122,526 309,252 309,252 1,301,540 1,301,540 528,342 528,342	144,552 22,910 3,015,877 254,838 1,184,697 23,115 23,115 20,148 20,148 367,118 367,118 60,688 60,688

summation of infinitesimal mass elements times the square of their distances from an axis about which the moment is computed. Therefore, if the volume is reduced, the representative distances from the axis are also reduced. Volume can be visualized as a third order function of distances while inertial moments are second order. A scale factor has been developed based on the 0.954 reduction factor for volume used in Section 8.2 as follows:

Volume (UMTRI) =
$$0.954V \sim (0.9844l^3)$$

Scale Factor = $(0.9844)^2 = 0.969$

This factor has been used in the computation of scaled segment inertial properties given in the last three columns of Table 14. In that McConville et al. show some evidence that their predicted inertial properties have larger magnitudes than those proposed by other investigators, it is felt that a small correction factor is justified. The one proposed may be too conservative as the mass on the periphery of an object has a greater effect on moment of inertia than mass near the center of gravity.

The principal axes of inertia for each segment have been computed by McConville et al. with respect to the respective segment anatomical coordinate system. For the present application, it has been necessary to alter the transformation matrices slightly to reflect body symmetry. In the case of body segments such as head, neck, thorax, abdomen, and pelvis, this meant setting small direction angles between the Y-principal axis and the Y-segment axis to zero and adjusting the remainder of the transformation slightly to maintain orthogonality. A typical example is the head. The transformations given by McConville et al. in degrees are:

$$\begin{bmatrix} X_A & Y_A & Z_A \\ X_P & 36.13 & 86.95 & 54.04 \\ Y_P & 93.75 & 3.75 & 90.02 \\ Z_P & 125.88 & 92.19 & 35.96 \end{bmatrix}$$

For symmetry this has been simplified to:

$$\begin{array}{c|ccccc}
 & X_A & Y_A & Z_A \\
X_P & 36 & 90 & 54 \\
Y_P & 90 & 0 & 90 \\
Z_P & 125 & 90 & 36
\end{array}$$

The quantities (X_A, Y_A, Z_A) refer to anatomical coordinates while (X_P, Y_P, Z_P) refer to principal axes.

In the case of body regions, such as upper and lower arms and legs as well as feet, it was necessary to develop an average set of axes for the two sides, then to make it symmetric. A typical case of this is for the feet. The transformations for the left and right feet were given as:

	Ē	Right Foo	<u>ot</u>		<u>!</u>	_eft_Foo	<u>t</u>	
		YA				YA	7	_
X P Y P Z P	9.85 95.18 98.35	85.95 8.76 97.75	81.04 82.95 11.14	X _P Y _P Z _P	8.97 87.21 98.52	92.17 4.83 85.69	81.30 93.94 9.56	

They have been simplified, averaged, and made symmetric yielding:

	<u>R</u>	ight Foo	<u>it</u>		<u>L</u>	eft Foot	•	
	XA	YA	ZA		XA	YA	z _A	_
X _P Y _P Z _P	10 94 99	86 7 95	81 85 10	X _P Y _P Z _P	10 86 99	94 7 85	81 95 10	

Problems with the McConville et al. data were identified for the right thigh and left forearm (with hand). These were confirmed (Kaleps 1982) as incorrect signs in coordinate system definitions. In cases where the symmetry appeared to be marginal between the two sides of the body, it was verified that the transformation matrix degenerates when two of the moments of inertia become the same.

The final results are given in Tables 15 through 18. Tables 15 and 16 give the principal axes of inertia with respect to anatomical axes expressed both in degrees and as cosines. Tables 17 and 18 give the principal axes with respect to the hip point axis system.

TABLE 15

PRINCIPAL AXES OF INERTIA WITH RESPECT TO ANATOMICAL AXES (Cosine Matrix Expressed in Degrees)

Co	T	T v	V	7
Segment		X _A	YA	ZA
Head	X _P	36.	90.	54.
	Y _P	90.	0.	90.
	Z _P	126.	90.	36.
Neck	X _P	11.	90.	79.
	Y _P	90.	0.	90.
	Z _P	101.	90.	11.
Thorax	X _P	14.5	90.	75.5
	Y _P	90.	0.	90.
	Z _P	104.5	90.	14.5
Abdomen	X _P	2.6	90.	92.2
	Y _P	90.	0.	90.
	Z _P	87.8	90.	2.6
Pelvis	X _P	8.4	90.	81.6
	Y _P	90.	0.	90.
	Z _P	98.4	90.	8.4
Upper Arm (L)	X _P	33.6	56.6	91.1
	Y _P	123.4	34.3	83.
	Z _P	90.	96.1	7.
Upper Arm (R)	X _P	33.6	123.4	91.1
	Y _P	56.6	34.3	96.1
	Z _P	90.	83.	7.
Lower Arm with Hand (L)	X _P	19.5	70.5	90.
	Y _P	109.5	19.5	90.
	Z _P	90.	90.	1.
Lower Arm with Hand (R)	X _P	19.5	109.5	90.
	Y _P	70.5	19.5	90.
	Z _P	90.	90.	1.
Upper Leg (L)	X _P	9.8	80.2	89.8
	Y _P	99.8	9.8	90.9
	Z _P	90.1	89.1	1.1
Upper Leg (R)	X _P	9.8	99.8	89.8
	Y _P	80.2	9.8	90.9
	Z _P	90.1	89.1	1.1

TABLE 15
PRINCIPAL AXES OF INERTIA WITH RESPECT TO ANATOMICAL AXES (Cosine Matrix Expressed in Degrees, Continued)

Segment		X _A	YA	ZA
Lower Leg (L)	X _P	24.	114.	90.
	Y _P	66.	24.	92.
	Z _P	90.	88.	1.
Lower Leg (R)	X _P	24.	66.	90.
	Y _P	114.	24.	88.
	Z _P	90.	92.	1.
Foot (L)	X _P	10.	94.	81.
	Y _P	86.	7.	95.
	Z _P	99.	85.	10.
Foot (R)	X _P	10.	86.	81.
	Y _P	94.	7.	85.
	Z _P	99.	95.	10.

TABLE 16

PRINCIPAL AXES OF INERTIA WITH RESPECT TO ANATOMICAL AXES (Cosine Matrix)

Segment		X _A	YA	z _A
Head	X _P	0.809	0.	0.588
	Y _P	0.	1.	0.
	Z _P	-0.588	0.	0.809
Neck	X _P	0.981	0.	0.192
	Y _P	0.	1.	0.
	Z _P	-0.192	0.	0.981
Thorax	X _P	0.968	0.	0.250
	Y _P	0.	1.	0.
	Z _P	-0.250	0.	0.968
Abdomen	X _P	0.999	0.	-0.038
	Y _P	0.	1.	0.
	Z _P	0.038	0.	0.999
Pelvis	X _P	0.989	0.	0.146
	Y ^P	0.	1.	0.
	Z ^P _P	-0.146	0.	0.989
Upper Arm (L)	X _P	0.829	0.545	-0.0175
	Y _P	-0.559	0.829	-0.104
	Z _P	0.	0.122	0.992
Upper Arm (R)	X _P	0.829	-0.559	-0.0175
	Y _P	0.545	0.829	0.122
	Z _P	0.	-0.104	0.992
Lower Arm with Hand (L)	X _P	0.943	0.334	0.
	Y _P	-0.334	0.943	0.
	Z _P	0.	0.	1.
Lower Arm with Hand (R)	X _P	0.943	-0.334	0.
	Y _P	0.334	0.943	0.
	Z _P	0.	0.	1.
Upper Leg (L)	X _P	0.985	0.170	0.00349
	Y _P	-0.170	0.985	-0.0157
	Z _P	-0.00175	0.0157	1.
Upper Leg (R)	X _P	0.985	-0.170	0.00349
	Y _P	0.170	0.985	-0.0157
	Z _P	-0.00175	0.0157	1.

TABLE 16
PRINCIPAL AXES OF INERTIA WITH RESPECT TO ANATOMICAL AXES (Cosine Matrix, Continued)

Segment		XA	YA	z _A
Lower Leg (L)	X _P	0.913	-0.407	0.000
	Y _P	0.407	0.913	-0.0349
	Z _P	0.	0.0349	1.
Lower Leg (R)	X _P	0.913	0.407	0.
	Y _P	-0.407	0.913	0.0349
	Z _P	0.	-0.0349	1.
Foot (L)	X _P	0.985	-0.0698	0.156
	Y _P	0.0698	0.992	-0.0872
	Z _P	-0.156	0.0872	0.985
Foot (R)	X _P Y ^P Z ^P	0.985 -0.0698 -0.156	0.0698 0.992 -0.0872	0.156 0.0872 0.985

PRINCIPAL AXES OF INERTIA WITH RESPECT TO HIP POINT AXIS SYSTEM (Cosine Matrix Expressed in Degrees)

Segment		ХН	YH	z _H
Head	X _P	39.8	90.	50.1
	Y _P	90.	0.	90.
	Z _P	129.9	90.	39.8
Neck	X _P	9.9	90.	99.7
	Y _P	90.	0.	90.
	Z _P	80.3	90.	9.9
Thorax	X _P	22.3	0.	67.7
	Y _P	90.	1.	90.
	Z _P	112.3	0.	22.3
Abdomen	X _P	26.	90.	64.1
	Y _P	90.	0.	90.
	Z _P	115.9	90.	26.
Pelvis	X _P	69.4	90.	20.6
	Y _P	90.	0.	90.
	Z _P	159.4	90.	69.4
Upper Arm (L)	X _P	56.	72.	40.
	Y _P	106.	20.	100.
	Z _P	142.	97.	53.
Upper Arm (R)	X _P	56.	108.	40.
	Y _P	74.	20.	80.
	Z _P	142.	83.	53.
Lower Arm with Hand (L)	X _P	177.	52.	50.
	Y _P	57.	40.	109.
	Z _P	134.	78.	134.
Lower Arm with Hand (R)	X _P	117.	128.	50.
	Y _P	123.	40.	71.
	Z _P	134.	102.	134.
Upper Leg (L)	X _P	110.	74.	26.
	Y _P	83.	16.	104.
	Z _P	159.	89.	111.
Upper Leg (R)	X _P	110.	106.	26.
	Y _P	97.	16.	76.
	Z _P	159.	91.	111.

TABLE 17
PRINCIPAL AXES OF INERTIA WITH RESPECT TO HIP POINT AXIS SYSTEM (Cosine Matrix Expressed in Degrees, Continued)

Segment		Х _Н	Yн	z _H
Lower Leg (L)	X _P	43.	92.	47.
	Y _P	85.	6.	93.
	Z _P	134.	84.	44.
Lower Leg (R)	X _P	43.	88.	47.
	Y _P	95.	6.	87.
	Z _P	134.	96.	44.
Foot (L)	X _P	69.	82.	23.
	Y _P	84.	14.	102.
	Z _P	158.	80.	71.
Foot (R)	X _P	69.	98.	23.
	Y _P	96.	14.	78.
	Z _P	158.	100.	71.

TABLE 18

PRINCIPAL AXES OF INERTIA WITH RESPECT TO HIP POINT AXIS SYSTEM (Cosine Matrix)

Segment		Х _Н	Y _H	z _H
Head	X Y P Z P	0.768 0. -0.641	0. 1. 0.	0.641 0. 0.768
Neck	X _P	0.985	0.	-0.169
	Y _P	0.	1.	0.
	Z _P	0.169	0.	0.985
Thorax	X _P	0.925	0.	0.379
	Y _P	0.	1.	0.
	Z _P	-0.379	0.	0.925
Abdomen	X _P	0.899	0.	0.437
	Y _P	0.	1.	0.
	Z _P	-0.437	0.	0.899
Pelvis	X _P	0.352	0.	0.936
	Y _P	0.	1.	0.
	Z _P	-0.936	0.	0.352
Upper Arm (L)	X _P	0.56	0.3	0.77
	Y _P	-0.28	0.94	-0.17
	Z _P	-0.78	-0.12	0.60
Upper Arm (R)	X _P	0.56	-0.30	0.77
	Y _P	0.28	0.94	0.17
	Z _P	-0.78	0.12	0.60
Lower Arm with Hand (L)	X _P	-0.461	0.61	0.644
	YP	0.551	0.767	-0.332
	Z _P	-0.697	0.201	-0.689
Lower Arm with Hand (R)	X _P	-0.461	-0.61	0.644
	Y _P	-0.551	0.767	0.332
	Z _P	-0.697	-0.201	-0.689
Upper Leg (L)	X _P	-0.342	0.275	0.898
	Y _P	0.130	0.96	-0.245
	Z _p	-0.931	0.0169	-0.364
Upper Leg (R)	X _P	-0.342	-0.275	0.898
	Y _P	-0.130	0.960	0.245
	Z _P	-0.931	-0.0169	-0.364

TABLE 18
PRINCIPAL AXES OF INERTIA WITH RESPECT TO HIP POINT AXIS SYSTEM (Cosine Matrix, Continued)

Segment		Х _Н	Yн	z _H
Lower Leg (L)	X _P	0.727	-0.026	0.685
	Y _P	0.092	0.995	-0.059
	Z _P	-0.691	0.103	0.716
Lower Leg (R)	X _P	0.727	0.026	0.685
	Y _P	-0.092	0.995	0.059
	Z _P	-0.691	-0.103	0.716
Foot (L)	X _P	0.359	0.147	0.922
	Y _P	0.11	0.969	-0.214
	Z _P	-0.93	0.168	0.328
Foot (R)	X _P	0.359	-0.147	0.922
	Y _P	-0.11	0.969	0.214
	Z _P	-0.93	-0.168	0.328



9.0 A MODEL FOR THE LOCATION OF JOINT CENTERS

9.1 Introduction

In order to quantify motions of one segment with respect to its neighbors in a linkage, it is necessary to define the connections between the elements in the linkage. Connections between elements of the bony skeleton are called articulations. If the position of the articulation coincides with a point about which rotations between neighboring bony segments can occur, it is called a center of rotation or joint center.

Joints in the human body most often exhibit more than one degree-of-freedom in describing the motion of one body segment with respect to its neighbors. Some, such as the knee and elbow, can probably be modeled as pins connecting the upper and lower arms and legs. However, it is known that the motions at these joints are more complex and involve a small amount of migration of the joint location within each of the neighboring segments as the body moves (Dempster (1955a). Others, such as the hip, ankle, and glenohumeral joints, are more like ball connections between the two segments.

The shoulder girdle is even more complex in that it is composed of three articulations: the glenohumeral, sternoclavicular, and acromioclavicular articulations. The glenohumeral articulation consists of the humeral head rotating on the glenoid fossa. As there is very little movement of the center of the humeral head with respect to the scapula in normal motion, this articulation can properly be called the glenohumeral joint. The sternoclavicular articulation has many properties of a ball joint while the acromioclavicular articulation combines with the conoid and trapezoid ligaments to form the claviscapular joint system which has been discussed by Dempster (1965). These joints are supplemented by a movable shoulder girdle mass, separate from the thorax, which rides with the scapula. The three joints, combined with the clavicle and scapula mass links, define the mobility of the arm with respect to the torso.

The vertebral column is actually a collection of seven cervical. twelve thoracic, and five lumbar vertebrae. In each articulation between the vertebrae there is the possibility of limited rotation, shear, and stretching. Two concepts have been used in the construction of cervical spines for crash test dummies such as the Hybrid III (Foster et al. 1977) and crash victim computer codes such as the MVMA 2D model (Bowman et al. 1979) and the various versions of the Calspan CVS. In the case of the dummy, the cervical spine is a deformable element connecting head to torso. The model lumps the rotational properties into head/neck and neck/thorax interface joints and uses an extensible neck link between the joints. Both concepts are simplifications of the actual vertebral structure which ignore coupling between the three possible rotational modes at the various articulations (flexion, lateral flexion, and rotation) as has been discussed by Bowman and Robbins (1972), as well as Schneider et al. (1975). This coupling is believed to exist for all lumped joint models of the vertebral column.

The thoracic vertebrae are usually assumed to be immobile with respect to each other in similar dummy and modeling applications. Studies such as the torso link mobility study by Snyder et al. (1972) and the spinal mobility study by Cheng et al. (1979) contradict each other as to the need for upgrading this model. The torso link study, which is a reach study and does not involve dynamic loading, identifies substantial mobility throughout the spine from neck to pelvis. The Wayne State study (Cheng et al. 1979) has gone so far as to suggest a rigid link from the C7/T1 to the lumbar sacral joint for use in a frontal impact dummy. It is clear that considerable work and discussion must take place before the definitive selection of the appropriate number of spinal joints and the linkage between them is resolved.

The lumbar spine is usually considered as a flexible element in dummy hardware. Alternatively, the mobility is concentrated at two joints representing connections to the pelvis and thorax. Data are very limited and incomplete, especially for non-frontal dynamic mobility, regarding both location and compliance for this joint model.

Joint center models for the seated occupant are derived from several sources and presented in the following three subsections. These

cover successively the vertebral column, the shoulder and arm, and finally, the hip, knee, and ankle. A summary of the results is given in Tables 19 and 20.

TABLE 19

LOCATION OF JOINT CENTERS IN WHOLE-BODY COORDINATES

Joint	X _H (mm)	Y _H (mm)	Z _H (mm)
Head/Neck	-196	0	588
C7/T1	-193	0	469
T4/T5	-220	0	397
Т8/Т9	-215	0	287
T12/L1	-177	0	165
L2/L3	-142	0	115
L5/S1	- 89	0	39
Sternoclavicular	-145	± 20	433
Claviscapular	-230	±168	427
Glenohumeral	-186	±173	393
Elbow	36	±208	201
Wrist	228	±158	393
Hip	0	± 82	0
Knee	406	±138	136
Ank l e	684	± 94	-169

TABLE 20

LOCATION OF JOINT CENTERS IN SEGMENT COORDINATES

Joint	Cogmont	Coor	dinates	(mm)
	Segment	XA	YA	ZA
Head/Neck Head/Neck C7/T1 C7/T1 T4/T5 T8/T9 T12/L1 L2/L3 L2/L3 L5/S1 L5/S1 Sternoclavicular (L) Sternoclavicular (R) Claviscapular (R) Glenohumeral (L) Glenohumeral (R)	Head Neck Neck Thorax Thorax Thorax Thorax Abdomen Abdomen Pelvis Thorax	- 13 30 75 70 32 25 47 85 - 39 - 40 - 67 106 106 21 21 60 60	0 0 0 0 0 0 0 0 0 43 - 43 - 168 - 168 - 173 - 173	- 25 117 7 392 338 220 105 38 6 - 87 29 347 354 354 314
Glenohumeral (L) Glenohumeral (R) Elbow (L) Elbow (R) Elbow (R) Elbow (R) Wrist (L) Wrist (R) Hip (L) Hip (R) Hip (R) Knee (L) Knee (R) Knee (R) Ankle (R)	Upper Arm (L) Upper Arm (R) Upper Arm (L) Upper Arm (R) Lower Arm (L) Lower Arm (L) Lower Arm (R) Pelvis Pelvis Upper Leg (L) Upper Leg (R) Upper Leg (R) Lower Leg (L) Lower Leg (R)	12 12 - 6 - 11 - 11 - 7 - 61 - 61 13 13 0 0 12 12	- 33 - 39 - 39 - 35 - 30 - 30 - 82 - 123 - 51 - 48 - 48 - 37 - 37	- 42 - 42 - 337 - 337 - 337 - 5 - 271 - 271 - 62 - 62 - 7 - 418 - 418 - 22 - 393 - 393

9.2 Joint Center Model for the Vertebral Column

A stated goal of the project was to obtain the spatial location for a seated person of the following vertebral joint centers:

Head/Neck	Interface	T12/L1
C7/T1		L2/L3
T4/T5		L5/S1
т8/т9		

This is a considerable reduction in the possible degrees of freedom when all elements of the vertebral column are taken into account, particularly with respect to the neck. However, it does break the spine in sufficiently small segments to fairly accurately define its overall position in space with respect to the remaining skeletal elements of the body such as the head, shoulder girdle, rib cage, and pelvis. Also, there is a reasonable data base available which can be adapted to this task.

The most commonly accepted location for a joint at the head/neck interface is at the occipital condyles. Mertz and Patrick (1971) and Ewing and Thomas (1973) have used this point for presentation of neck torque data. Its location has been given in anatomical coordinates constructed from targets on the superior edge of each auditory meatus and at the infraorbital notches (Ewing and Thomas 1972). Although tragion, as used in the present study, and external auditory meatus are different anatomical entities, and there is bound to be some variation between individuals in shape and exact location of tragus, there probably is no more variation than in taking the measurement itself. So, it will be assumed that the coordinate system of Ewing and Thomas (1972) is coincident with that of the present project. The average distance from origin to occipital condyle point is thus assumed to be $X_{\Lambda} = -11$, $Z_{\Lambda} = -26$, which are averages from Table 3 of the Ewing and Thomas report (1973). In the UMTRI coordinate system based on the hip point, this places the head/neck joint center at:

$$X_{H} = -196, Y_{H} = 0, Z_{H} = 588.$$

The location is graphically displayed in Figure 1.

The Snyder et al. report (1972), dealing with the link system of the human torso, provides the only known source of data which relates external spinal landmarks to vertebral interspaces. As such, it has been used to construct the spinal linkage from the C7/T1 to the lumbar/sacral interface. The seated posture used in the torso link study was most often more erect than that assumed in the automobile seated posture. However, the position of the arm in the current study was about the mid-range for most of those assumed by subjects in the torso link study.

Figure 11 shows the geometric construction of the C7/T1 interface using torso link data. Cervical vector prediction equations were used. These required the availability of C7 and nasion surface markers. The angle of a vector from C7 to glabella with the vertical was entered into the appropriate regression equation to yield the distance from the C7 surface marker to the C7/T1 interspace as well as the angle made by the vector connecting C7 to the C7/T1 interspace (74.7 degrees). The use of glabella instead of nasion resulted in a difference of about one millimeter in the location of the joint center.

Similarly, thoracic vector prediction equations were used in estimating the T4/T5, T8/T9, and T12/L1 interfaces. These required the availability of T4 and T12 surface markers. The angle between a line connecting these two points and a vertical line serves as the reference angle for use in the regression equations. These equations are then used to predict the following:

- Distance from T4 to T4/T5 interspace
- Vector direction from T4 to T4/T5 interspace
- Distance from T8 to T8/T9 interspace
- Vector Direction from T8 to T8/T9 interspace
- Distance from T12 to T12/L1 interspace
- Vector direction from Tl2 to Tl2/Ll interspace

The reconstruction is shown in Figure 12.

Even though the regression equations in the torso link study had no obvious data available for defining a reference angle in the lumbar region of the back (interior landmarks were required) several techniques using the L2 and L5 surface targets were attempted. The techniques involved backwards solution of the regression equations for the interior reference angle using surface target coordinates to develop the input. The solution of each equation led to a different value for the interior

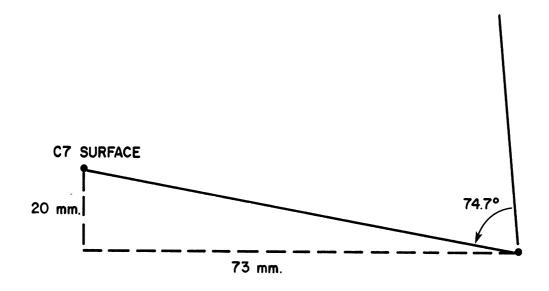


FIGURE 11. Construction of C7/T1 joint.

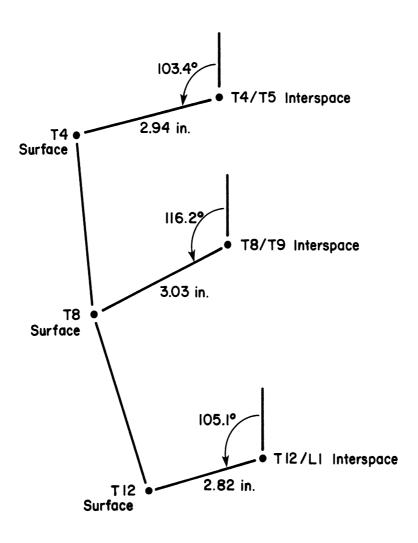


FIGURE 12. Construction of thoracic joints.

angle. When these values were used for frontwards solution and prediction, a similar variety of interspace locations were predicted. These estimations for the L2/L3 and L5/S1 interspace locations were clustered in a circle with a radius of about 5 mm for the L5/S1 interface and about 7 mm for the L2/L3 interface. It was also noted that the lateral point on the first sacral vertebral body, determined from the Reynolds et al. (1981) data and discussed in Section 3, was within the circle for L5/S1 predictions. Because of this, a simpler procedure has been adopted which yields interface points within these circles. As a first step, the lateral point on the first sacral vertebral body was chosen to represent the connection of the vertebral column to the pelvis (or L5/S1 joint). As a second step, a straight line was constructed from this point to the predicted T12/L1 interface. The assumption was then made that the thicknesses of the lumbar vertebral bodies are similar. This led to the approximation that the L2/L3 interface is 60 percent of the way from the pelvis to the T12/LT interface. The point defined by this construction lies within the circle of estimates discussed above. The results of this reconstruction are shown in Figure 13.

9.3 Joint Centers in the Shoulder and Arm

The shoulder girdle is the structure which connects the arms to the remainder of the bony skeleton. This structure, often represented by a simple ball joint in crash test dummies, actually consists of three independent joints and two bony links. The joints are the:

- Sternoclavicular joint where the clavicle meets the sternum
- Claviscapular joint which models the complex connection of the scapula to the clavicle (Dempster 1965)
- 3. Glenohumeral joint where the humerus interacts with the scapula at the glenoid fossa

The bony links can be modeled as:

- 1. The clavicle from the sternoclavicular to the claviscapular joint
- 2. The scapula from the claviscapular to the glenohumeral joint

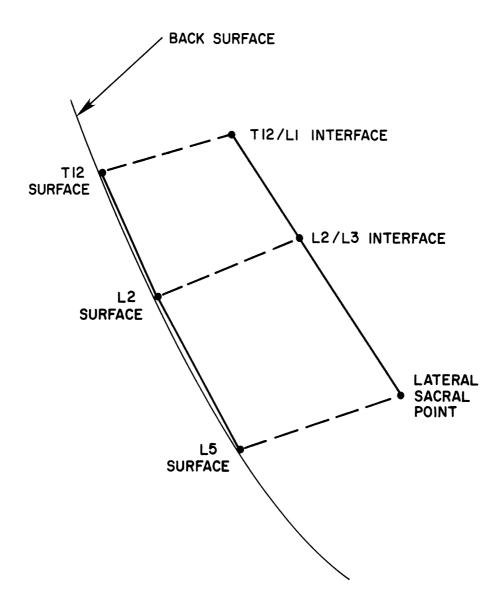


FIGURE 13. Construction of lumbar joints.

Figure 14 illustrates the location of the various elements in the shoulder girdle complex. Instead of a direct connection of the humerus to the thoracic skeleton, then, shoulder mobility should take into account this more complex linkage. Dempster (1965, 1955a, 1955b) has discussed this in detail and demonstrates differences in upper arm mobility when one or more of the joints are locked up. Figure 15 shows a superposition of three profiles of the maximum excursion curves traversed by the elbow if: (1) only the glenohumeral joint is free; (2) the glenohumeral and claviscapular joints are free; and (3) all three are free.

In the first case it should be noted that there does not appear to be much of a change in the center of rotation. Reuleaux analysis shows the center staying within the head of the humerus (Dempster 1955b); hence the center of the head of the humerus will now be called the glenohumeral joint. In the second case, it does not appear that there is much rotation or motion of the scapula with respect to the end of the clavicle. However, the rather small rotation of the free scapula allows large changes in the possible motions of the humerus. In the third case, the glenohumeral joint center (as well as the scapula and claviscapular joint) can undergo large motions with respect to the thorax as the clavicle rotates at its articulation with the sternum.

Dempster (1955a) has defined the sternoclavicular joint center as the "midpoint position of the palpable junction between the proximal end of the clavicle and the sternum at the upper border (jugular notch) of the sternum." It is estimated that this point is one centimeter below the clavicale surface landmark and 2 centimeters lateral from the body centerline. The laboratory coordinates of the sternoclavicular joint are thus:

$$X_{H} = -145, Y_{H} = \pm 20, Z_{H} = 433$$

The claviscapular joint center was defined as "the midpoint of a line between the coracoid tuberosity of the clavicle (at the posterior border of the bone) and the acromio-clavicular articulation (or the tubercle) at the lateral end of the clavicle; the point, however, should be visualized as on the underside of the clavicle." On the basis of

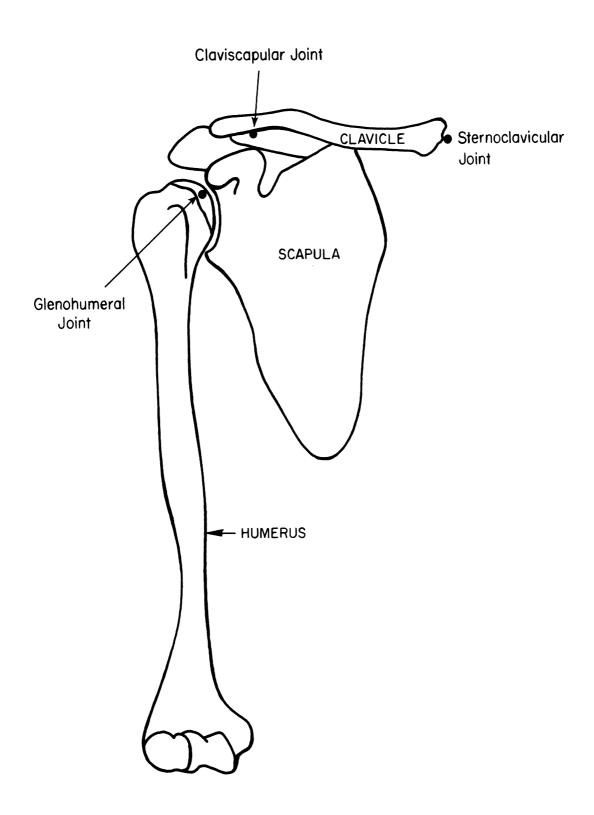
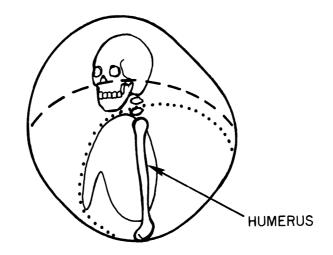


FIGURE 14. The three joints of the shoulder girdle.



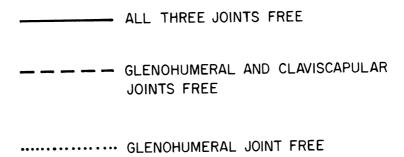


FIGURE 15. Range of motion at shoulder joint as a function of degrees of freedom.

measurements on skeletal material, it is estimated that the shift from the acromio-clavicular articulation surface landmark point is:

Y = 2.75/2 cm toward the center of the body X = 1.5 cm toward the rear of the body

Z' = 1 cm down

The estimated location of the claviscapular joint center is thus:

$$X_{H} = -230, Y_{H} = \pm 168, Z_{H} = 427$$

The glenohumeral joint center is defined by Dempster (1955a) as the "midregion of the palpable bony mass of the head and tuberosities of the humerus, ..." The remainder of the definition prescribed an arm position in which to make a measurement which was not adaptable to presentation into precise three-dimensional coordinates. Three surface landmarks used during the present project define the location in space of the humerus with the assumption that the tissue depths are correct. These landmarks are:

Greater tubercle of the humerus Lateral humeral epicondyle Medial humeral epicondyle

A humerus with a 50th percentile length was set up in a three-dimensional measurement frame so that its coordinate system was parallel to the laboratory frame and so that the three skeletal landmarks were in locations prescribed in Table 4. The head of the humerus was modeled as a sphere so that the center could be determined from points on the surface. This construction yielded a glenohumeral joint center of:

$$X_{H} = -186, Y_{H} = \pm 173, Z_{H} = 393$$

There was not sufficient time remaining in the project to complete a comparison of the shoulder girdle reconstruction based on these direct applications of Dempster with a reconstruction using the definitions and formula of the torso link study.

Dempster has defined the elbow joint to be the "midpoint of a line between (1) the lower palpable point of the medial epicondyle of the humerus, and (2) a point 8 mm above the radiale (radio-humeral

junction)." The two bony landmarks available from the present project which were used in this reconstruction were the radiale and the medial humeral epicondyle. The 8-mm point was chosen to be along an extension of the lower arm defined simply as a line from the ulnar styloid to the radiale. This resulted in a shift of the radiale point of X_H =-6, Z_H =-6 to form the point required under item (2). The elbow joint center was thus determined from the two points as:

$$X_{H} = 36, Y_{H} = \pm 208, Z_{H} = 201$$

The wrist joint has been added to the list of joints required in order to define a long axis of the forearm based on joint centers. Dempster's definition is that the joint is "on the palmar side of the hand, the distal wrist crease at the palmaris longus tendon, or the midpoint of a line between the radial styloid and the center of the pisiform bone; on the dorsal side of the hand, the palpable groove between the lunate and capitale bones, on a line with metacarpal bone III." It was estimated that for the UMTRI seated subjects the pisiform bone is approximately 20 mm distal in the X_H coordinate to the ulnar styloid, or can be approximated on the surface by the "pisiform surface location:"

$$X_{H} = 246, Y_{H} = 191, Z_{H} = 387$$

An additional shift of $Y_H = -10$ is estimated to reach the pisiform bone centers which would be:

$$X_{H} = 246, Y_{H} = 181, Z_{H} = 387$$

The wrist joint center can now be approximated by the center of a line connecting this point with the stylion as:

$$X_{H} = 228, Y_{H} = 158, Z_{H} = 393$$

9.4 Joint Centers in Hip, Knee, and Ankle

The hip joint centers have been discussed in detail in Section 3. The center of the line connecting these points is used as the origin of the standard seat coordinate system. They have been developed based on symphysion and anterior-superior iliac spine surface landmarks in conjunction with the pelvic reconstruction of Reynolds et al. (1981).

Based on Dempster and Frankel et al. (1971) it is estimated that knee joint center can be approximated by the center of a line connecting the lateral and medial femoral epicondyles. The axis of the pin joint will be on a line perpendicular to the plane formed by the lines connecting joint centers in the upper and lower legs. The center of the line, which is based on two available surface landmarks, is:

$$X_{H} = 406, Y_{H} = \pm 138, Z_{H} = 136$$

The ankle joint center has been defined by Dempster to be on the "level of a line between the tip of the lateral malleolus of the fibula and a point 5 mm distal to the tibial malleolus. The distal translation is further down the leg from the sphyrion which involves both X_H and Z_H translations for the seated occupant of $X_H = 3$, $Z_H = -4$. So the ankle joint center is at the center of the line connecting the shifted sphyrion landmark with the lateral malleolus of the fibula which was also measured in the current project. Its coordinates are:

$$X_{H} = 684, Y_{H} = 94, Z_{H} = -169$$

10.0 JOINT PARAMETERS

10.1 Introduction

There are two basic types of parameters which should be considered in the development of joint parameters. The first of these is an identification of the normal range of mobility between different segments of the body. The second is the resistance to motion when one segment of the body moves with respect to its neighbors.

The normal range of mobility of the body is usually described as joint range of motion data. The most commonly used sources are Dempster (1955a), Barter et al. (1957), and Glanville and Kreezer (1937). References with particularly extensive data on neck mobility have been prepared by Ferlic (1962) and Snyder et al. (1975a, 1975b). Thoracic and lumbar spine mobility data have been reported by Nyquist and Murton (1975) as well as Mital et al. (1978, 1979) and Krieger (1976). The Mital work at Wayne State University is part of activity under Department of Transportation Contract No. DOT-HS-5-01232. The thoracic and lumbar range of motion data in the coronal plane and about the vertebral axes, which have been gathered under that contract, are in draft report form. Additional extensive range-of-motion data on head/neck flexion, extension, lateral flexion, rotation, and combined modes are expected in the near future from the Naval Aeromedical Research Laboratory in New Orleans.

Data on resistance to motion is very much more difficult to find, interpret, and assemble into a form usable in dummy design work. The most directly applicable data have been reported for the:

- Neck by Mertz and Patrick (1971), Snyder et al. (1975a, 1975b), and Robbins et al. (1974)
- Head/trunk, waist, hip, knee, shoulder, elbow by Krieger (1976)
- Lower spine by Nyquist and Murton (1975) and Mital et al. (1978, 1979)
- Shoulder, arms, and legs by Engin (1979, 1980, 1981), Engin and Kaleps (1980), and Engin and Kazarian (1981)

The final two subsections of the report cover the two basic issues just sketched out--range of motion at joint structures and resistance to motion at joint structures.

10.2 Range of Motion at Joint Structures

Dempster (1955a) has gathered the most comprehensive set of range of voluntary motion data. These were reanalyzed, graphically illustrated, and reported in an easier to understand format by Barter et al. (1957). Dempster did not report range-of-motion data for the spinal column or abductions in the coronal plane for the shoulder. Traditional data on the neck and shoulder are available from Glanville and Kreezer (1937) while more recent data of Snyder et al. (1975a, 1975b) supplement the neck information. Available thoracic and lumbar spine mobility are limited to flexion studies by Nyquist and Murton (1975) and Mital et al. (1978, 1979).

Table 21 is a summary of range-of-motion data with the source indicated. The various measures are illustrated in Figure 16. The coronal plane corresponds to a $Y_H Z_H$ plane for a standing person while the transverse plane is an $X_H Y_H$ plane. The sagittal plane $(X_H Z_H)$ is the plane of flexion and extension.

10.3 Resistance to Motion at Joint Structures

For the neck, the corridor proposed by Mertz and Patrick (1971) is the best available description of neck resistance to motion in flexion and extension. These data, illustrated in Figure 17, are already in use in dummy construction and give values of torque at the occipital condyles versus head rotation angle relative to the torso.

In the case of lateral flexion, the only known data are derived from the lateral hyperflexion injury study at UMTRI (Snyder et al. 1975b). Using head jerk test data, a computer simulation was used to estimate spring rates of about 16 in. lb/degree of lateral flexion for small motions. Figure 18 shows a hypothesized form for resistance to lateral flexion. The dotted line represents stiffening at the end of the voluntary motion range.

No data are known to be available for neck rotation. However, some are anticipated based on analyses currently being conducted on NAMRL data.

All data known to the present author for the vertebral column have been gathered by Nyquist and Murton (1975), Mital et al. (1978, 1979), and Krieger (1976). The slope of the Krieger data appear to fall within the bounds set by Nyquist and Murton. A simple version of the Krieger data, with increased stiffness at the end of the range of motion is shown in Figure 19. Lateral flexion and rotation about the axis of the spinal column are not yet available but should appear in the near future under DOT contract No. DOT-HS-5-01232.

Engin (1980) provides a considerable body of information on the overall resistance of the shoulder complex to rotation. Not only are extension and flexion in the sagittal plane given but also the rotation about the long axis of the humerus. Figure 20 illustrates part of Engin's information. The data shown give only the maximum moment curve at the joint. Engin has developed the complete three-dimensional moment vector. Further information on the force resistance to shrugging motions is also presented (Engin 1981).

Krieger has provided some limited information on the elbow. Figure 21 is a simple model for the untensed elbow with a stiffness at the fully flexed position less than that for the extended position. Engin (1979) and Engin and Kaleps (1980) also provided torque/angle information on pronation and supination of the hand at the wrist.

Hip flexion and extension data have been developed by both Nyquist and Murton (1975) and Krieger (1976). As is the case with the spinal data, Nyquist and Murton report very different results for the cases of relaxed or tensed subjects. Further they suggest that: "A decision should be made with regard to dummy design philosophy. Should the dummy respond as a relaxed or as a tensed human, or perhaps in accordance with some intermediate criteria?" An idealized version of Krieger's data is shown in Figure 22. Data on resistance to rotation about the long axis of both the femur and tibia are available based on the work of Engin (1979) and Engin and Kaleps (1980).

Data on torque at the knee are available from a variety of sources including Krieger (1976) and Robbins et al. (1971). An idealization of Krieger's data is included as Figure 23. A part of a study of human volunteer sled test subjects involved a measurement of the amount of knee tensing which is possible. A maximum value of 5040 in.lb. was measured which is the equivalent of 20 Gs of joint strength. This emphasizes the comment of Nyquist and Murton made in the previous paragraph.

In summary, a variety of data are available which raises some hope that it may be possible to make estimates for joint ranges of motion and resistance to such motions. Questions must be answered as to whether to define a range of performance based on free-moving or tensed joints. Some data gaps must be filled and the results of the various investigators pulled together in a consistent format.

TABLE 21

RANGE-OF-MOTION DATA

Quantity	Value (deg)	Reference
Head Ventral flexion Dorsal flexion (hyperextension) Lateral Flexion Rotation	55 (60) 49 (61) 35 (41) 67 (74)	Snyder et al. (1975a,b) (Glanville & Kreezer 1937)
Vertebral Column Rotation of Tl with respect to Tl2 (flexion)	15	Mital et al. (1979)
Rotation of T12 with respect to pelvis (flexion)	16	Mital et al. (1979)
Rotation of T1 with respect to T12	20	Mital et al. (1979)
(extension) Rotation of T12 with respect to	7	Mital et al. (1979)
pelvis (extension) Lateral flexion Rotation about long axis	42 ? ±45 ?	Robbins et al. (1971) (Con. No. DOT-HS-5-01232)
Shoulder (Three Links) Flexion (sagittal plane) Extension (sagittal plane) Abduction (coronal plane) Abduction (transverse plane) Adduction (transverse plane)	188 61 129 134 48	Dempster (1955a) Dempster (1955a) Glanville & Kreezer (1937) Dempster (1955a) Dempster (1955a)
Shoulder (Clavicle Link) Protraction (transverse plane) Retraction (transverse plane) Depressed (coronal plane) Shrugged (coronal plane)	15 20 8 36	(Derived from Dempster 1955a)
Elbow Extension Flexion	0 142	Dempster (1955a) Dempster (1955a)
<u>Hip</u> Flexion	113 (168)	Dempster (1955a)
Abduction (transverse plane) Adduction (transverse plane) Abduction (coronal plane) Medial rotation (prone) Lateral rotation (prone) Medial rotation (sitting) Lateral rotation (sitting)	53 31 70 39 34 31 30	(Glanville & Kreezer 1937) Dempster (1955a) Dempster (1955a) Glanville & Kreezer (1937) Dempster (1955a) Dempster (1955a) Dempster (1955a) Dempster (1955a) Dempster (1955a)

TABLE 21
RANGE OF MOTION DATA (Continued)

Quantity	Value (deg)	Reference
Knee Voluntary flexion (prone) Forced flexion Forced flexion (kneeling) Medial rotation Lateral rotation	125 144 159 35 43	Dempster (1955a) Dempster (1955a) Dempster (1955a) Dempster (1955a) Dempster (1955a)
Ankle Dorsiflexion Plantar flexion Inversion Eversion	35 38 24 23	Dempster (1955a) Dempster (1955a) Dempster (1955a) Dempster (1955a)

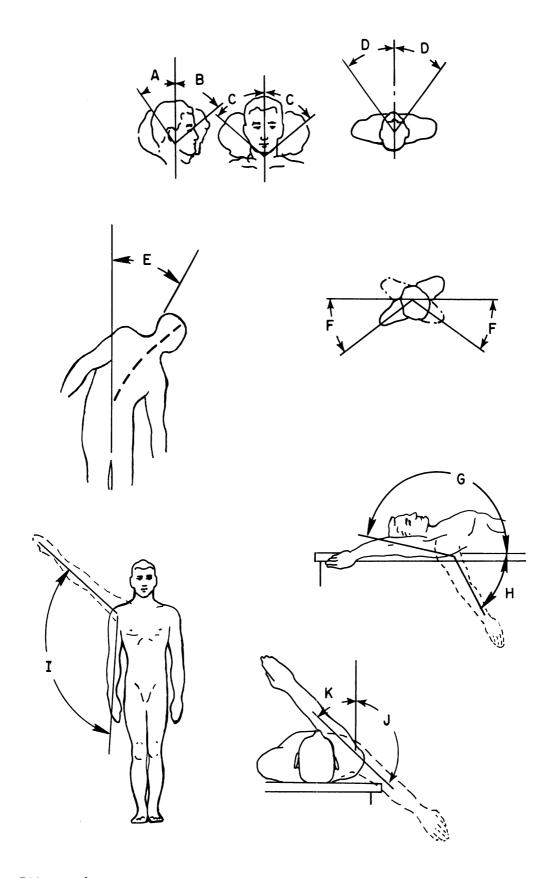


FIGURE 16. Illustrations of range-of-motion definitions (1 of 4).

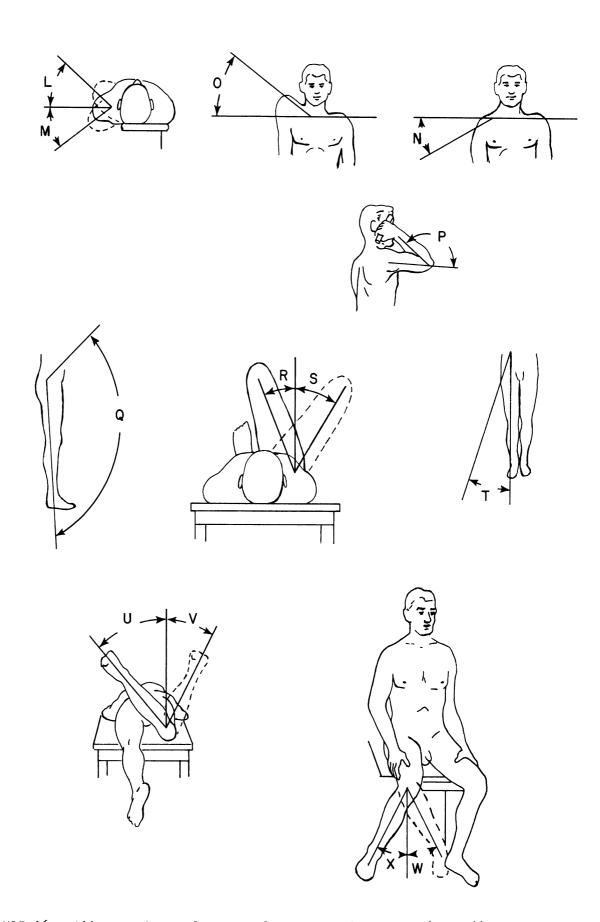


FIGURE 16. Illustrations of range-of-motion definitions (2 of 4).

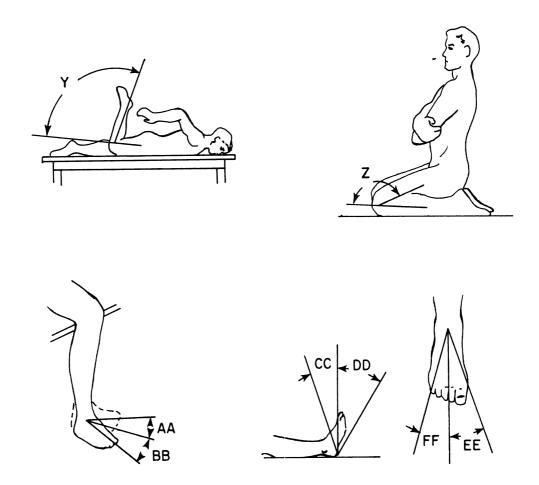
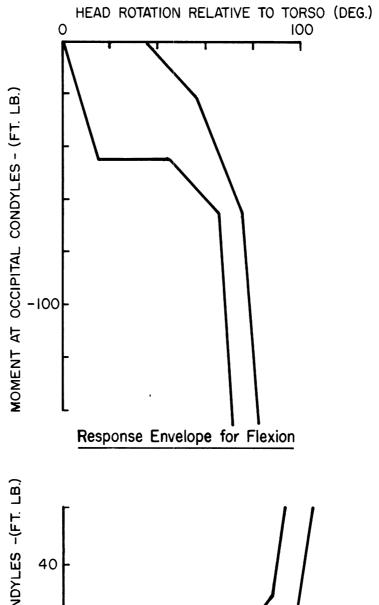


FIGURE 16. Illustrations of range of motion definitions (3 of 4).

Range-of-Motion Illustration Code

```
A - Head dorsal flexion (hyperextension)
 B - Head ventral flexion
 C - Head lateral flexion
 D - Head rotation
 E - Torso lateral flexion
 F - Torso rotation about long axis
 G - Shoulder flexion (sagittal plane) (3 links)
 H - Shoulder extension (sagittal plane) (3 links)
 I - Shoulder abduction (coronal plane) (3 links)
 J - Shoulder abduction (transverse plane) (3 links)
 K - Shoulder adduction (transverse plane) (3 links)
 L - Shoulder protraction (transverse plane) (clavicle)
 M - Shoulder retraction (transverse plane) (clavicle)
N - Shoulder depressed (coronal plane) (clavicle)
0 - Shoulder shrugged (coronal plane) (clavicle)
P - Elbow flexion
0 - Hip flexion
R - Hip abduction (transverse plane)
S - Hip adduction (transverse plane)
T - Hip abduction (coronal plane)
U - Hip medial rotation (prone)
V - Hip lateral rotation (prone)
W - Hip medial rotation (sitting)
X - Hip lateral rotation (sitting)
Y - Knee voluntary flexion (prone)
Z - Knee forced flexion (kneeling)
AA - Knee medial rotation
BB - Knee lateral rotation
CC - Ankle dorsiflexion
DD - Ankle plantar flexion
EE - Ankle inversion
FF - Ankle eversion
```

FIGURE 16. Illustrations of range-of-motion definitions (4 of 4).



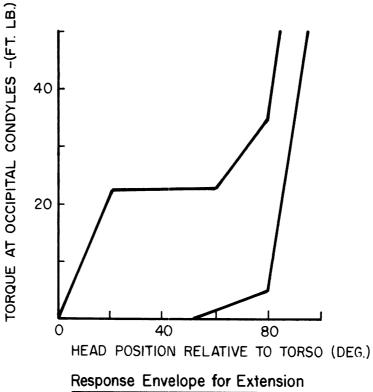


FIGURE 17. Head resistance to flexion and extension (after Mertz and Patrick 1971).

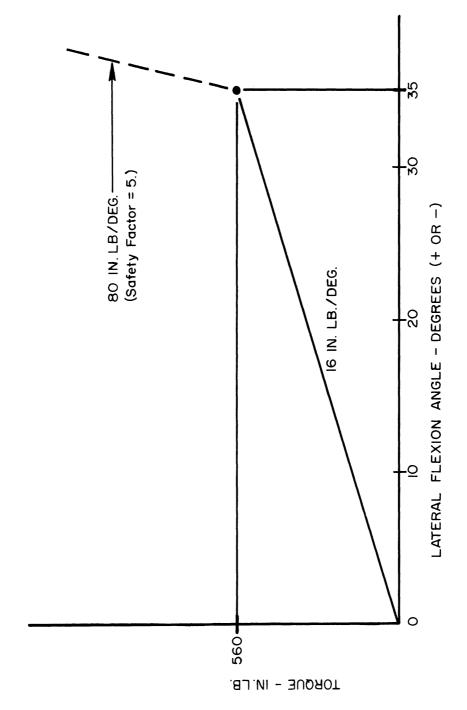
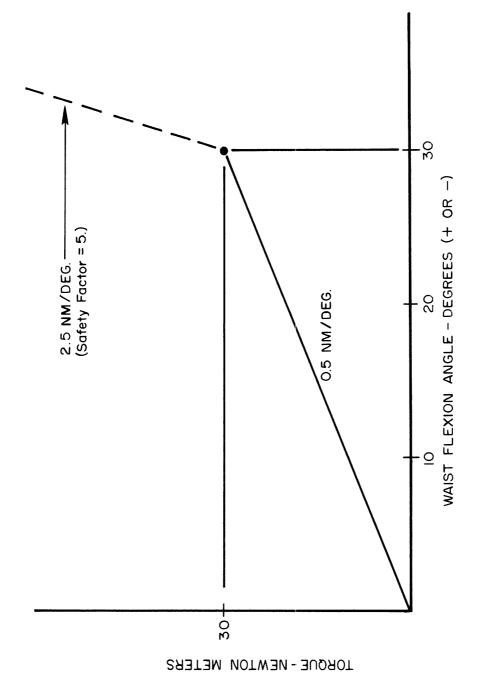
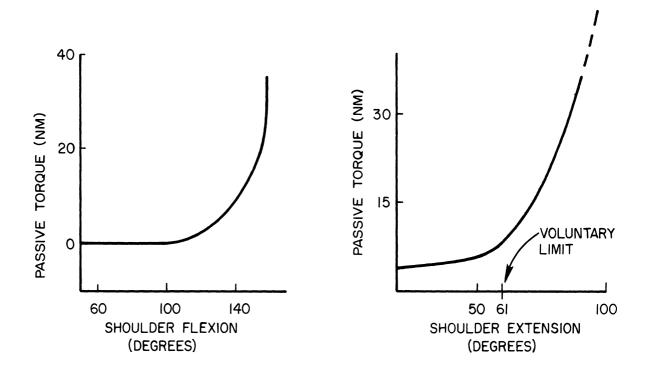


FIGURE 18. Head resistance to lateral flexion (after Snyder et al. 1975b).



Waist resistance to flexion and extension (after Krieger 1976). FIGURE 19.



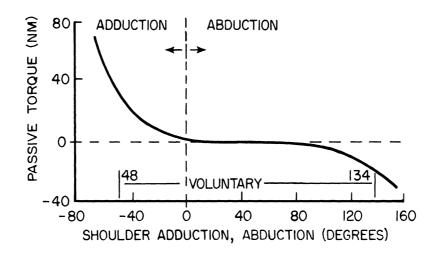


FIGURE 20. Shoulder resistance to rotation (after Engin 1980).

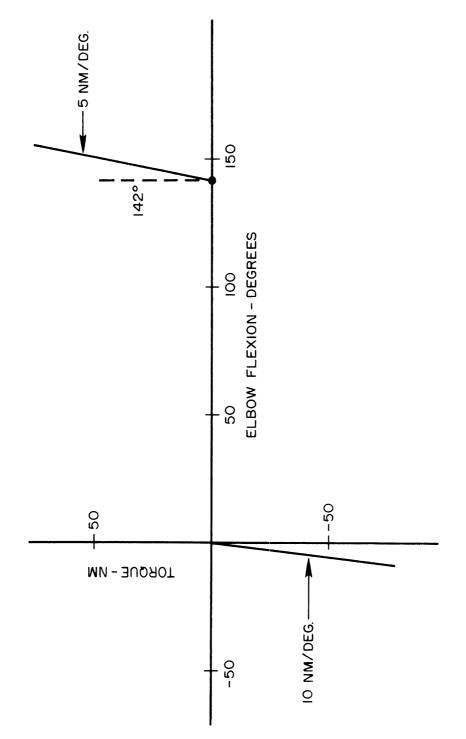


FIGURE 21. Elbow resistance to flexion (after Krieger 1976).

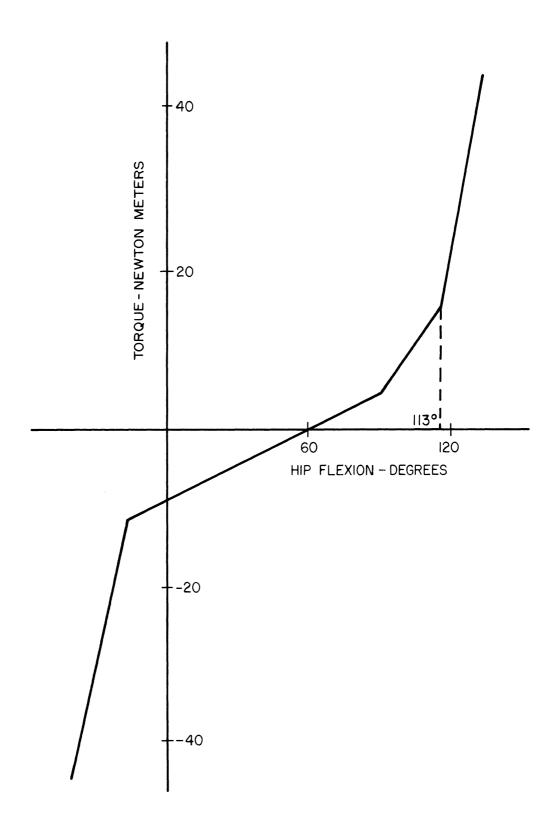


FIGURE 22. Resistance to hip flexion and extension (after Krieger 1976).

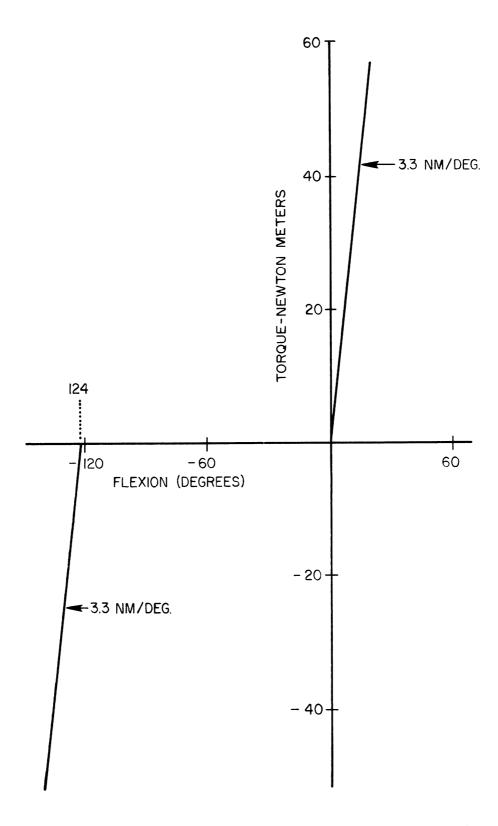


FIGURE 23. Resistance to flexion at knees (after Krieger 1976).

	,	

11.0 REFERENCES

- Barter, J.T.; Emanuel, I.; and Truett, B. (1957) <u>A statistical</u>
 evaluation of joint range data. Wright-Patterson AFB, Wright Air
 Development Center, WADC TN-57-311.
- Beier, G.; Schuller, E.; Schuck, M.; Ewing, C.L.; Becker, E.D.; and Thomas, D.J. (1980) Center of gravity and moments of inertia of human heads. Proc. 5th International IRCOBI Conference on the Biomechanics of Impacts, pp. 218-228. Edited by J.P. Cotte and A. Charpenne. IRCOBI, Bron.
- Bowman, B.M.; and Robbins, D.H. (1972) Parameter study of biomechanical quantities in analytical neck models. <u>Proc. 16th Stapp Car Crash</u> Conference, pp. 14-44.
- Bowman, B.M.; Bennett, R.O.; and Robbins, D.H. (1979) MVMA two-dimensional crash victim simulation, Version 4. The University of Michigan, Highway Safety Research Institute, Report No. UM-HSRI-79-5-1.
- Chandler, R.F.; and Young, J. (1981) <u>Uniform mass distribution</u>
 <u>properties and body size appropriate for the 50th percentile male</u>
 <u>aircrewmember during 1980-1990</u>. Federal Aviation Administration,
 Memorandum Report No. AAC-119-81-4.
- Cheng, R.; Mital, N.K.; Levine, R.S.; and King, A.I. (1979) Biodynamics of the living spine during -Gx impact acceleration. Proc. 23rd Stapp Car Crash Conference, pp. 721-764.
- Churchill, E.; and Truett, B. (1957) Metrical relations among dimensions of the head and face. Wright-Patterson AFB, Wright Air Development Center, WADC-TD-56-621.
- Clauser, C.E.; McConville, J.T.; and Young, J.W. (1969) Weight, volume, and center of mass of segments of the human body. Wright-Patterson AFB, Aerospace Medical Research Laboratory, AMRL-TR-69-70.
- Dempster, W.T. (1955a) <u>Space requirements of the seated operator</u>. Wright-Patterson AFB, Wright Air Development Center, WADC-TR-55-159.
- Dempster, W.T. (1955b) The anthropometry of body action. <u>New York</u>
 <u>Academy of Sciences Annals</u>, 63:559-585.
- Dempster, W.T. (1965) Mechanics of shoulder movement. <u>Archives of Physical Medicine and Rehabilitation</u>, 46:49-69.
- Dempster, W.T.; and Gaughran, G.R.L. (1967) Properties of body segments based on size and weight. American Journal of Anatomy, 120:33-54.

- Engin, A.E. (1979) Passive resistive torques about long bone axes of major human joints. <u>Aviation, Space, and Environmental Medicine</u>, 50:1052-57.
- Engin, A.E. (1980) On the biomechanics of the shoulder complex. <u>Journal</u> of Biomechanics, 13:575-590.
- Engin, A.E. (1981) Long bone and joint response to mechanical loading.
 Ohio State University for Air Force Office of Scientific Research.
 Bolling Air Force Base, Contract F49620-79-C-0110.
- Engin, A.E.; and Kaleps, I. (1980) Active muscle torques about long-bone axes of major human joints. <u>Aviation, Space, and Environmental</u> Medicine, 51:551-555.
- Engin, A.E.; and Kazarian, L. (1981) Active muscle force and moment response of the human arm and shoulder. <u>Aviation, Space, and Environmental Medicine</u>, 52:523-530.
- Ewing, C.L.; and Thomas, D.J. (1972) <u>Human head and neck response to impact acceleration</u>. Naval Aerospace medical Research Laboratory, Monograph 21.
- Ewing, C.L.; and Thomas, D.J. (1973) Response of human head to impact. Proc. 17th Stapp Car Crash Conference, pp. 309-342.
- Ferlic, D. (1962) The range of motion of the normal cervical spine. Hopkins Hospital Bulletin, 110.
- Foster, J.K.; Kortge, J.O.; and Wolanin, M.J. (1977) Hybrid III--A biomechanically based crash test dummy. Proc. 21st Stapp Car Crash Conference, pp. 973-1014.
- Frankel, V.H.; Burstein, A.H.; and Brooks, D.B. (1971) Biomechanics of internal derangement of the knee. <u>Journal of Bone and Joint Surgery</u>, 53A:945-962.
- Glanville, A.D.; and Kreezer, G. (1937) The maximum amplitude and velocity of joint movements in normal male human adults. <u>Human Biology</u>, 9:197-211.
- Kaleps, I. (1982) Phone conversations, July 20 and 27.
- Krieger, K. (1976) <u>Full scale experimental simulation of pedestrian-vehicle impacts</u>. Ph.D. dissertation, Wayne State University, Detroit.
- McConville, J.T.; Churchill, T.D.; Kaleps, I.; Clauser, C.E.; and Cuzzi, J. (1980) Anthropometric relationships of body and body segment moments of inertia. Wright-Patterson AFB, Aerospace Medical Research Laboratory, AMRL-TR-80-119.
- Mertz, H.J.; and Patrick, L.M. (1971) Strength and response of the human neck. Proc. 15th Stapp Car Crash Conference, pp. 207-255.

- Mital, N.K.; Cheng, R.; Levine, R.S.; and King, A.I. (1978) Dynamic characteristics of the human spine during -Gx acceleration. <u>Proc. 22nd Stapp Car Crash Conference</u>, pp. 139-165.
- Mital, N.K.; Cheng, R.; King, A.I.; and Eppinger, R.H. (1979) A new design for a surrogate spine. Proc. 7th International Technical Conference on Experimental Safety Vehicles, pp. 427-428. U.S. Government Printing Office, Washington, D.C.
- Nyquist, G.W.; and Murton, C.J. (1975) Static bending response of the lower human torso. <u>Proc. 19th Stapp Car Crash Conference</u>, pp. 513-541.
- Reynolds, H.M.; Clauser, C.E.; McConville, J.; Chandler, R.; and Young, J.W. (1975) Mass distribution properties of the male cadaver. SAE paper no. 750424.
- Reynolds, H.M.; Snow, C.C.; and Young, J.W. (1981) <u>Spatial geometry of the human pelvis</u>. Federal Aviation Administration, Memorandum Report No. AAC-119-81-5.
- Robbins, D.H. (1977) Errors in definition of an anatomically based coordinate system using anthropometric data. In Task Report, Phase I, Interim Report to AFOSR, Contract F44620-76-C-0115, Highway Safety Research Institute, The University of Michigan.
- Robbins, D.H.; Snyder, R.G.; and Roberts, V.L. (1971) <u>Mathematical</u> <u>simulation of daisy track human volunteer tests</u>. The University of Michigan, Highway Safety Research Institute, HSRI-BIOM-71-6.
- Robbins, D.H.; Snyder, R.G.; Chaffin, D.B.; and Foust, D.R. (1974) <u>A</u>

 mathematical study of the effect of neck physical parameters on

 injury susceptibility. SAE paper no. 740274.
- Schneider, L.W.; Foust, D.R.; Bowman, B.M.; Snyder, R.G.; Chaffin, D.B.; Abdelnour, T.R.; and Baum, J.K. (1975) Biomechanical properties of the human neck in lateral flexion. Proc. 19th Stapp Car Crash Conference, pp. 455-485.
- Snyder, R.G.; Chaffin, D.B.; and Schutz, R.K. (1972) <u>Link system of the human torso</u>. Wright-Patterson AFB, Aerospace Medical Research Laboratory, AMRL-TR-71-88.
- Snyder, R.G.; Chaffin, D.B.; and Foust, D.R. (1975a) <u>Bioengineering</u> study of basic physical measurements related to susceptibility to cervical hyperextension-hyperflexion injury. The University of Michigan, Highway Safety Research Institute, UM-HSRI-B1-75-6.
- Snyder, R.G.; Chaffin, D.B.; Schneider, L.W.; Foust, D.R.; Bowman, B.M.; Abdelnour, T.A.; and Baum, J.K. (1975b) <u>Basic biomechanical properties of the human neck related to lateral hyperflexion injury</u>. The University of Michigan, Highway Safety Research Institute, UM-HSRI-B1-75-4.



Technical Report Documentation Page

1. Report No.	2. Government Access	sion No. 3. R	ecipient's Catalog N	lo.	
4. Title and Subtitle			eport Date		
ANTHROPOMETRIC SPECIFIC	ATIONS FOR S	MALI	ecember 198		
AND LARGE MALE DUMMIES,		6. P	erforming Organizati	on Code	
		8. P	erforming Organization	on Report No.	
7. Author's) D.H. Robbins		U	MTR1-83-53-	·3	
9. Performing Organization Name and Address		10.	Work Unit No. (TRAI	S)	
The University of Michi Transportation Research		ļ.,			
2901 Baxter Road	mstreate		Contract or Grant No TNH22-80-C-		
Ann Arbor, Michigan 48109		13.	Type of Report and P	eriod Covered	
12. Sponsoring Agency Name and Address	_		INAL REPORT		
U.S. Department of Tran			oct. 1980-De	ec. 1983	
National Highway Traffi Washington, D.C. 20590	•	inistration 14.	Sponsoring Agency C	ode	
•	.0. 20590				
15. Supplementary Notes Vol. 1: Development of	Anthropometr	ically Based Des	ign Specifi	cations	
•	•	opomorphic Dummy	•		
Vol. 2: Anthropometric	<u>Specificatio</u>	ns for Mid-Sized	Male Dummy	/	
This report is	Volume 3 of	the Final Report	under Cont	ract	
DTNH22-80-C-07502, ''Dev	•	•	•	-	
Specifications for an A		• •	•	•	
Volume I describes the are based as well as th			•	cations	
` ·		to present the a		·ic	
specifications for smal		•	•		
during the project as w		_		-	
used in formulating the	se specifica	tions. Most of	the analyti	cal	
techniques used in comb	-				
described in Volume 2 w	•	•			
mid-sized male dummy. are included in Volume	_	ques and procedu	ires differ,	, they	
	<i>-</i>	by full-size blu	eprint nos.	SF-201.	
SF-202, and SF-203 for					
LM-303 for the large ma					
the following: surface	-				
gravity, origins of seg		•	•		
actual surface forms, i			ı principal	axes,	
and information on segm	entation pla	18. Distribution Statement			
Anthropometry		 _n 1	mited		
Crash Test Dummy		UIITI	III I LEU		
			T		
19. Security Classif. (of this report) None	20. Security Class	iif. (of this page) None	21- No. of Pages 85	22. Price	
HOHE	1	NOTIC	ر ن	į	

This document is disseminated under the sponsorship of the Department of Transportation in the interest of information exchange. The United States Government assumes no liability for the contents or the use thereof.

NOTICE

The rights, welfare, and informed consent of the volunteer subjects who participated in this study were observed under guidelines established by the U.S. Department of Health, Education and Welfare Policy (now Health and Human Services) on Protection of Human Subjects and accomplished under medical research design protocol standards approved by the Committee to Review Grants for Clinical Research and Investigation Involving Human Beings, Medical School, The University of Michigan.

VOLUME 3: CONTENTS

LIST	OF TABLES	٧
1.0	INTRODUCTION	1
2.0	SMALL FEMALE AND LARGE MALE SUBJECT DATA IN HIP POINT COORDINATES	3
	2.1 Development of Standard Seat	2
	Coordinate Systems	3
	Standard Seat Coordinate System	6
3.0	BODY SEGMENTATION	7
4.0	DEVELOPMENT OF ANATOMICALLY BASED SEGMENT	
,,,,	COORDINATE SYSTEMS	9
5.0	VOLUME, MASS, AND INERTIAL PROPERTIES	11
6.0	JOINT CENTERS	15
7.0	REFERENCES	75

LIST OF TABLES

		Page
1.	Surface Landmarks Relative to H-Point: Small Female	19
2.	Surface Landmarks Relative to H-Point: Large Male	22
3.	Formulation of Segmentation Planes: Small Female	25
4.	Formulation of Segmentation Planes: Large Male	26
5.	Location of Origins of Segment Anatomical Coordinate Systems: Small Female	27
6.	Location of Origin of Segment Anatomical Coordinate Systems: Large Male	27
7.	Anatomical Axes with Respect to Hip Point Axis System: Small Female (Cosine Matrix Expressed in Degrees)	28
8.	Anatomical Axes with Respect to Hip Point Axis System: Large Male (Cosine Matrix Expressed in Degrees)	30
9.	Anatomical Axes with Respect to Hip Point Axis System: Small Female (Cosine Matrix)	32
10.	Anatomical Axes with Respect to Hip Point Axis System: Large Male (Cosine Matrix)	34
11.	Coordinates of Surface Points on Clay Form: Small Female .	36
12.	Coordinates of Surface Points on Clay Form: Large Male	43
13.	Estimated Segment Mass and Volume: Small Female	49
14.	Estimated Segment Mass and Volume: Large Male	50
15.	Location of Estimated Segment Centers of Gravity with Respect to Whole-Body Coordinate System: Small Female	51
16.	Location of Estimated Segment Centers of Gravity with Respect to Whole-Body Coordinate System: Large Male	51
17.	Location of Estimated Segment Centers of Gravity with Respect to Segment Coordinate Systems: Small Female	52
18.	Location of Estimated Segment Centers of Gravity with Respect to Segment Coordinate Systems: Large Male	52
19.	Anthropometric Variables Used in Moment of Inertia Regression Equations: Small Female	53

20.	Anthropometric Variables Used in Moment of Inertia Regression Equations: Large Male	51
21.	Estimated Segment Inertial Properties: Small Female	55
22.	Estimated Segment Inertial Properties: Large Male	55
23.	Principal Axes of Inertia with Respect to Anatomical Axes: Small Female (Cosine Matrix Expressed in Degrees)	56
24.	Principal Axes of Inertia with Respect to Anatomical Axes: Large Male (Cosine Matrix Expressed in Degrees)	58
25.	Principal Axes of Inertia with Respect to Anatomical Axes Small Female: (Cosine Matrix)	60
26.	Principal Axes of Inertia with Respect to Anatomical Axes: Large Male (Cosine Matrix)	62
27.	Principal Axes of Inertia with Respect to Hip Point Axis System: Small Female (Cosine Matrix Expressed in Degrees)	64
28.	Principal Axes of Inertia with Respect to Hip Point Axis System: Large Male (Cosine Matrix Expressed in Degrees) .	66
29.	Principal Axes of Inertia with Respect to Hip Point Axis System: Small Female (Cosine Matrix)	68
30.	Principal Axes of Inertia with Respect to Hip Point Axis System: Large Male (Cosine Matrix)	70
31.	Location of Joint Centers: Small Female	72
32.	Location of Joint Centers: Large Male	72
33.	Location of Joint Centers in Segment Coordinates: Small Female	73
34.	Location of Joint Centers in Segment Coordinates:	71

1.0 INTRODUCTION

The purpose of Volume 3 is to present the anthropometric specifications for small female and large male dummies. Data gathered during the project as well as data available in the literature were used in formulating these specifications. Most of the analytical techniques and procedures used in combining the various data resources have been described in Volume 2 which presents the specifications for the midsized male dummy. Where techniques and procedures differ, they are included in Volume 2. As in Volumes 1 and 2 the subscripts L, H, and A are used with coordinate axes to indicate the laboratory, the whole body or H-point, and the anatomical or body segment reference systems, respectively.

The report is supplemented by full-size blueprint nos. SF-201, SF-202, and SF-203 for the small female and Nos. LM-301, LM-302, and LM-303 for the large male. These show side, front, and top views of the following:

- Surface landmarks
- Joint centers
- Segment centers of gravity
- Origins of segment coordinate systems
- Surface profile of actual surface form
- Information on anatomical and principal axes
- Information on segmentation planes



2.0 SMALL FEMALE AND LARGE MALE SUBJECT DATA IN HIP POINT COORDINATES

2.1 Development of Standard Seat Coordinate Systems

The same system of surface landmarks has been used to define the small female and large male surface forms as was used for the mid-sized male. These are described in detail in Volume 2.

To locate the hip joints (used to define an H-point which has been selected as the origin of coordinates for the surface form), the data of Reynolds et al. (1981) were again used. For the small female, Reynolds et al. obtained data from two body size cells. Both cells are for short females, but the weights range from light to heavy. The following compares the two cells of Reynolds et al. with the current data.

	Cell l	Cell 2	Current Study
Weight, kg (lb)	74.8 (165)	46.9 (103)	46.4 (102)
Stature, cm (in)	151.5 (59.6)	153.9 (60.6)	151.1 (59.5)

As should be expected, the match is good with the short, light segment of the population. In that the short height of all subjects generally implies a small frame, the pelvic data were accepted even though they may be slightly too large. No alternative data are known to exist.

Likewise, two body size cells were used for the large male. The two cells are fixed on tall subjects with weight varying widely. The following is a comparison of the two cells with the large male subject group of the current study.

	Cell 3	Cell 6	Current Study
Weight, kg (lb)	91.5 (201.3)	76.1 (167.4)	102.6 (225.8)
Stature, cm (in)	182.8 (72.0)	184.8 (72.8)	186.4 (73.4)

Although somewhat heavy, the large male standing height matches fairly well with the Reynolds et al. sample. Again, it is assumed that the height variable is the more important predictor of skeletal dimensions for the pelvis. Although the Reynolds et al. pelvis data may be somewhat small for the large male, there are no known alternatives and it is believed any differences will be small (less than 1 cm).

The direction of the Reynolds et al. coordinate system was superimposed upon the UMTRI data for anterior-superior iliac spine (ilio-spinale summum) and pelvic crest (pubic symphysis). In order to accomplish this, tissue thickness estimates were made for the distances from the surface targets to the underlying bony landmarks in the vehicle-seated posture. The first estimates were made for the mid-sized male. A tissue depth of 5 mm over the anterior-superior iliac spines was estimated from palpation of this point on standing subjects. While the subjects were standing, the overlying tissue is fairly taut across the pelvic spines. However, when they were seated, the abdominal tissue tended to slacken and rest over the pelvic girdle. Therefore, the tissue thickness was much greater in the seated subjects. For photographic determination of the pelvic surface landmarks, the technique used was to palpate the point and place the end of a metal probe rod firmly on the location so that a projection to the landmark could be determined by photometric analysis of calibrated marks on the Because the tissue was effectively pushed out of the way by the probe, the 5-mm tissue thickness estimate was used for pelvic location. Also, because the probe was held within 10° of vertical, the depth to the bone was applied to the Z_1 coordinate.

A tissue depth of 15 mm over the pubic symphysis was estimated by palpation in placing the probe and by analysis of general anatomical factors such as muscle attachments in this region. The probe was held within 10° of vertical in the $Y_L Z_L$ plane and 30° of vertical in the $X_L Z_L$ plane. Therefore, with an estimated tissue thickness of 15 mm, the depth to the bone landmark was 13 mm in the Z_L coordinate and 7 mm in the Z_L coordinate. These results were scaled for the case of the small

female and large male. The data used to locate points on the pelvis from surface landmark data are summarized as follows:

Surface	Coordinate	Small	Mid-Sized	Large
Landmark		Female	<u>Male</u>	<u>Male</u>
ASIS	X _L coord (+ to front)	0	0	0
	Z _L coord (+ up)	-3	- 5	- 7
Symphysis	X _L coord (+ to front)	-5	- 7	-10
	X _L coord (+ up)	-8	-13	-17

With respect to laboratory coordinates the two coordinate systems made angles of 55.53° (large male) and 48.37° (small female). These compare with the 54.07° for the mid-sized male. Using the resulting coordinate transformation it was possible to obtain the following points needed for construction of joint centers, segmentation planes, anatomical segment axis construction, etc.

- H-points
- Pubic symphysis
- Inferior symphyseal pole
- Superior pole, pubic symphysis
- Ilio-spinale summum
- Ilio-cristale summum
- Inferior tuberosity point
- Posterior point on 1st sacral vertebral body
- Promontorion
- Lateral point on 1st sacral vertebral body
- Pubotuberosity
- Lateral tuberosity point

The key points for development of standard seat coordinate systems for the surface forms were the H-points which, when referred to the original UMTRI laboratory coordinate system, are at:

Form		X _L (mm)	Y _L (mm)	Z _L (mm)	
Small Female:	Left Right	755 755	699 539	425 425	
Large Male:	Left Right	618 618	705 533	409 409	

The Y_L -shifts from the body centerline where ± 80 and 86 mm as reported by Reynolds et al. The centers of the lines connecting the two H-points are at Y_L =619 mm, yielding the origins of the standard seat coordinate systems for the two forms.

2.2 <u>Subject Data Translated to</u> <u>Standard Seat Coordinate System</u>

Tables 1 and 2 present all skeletal and surface landmarks used in the development of the anthropometric specifications for the small female and large male surface forms. The origin of coordinates is the center of a line connecting the H-points.

3.0 BODY SEGMENTATION

The segmentation scheme used for the mid-sized male (and documented in detail in Volume 2) has been adopted for use in developing segmentation plane formulae for the small female and large male specification packages. Using this scheme, it was necessary to quantify a variety of points in addition to those already available in the list of measured surface landmarks. These included:

- Nuchale
- Intersection point on back of surface form of a perpendicular from the center of a line connecting the 10th rib targets to a line connecting the T12 and L5 surface targets
- Intersection point on back of surface form of a perpendicular from the center of a line connecting the iliocristale targets to a line connecting the T12 and L5 surface targets
- Pubotuberosity surface (35 mm lateral from pubic symphysis surface point)
- Shifted ASIS (a point 10 mm lateral to ASIS surface)
- Shifted inferior tuberosity (a point 10 mm lateral to inferior tuberosity point which is projected vertically to the seat surface)

Other than nuchale, these points were obtained directly using geometric construction.

For the small female an estimation of the nuchale location was obtained using the data of Young et al. (1983). In their report, the location of nuchale was given in anatomical coordinates (millimeters) as $X_A=-88$, $Y_A=0$, $Z_A=-31$. In otherwords, nuchale is behind and below the center of a line connecting the tragions which serves as the origin. In addition, the coordinates of the center of a line connecting the infraorbitales are given as $X_A=69.8$ mm. When this construction is superimposed on the same coordinate direction using the same origin, it is found that the Young et al. (1983) infraorbitale is 9 mm behind that obtained in the current study. Also, the nuchale was projected to be 18 mm behind the surface of the head profile line which was measured directly. If the mismatch between infraorbitales is eliminated by shifting tragion forward, then the nuchale still falls 9 mm behind the

surface of the head. It can be suggested that the nuchale target was measured too far behind tragion in the Young et al. study based on hair thickness and the use of a cap during their photography. Based on this assumption, the nuchale point was moved along the X_{L} coordinate axis to lie on the surface form. A similar shift was necessary in the case of the large male form. In that case the infraorbitale predicted from the McConville et al. (1980) report was found to be 17 mm behind that measured at UMTRI. Also, the nuchale was 16 mm behind the surface of the dummy form. It appears that there is a discrepancy in tragion locations as measured in the two sets of studies. This issue has also been discussed in Volume 2 on the mid-sized male.

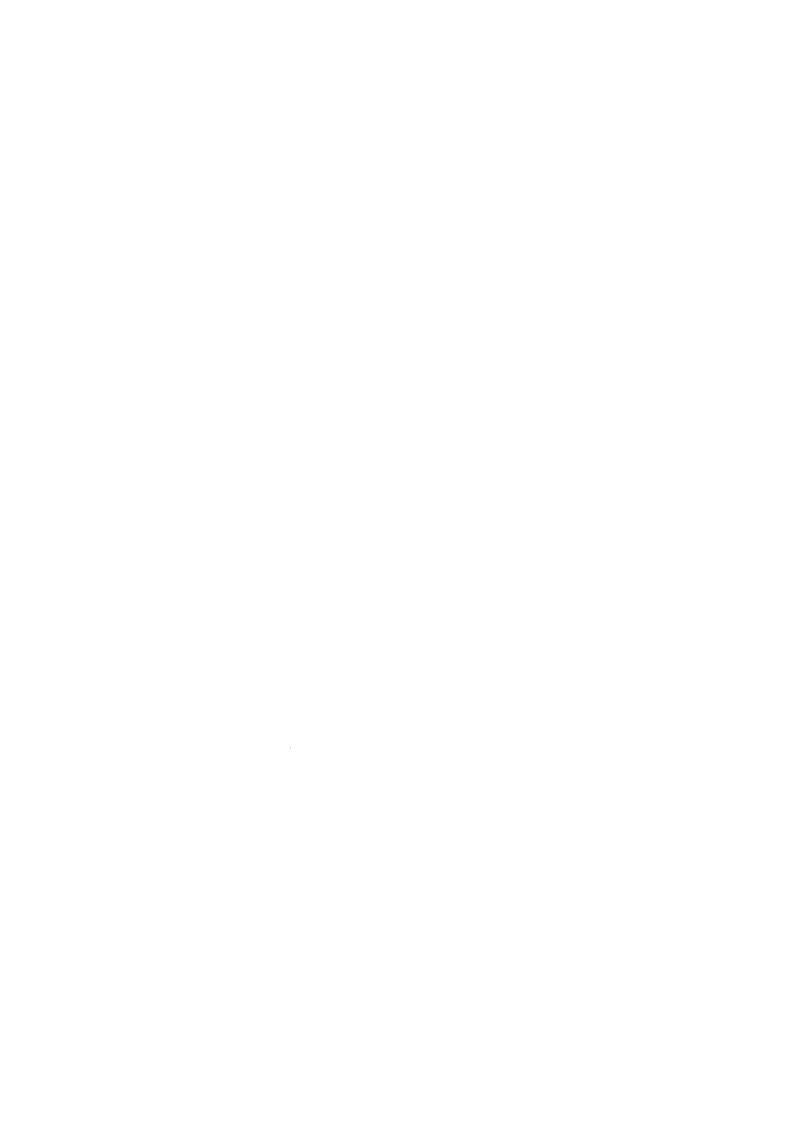
With all the points available, each segmentation plane was computed directly using three points. Tables 3 and 4 show the formulae for the segmentation plans for the small female and large male surface forms.

4.0 DEVELOPMENT OF ANATOMICALLY BASED SEGMENT COORDINATE SYSTEMS

This section of the report summarizes the development of anatomically based coordinate systems for each of the various segments of the body. The coordinate systems which have been constructed are the same as, or very similar to, those which have been reported by McConville et al. (1980) in developing anthropometric relationships of body and body segment moments of inertia. As such, they have been used directly in the presentation of center of mass and inertial data and provide the linkage between the coordinate system defining the principal axes of inertia and the standard coordinate system at the center of the H-points. In order to construct coordinate systems and relate them to the standard system, it was necessary to know three points in the segment. The following three were used:

- One at the origin
- One on an axis
- One in one of the orthogonal planes

The points used for each system are defined in Table 2 of Volume 2. Data used are given in Tables 1 and 2 of this volume. The locations of the origins of the various segment anatomical coordinate systems are given in Tables 5 and 6 for the small female and large male. Tables 7 and 8 give the cosine matrices expressed in degrees for all anatomical axis systems with respect to the hip point coordinate system, while Tables 9 and 10 present the cosine matrices directly.



5.0 VOLUME, MASS, AND INTERTITAL PROPERTIES

The basic information for these computations is contained in the reports by McConville et al. (1980) and Young et al. (1983). Specific numbers are given for the distance from the origins of anatomically based segment coordinate systems to centers of volume. In addition, regression formulas have been provided to predict volume and inertial properties of the various segments of the body.

The basic anthropometric data for the small female and large male groups (see Section 3 of Volume 1) have been supplemented by the surface profile data given in Tables 11 and 12. These were measured directly on the clay form before molds and castings for the final surface forms were made. The data from these two resources was then used to select anthropometric variables for use in the regression equations. This task was made more complicated by the difference between the seated postures of the current study and the standing postures which were the basis of the regression equations. Variables selected were similar to those used in the mid-sized male computations (Volume 2).

The predicted volumes and the sum of volumes for the whole body are given in Tables 13 and 14 for the small female and large male surface forms. The values obtained for the left and right sides of the body have been averaged. These calculations are based on a density assumption of 1.0 gm/cm 3 . Using this value for density, the resulting total body weights would be overestimated by

Small Female = 3.0 percent Large Male = 5.4 percent

If a density value of 0.92, as has been proposed by Dempster (1955), is used for the thorax, the predicted values for weight are much closer to subject means, especially for the small female. Because of the apparent overestimation, volume scaling factors were used to yield body segment weights which, when summed, yielded the correct total body weight. For

volume, the large male scale factor was 0.949 based on the 5.4 percent overestimation. For moment of inertia corrections this led to a scale factor of 0.966 using the analog

Volume =
$$0.949V \sim (.9827l)^3$$

The scale factor for the small female was selected as 1.0. This was based on the smaller overestimation of volume and the fact that using Dempster's data (1955), the overestimation can become an underestimation. Clearly, some additional work should be done to better specify segment densities.

Young et al. (1983) and McConville et al. (1980) give the locations of centers of volume in segment anatomical coordinate systems. The assumption has been made that center of volume and center of mass are coincident. These data are provided for average females and males. To take this into account, the data have been scaled down for the small female and scaled up for the large male. The scaling is based on comparisons of anthropometric data on length, depth, height, breadth, etc. for the various segments. As anatomically based coordinate systems are oriented primarily in the same directions as heights, depths, and breadths are measured, this scaling procedure appears reasonable. Tables 15 and 16 give the locations of estimated segment centers of gravity with respect to the whole-body coordinate systems for the small female and large male. Tables 17 and 18 give the locations with respect to the individual segment coordinate system, thus documenting the scaling which was carried out.

The anthropometric variables used in the moment of inertia regression equations are given in Tables 19 and 20 for the two surface forms. The resulting moments of inertia are given in Tables 21 and 22. Both predicted and scaled results are included in the tables.

The principal axes of inertial for each segment have been computed by both Young et al. (1983) and McConville et al. (1980) with respect to segment anatomical coordinate systems. In the present study, these transformations were modified slightly to reflect the body symmetry assumption. Tables 23 and 24 present the principal axes of

inertia with respect to anatomical axes as cosine matrices in degrees while Tables 25 and 26 present the cosine matrices directly. Tables 27 through 30 do the same for the principal axes with respect to the H-point coordinate system.



6.0 JOINT CENTERS

The development of joint centers for the small female and large male was based on the results already obtained for the mid-sized male and presented in Volume 2. Because of the similarity of body posture of the three surface forms, it was possible to scale up for the large male and scale down for the small female. The locations of the resulting joint centers are given in Tables 31 and 32 with respect to H-point coordinates. Tables 33 and 34 list the results in segment coordinates.

Head/Neck. For the head/neck junction, the location is chosen to be the occipital condyles. For the mid-sized male, this point is at $(X_H Z_H) = (-11, -26)$ in head segment coordinates. The scale factor on head length (X_H) and head height (Z_H) is 0.978 for the small female yielding a scaled joint which rounds off to (-11, -25). The location of this point can be transformed to H-point coordinates using the appropriate cosine matrix and translated to the origin using data from the table listing segment origins. Scale factors for the large male are 1.025 on the X_H coordinate and 1.009 on the Z_H coordinate. This yields a scaled condyle point with segment coordinates (-11, -26). Scaled locations for some joints show a greater difference from the mid-sized male.

<u>C7/T1</u>. In this case the C7 and glabella surface landmark data were used to establish the angle required for use in the regression equations given in the torso link study by Snyder et al. (1972). Cervical vector prediction equations were available to predict the distance of the C7 surface marker to the C7/T1 interspace as well as the angle made by the vector connecting C7 to the interspace. The predicted angle to the interspace was used directly. However, the distance to the interspace was scaled.

The following chart shows the scaling used in the torso from ${\tt C7}$ to ${\tt S1.}$

Quantity	Large Male	Mid-Sized Male	Small Female
Upper torso depth (cm)	13.788 31.608	11.912	8.976
Abdominal depth (cm) C7-T12 vector distance (mm)	-	26.948 344	20.956 325
T12-L5 vector distance (mm)	158	151	109
Upper torso Z _u scale factor	1.09	1	0.86
Upper torso X scale factor	1.16	1	0.75
Abdomen Z, scale factor	1.05	1	0.72
Upper torso Z _H scale factor Upper torso X _H scale factor Abdomen Z _H scale factor Abdomen X _H scale factor	1.17	1	0.78

So, the value of 2.99 inches, the distance from the C7 surface marker to the C7/T1 interspace for the mid-sized male, was broken into Z_H and X_H components and scaled to 2.26 inches (57.4 mm) for the small female and 3.45 inches (87.6 mm) for the large male.

T4/T5, T8/T9, T12/L1. Similarly, thorax vector prediction equations were used in estimating the location of these interspaces. These required the availability of T4 and T12 surface markers. The angle between a line connecting these two points and a vertical line served as the reference angle for use in the regression equations. After computation of this angle for the small female and large male forms, the equations were then used to predict the following:

- Distance from T4 to T4/T5 interspace
- Vector direction from T4 to T4/T5 interspace
- Distance from T8 to T8/T9 interspace
- Vector direction from T8 to T8/T9 interface
- Distance from T12 to T12/L1 interspace
- Vector direction from Tl2 to Tl2/Ll interspace

In each case the predicted distance was broken into components and scaled for large male or small female.

<u>L5/S1</u>. The same procedure was adopted for definition of the L5/S1 joint as has been used for the mid-sized male. This was to choose a point on the centerline of the body with X_H and Z_H coordinates the same as the lateral point on the first sacral vertebral body. These values were taken directly from the pelvis skeletal reconstruction discussed in Section 2 and presented in Tables 1 and 2.

L2/L3. As in the case of the mid-sized male, this joint was selected to be 60 percent of the distance along a line connecting L5/S1 with T12/L1.

Sternoclavicular. For the mid-sized male, this point was estimated to be one centimeter below and two centimeters lateral from the body centerline. Scaling for this point is based on the Y_{μ} values for the acromion points or 0.84 for the small female and 1.02 for the large male.

Claviscapular. For the mid-sized male, this point was estimated from a definition by Dempster (1955) and measurements on bony material to be the following distances from the acromic-clavicular articulation landmark.

- $\Delta Y_H = 27.5/2$ mm toward the center of the body $\Delta X_H = 15$ mm toward the rear of the body $\Delta Z_H = 10$ mm down

The scale factor based on biacromial diameter developed for the sternoclavicular joint was also used for this joint.

Glenohumeral. The glenohumeral joint center for the mid-sized male was based on a reconstruction of skeletal material (the humerus) in threedimensional space using tissue thickness estimates and three surface landmarks (greater tubercle of the humerus, lateral humeral epicondyle, and medial humeral epicondyle). This point is more or less fixed with respect to the scapula, and as such, with respect to the acromion. To estimate the glenohumeral joint center for the small female and large male, the mid-sized male vector from acromion to this joint was scaled by the factor used for the sternoclavicular and claviscapular joints.

Elbow. This point was computed directly for both the small female and large male as the midpoint of a line between the medial humeral epicondyle and a point 8 mm above the radiale. The "8 mm" point was estimated to be along a line connecting radiale with ulnar styloid for the seated occupants.

<u>Wrist</u>. The reconstruction of the wrist joint was based on the definitions used for the mid-sized male. The dimensions used were scaled based on radius length for the two forms (0.84 for the small female and 1.07 for the large male).

<u>Hip</u>. The hip joints are the H-points discussed earlier and given in Tables 1 and 2.

<u>Knee</u>. The knee joints were computed directly as the center of a line connecting the medial and lateral femoral epicondyle.

Ankle. The ankle joint has been defined for the mid-sized male as the midpoint of a line between the tip of the lateral malleolus of the fibula and a point 5 mm distal to the tibial malleolus. In order to obtain the "5 mm" point, the sphyrion was shifted down the leg a resultant of 5 mm for the seated subjects.

TABLE 1

SURFACE LANDMARKS RELATIVE TO H-POINT (mm):

SMALL FEMALE

Landmark	x _H	YH	z _H
HEAD			
Glabella Infraorbitale (L) Infraorbitale (R) Tragion (L) Tragion (R) Gonion (L) Gonion (R) Gnathion Nuchale*	- 90 -103 -103 -180 -180 -167 -167 - 91 -247	0 32 - 32 67 - 67 - 55 - 55 0	578 550 555 545 545 484 465 517
TORSO			
Suprasternale Mesosternale Substernale Nipple (L) Nipple (R) 10th Rib, anterior, midline Umbilicus Maximum Abdominal Protrusion 10th Rib (L) 10th Rib (R)	-144 -110 - 89 - 39 - 39 - 10 1 22 - 96 - 96	0 0 85 - 85 0 0 0 129 -129	391 353 316 250 250 150 141 129 125
VERTEBRAL COLUMN			
C7 T4 T8 T12 L2 L5 Mid-Spine 10th Rib Intersection point on back of surface form of a perpendicular from center of line connecting 10th rib targets to line connecting T12 and L5 surface targets* Intersection point on back of surface form of a perpendicular from center of line connecting iliocristale targets to line connecting T12 and L5 surface targets*	-238 -259 -247 -200 -180 -154 -201 -183	0 0 0 0 0 0	445 364 242 122 79 23 126 85

TABLE 1
SURFACE LANDMARKS RELATIVE TO H-POINT (mm):
SMALL FEMALE (Continued)

Landmark	X _H	YH	z _H
PELVIS (SURFACE)			
Trochanterion (UMTRI photo) (L) Trochanterion (UMTRI photo) (R) Iliocristale (L) Iliocristale (R) Anterior-Superior Iliac Spine (L) Anterior-Superior Iliac Spine (R) Pubic Symphysis Thigh/Abdominal Junction (L) Thigh/Abdominal Junction (R) Trochanterion (Skeletal Reconstruction)* Pubotuberosity	- 3 - 83 - 83 - 15 - 15 - 15 - 44 - 22 - 22 - 18 - 44	187 -187 138 -138 103 -103 0 117 -117 ±190 ± 35	- 19 - 19 - 86 - 86 - 75 - 75 - 32 - 60 - 18 - 32
PELVIS (SKELETAL)			
Pubic Symphysis H-Point Inferior Symphyseal Pole Left Superior Pole, Pubic Symphysis Ilio-Spinale Summum Iliocristale Summum Inferior Tuberosity Point Posterior Point, 1st Sacral Vertebral Body Promontorion Lateral Point, 1st Sacral Vertebral Body	42 0 40 46 - 15 - 81 24 - 92 - 66 - 80	0 ± 80 ± 4 ± 5 ±109 ±114 ± 48 0 0 ± 19	22 0 - 10 26 72 77 - 56 41 42 46
SHOULDER			
Clavicale (L) Clavicale (R) Acromio-Clavicular Articulation (L) Acromio-Clavicular Articulation (R) Greater Tubercle Humerus (L) Greater Tubercle Humerus (R) Acromion (L) Acromion (R) Anterior Scye (L) Anterior Scye (R) Posterior Scye (R) Superior Margin Scapula (L) Inferior Margin Scapula (R)	-146 -146 -198 -198 -152 -152 -206 -206 -106 -191 -191 -262 -262 -250	17 - 17 152 -152 178 -178 171 -171 130 -130 164 -164 66 - 66	397 398 398 398 380 376 376 337 286 286 379 292 292

TABLE 1
SURFACE LANDMARKS RELATIVE TO H-POINT (mm):
SMALL FEMALE (Continued)

Landmark	Х _Н	YH	z _H
ARM			
Lateral Humeral Epicondyle (L) Lateral Humeral Epicondyle (R) Radiale (L) Radiale (R) Medial Humeral Epicondyle (L) Medial Humeral Epicondyle (R) Olecranon (L) Olecranon (R) Ulnar Styloid (L) Ulnar Styloid (R) Stylion (L) Stylion (R)	12 12 28 28 15 15 34 34 130 130 121	211 -211 207 -207 150 -150 183 -183 182 -182 136 -136	206 206 193 193 190 190 177 177 383 383 387 387
LEG AND FOOT		.	<u> </u>
Lateral Femoral Epicondyle (L) Lateral Femoral Epicondyle (R) Medial Femoral Epicondyle (L) Medial Femoral Epicondyle (R) Tibiale (L) Tibiale (R) Patella (L) Patella (R) Sphyrion (L) Sphyrion (R) Metatarsal-Phalangeal I (L) Metatarsal-Phalangeal I (R) Digit II (R) Metatarsal-Phalangeal V (L) Metatarsal-Phalangeal V (R) Lateral Malleolus (L) Lateral Malleolus (R) Posterior Calcaneus (heel point) (R)*	360 365 365 378 404 599 698 729 683 584 584 618	119 -119 32 - 32 35 - 35 81 - 81 - 57 - 76 - 76 - 126 - 126 - 126 - 157 - 115 - 115 - 90 - 90	72 72 69 69 58 91 -172 -120 -120 -147 -147 -194 -254

^{*}Landmark determined by construction.

TABLE 2

SURFACE LANDMARKS RELATIVE TO H-POINT (mm):

LARGE MALE

Landmark	x _H	YH	z _H
HEAD	•		la mana di mana
Glabella Infraorbitale (L) Infraorbitale (R) Tragion (L) Tragion (R) Gonion (L) Gonion (R) Gnathion Nuchale*	-111 -128 -128 -212 -212 -195 -195 -108 -293	0 37 - 37 83 - 83 70 - 70 0	684 650 650 646 646 576 576 555 612
TORSO			
Suprasternale Mesosternale Substernale Nipple (L) Nipple (R) 10th Rib, anterior, midline Umbilicus Maximum Abdominal Protrusion 10th Rib (L) 10th Rib (R)	-162 -119 - 89 - 59 - 59 - 33 - 60 - 75 -126 -126	0 0 132 -132 0 0 0 194 -194	459 415 364 320 320 218 172 153 143
VERTEBRAL COLUMN			
C7 T4 T8 T12 L2 L5 Mid-Spine 10th Rib Intersection point on back of surface form of a perpendicular from center of line connecting R10 targets to line connecting T12 and L5 surface targets* Intersection point on back of surface form of a perpendicular from center of line connecting iliocristale targets to line connecting Iliocristale targets to line connecting T12 and L5 surface targets*	-300 -333 -327 -283 -246 -202 -277 -237	0 0 0 0 0 0	531 421 284 155 95 19 144 77

TABLE 2
SURFACE LANDMARKS RELATIVE TO H-POINT (mm):
LARGE MALE (Continued)

Landmark	x _H	YH	z_H		
PELVIS (SURFACE)					
Trochanterion (UMTRI photo) (L) Trochanterion (UMTRI photo) (R) Iliocristale (L) Iliocristale (R) Anterior-Posterior Iliac Spine (L) Anterior-Posterior Iliac Spine (R) Pubic Symphysis Thigh-Abdominal Junction (L) Thigh-Abdominal Junction (R) Trochanterion (Skeletal reconstruction)* Inferior Tuberosity Point* Pubotuberosity*	- 34 - 34 - 114 - 114 - 27 - 27 50 19 19 22 42 50	217 -217 197 -197 121 -121 0 155 -155 ±215 ± 51 ± 35	33 105 105 86 86 50 94 - 22 -115		
PELVIS (SKELETAL)					
Pubic Symphysis H-Point Inferior Symphyseal Pole Left Superior Pole, Pubic Symphysis Ilio-Spinale Summum Iliocristale Summum Inferior Tuberosity Point* Posterior Point, 1st Sacral Vertebral Body Promontorion Lateral Point, 1st Sacral Vertebral Body	40 0 43 38 - 27 -107 42 -105 - 73 - 93	0 ± 86 ± 4 ± 5 ±115 ±125 ± 41 0 0 ± 28	33 0 - 6 37 79 74 - 62 34 41 42		
SHOULDER					
Clavicale (L) Clavicale (R) Acromio-Clavicular Articulation (L) Acromio-Clavicular Articulation (R) Greater Tubercle Humerus (L) Greater Tubercle Humerus (R) Acromion (L) Acromion (R) Anterior Scye (L) Anterior Scye (R) Posterior Scye (L) Posterior Scye (R) Superior Margin Scapula (L) Inferior Margin Scapula (R)	-171 -171 -247 -247 -185 -185 -256 -256 -115 -245 -245 -331 -301 -301	25 -25 192 -192 223 -223 -227 -217 167 -167 221 -221 83 -83 147 -147	473 473 480 480 469 469 454 421 328 328 446 271 271		

TABLE 2
SURFACE LANDMARKS RELATIVE TO H-POINT (mm):
LARGE MALE (Continued)

Landmark	X _H	Y _H	z _H
ARM			
Lateral Humeral Epicondyle (L) Lateral Humeral Epicondyle (R) Radiale (L) Radiale (R) Medial Humeral Epicondyle (L) Medial Humeral Epicondyle (R) Olecranon (L) Olecranon (R) Ulnar Styloid (L) Ulnar Styloid (R) Stylion (L)	34 34 52 52 27 27 48 48 262 262 245 245	266 -266 261 -261 189 -189 -234 -234 197 -197 138 -138	270 270 252 252 236 236 225 398 398 414 414
LEG AND FOOT			•
Lateral Femoral Epicondyle (L) Lateral Femoral Epicondyle (R) Medial Femoral Epicondyle (L) Medial Femoral Epicondyle (R) Tibiale (L) Tibiale (R) Patella (L) Patella (R) Sphyrion (L) Sphyrion (R) Metatarsal-Phalangeal I (L) Metatarsal-Phalangeal I (R) Digit II (L) Digit II (R) Metatarsal-Phalangeal V (L) Metatarsal-Phalangeal V (R) Lateral Malleolus (L) Lateral Malleolus (R) Posterior Calcaneus (heel point) (L)* Posterior Calcaneus (heel point) (R)*	411 411 414 433 460 721 845 889 889 832 711 741	207 -207 -207 -98 -97 -97 -168 -168 -63 -63 -85 -150 -150 -187 -135 -135 -97	157 157 175 163 163 202 202 -131 -131 - 70 - 14 - 105 - 169 - 169 - 238 - 238

^{*}Landmark determined by construction.

TABLE 3

FORMULATION OF SEGMENTATION PLANES: SMALL FEMALE

Head:	$.38133X_{H} + .92444Z_{H} - 383.75 = 0$
Neck:	$.70711X_{H} + .70711Z_{H} - 177.48 = 0$
	(for all X _H ≥ -194)
Thorax:	$.41773X_{H}90857Z_{H} + 153.67 = 0$
Abdomen:	$.42046x_{H}90731z_{H} + 112.93 = 0$
Hip:	$79326x_{H} \pm .60868y_{H} + .01568z_{H} + .55.706 = 0$
	(+ sign on Y _H for right side of body)
Knee:	$95067x_{H} + .31022Z_{H} + 319.90 = 0$
Ankle:	$.74130x_{H}67118z_{H} - 519.21 = 0$
Shoulder:	$.37621x_{H} \pm .92649y_{H}00936z_{H} - 77.411 = 0$
	(+ sign on Y _H for left side of body)
Elbow:	$71664x_{H} \pm .14376Y_{H}68246Z_{H} + 118.85 = 0$
	(+ sign on Y _H for left side of body)

TABLE 4

FORMULATION OF SEGMENTATION PLANES: LARGE MALE

Head:	$.34482X_{H} + .93867Z_{H} - 473.43 = 0$
Neck:	.70711X _H + .70711Z _H - 213.55 = 0
Thorax:	$.51108x_{H}85954z_{H} + 187.31 = 0$
Abdomen:	$.50957X_{H}86043Z_{H} + 148.44 = 0$
Hip:	$78392X_{H} \pm .62046Y_{H}02216Z_{H} + 62.020 = 0$
	(+ sign on ${\sf Y}_{\sf H}$ for right side of body)
Knee:	$97780x_{H} + .20953z_{H} + 368.98 = 0$
Ankle:	.69191X _H 72199Z _H - 593.44 = 0
Shoulder:	$.34605X_{H} \pm .93630Y_{H} + .05993Z_{H} - 141.80 = 0$
	(+ sign on Y _H for left side of body)
Elbow:	$84192X_{H} \pm .28017Y_{H}46117Z_{H} + 78.614 = 0$
	(+ sign on Y _H for left side of body)

TABLE 5

LOCATION OF ORIGIN OF SEGMENT ANATOMICAL COORDINATE SYSTEMS: SMALL FEMALE

Segment	X _H (mm)	Y _H (mm)	Z _H (mm)
Head	-180	0	545
Neck	-238	0	445
Thorax	-183	0	85
Abdomen	- 96	0	125
Pelvis	- 15	0	75
Upper Arms	-206	±171*	376
Lower Arms	28	±207	193
Upper Legs	18	±190	- 18
Lower Legs	378	± 35	58
Feet	695	±115	-126

*Positive sign on $\boldsymbol{Y}_{\boldsymbol{H}}$ for left side of body.

TABLE 6

LOCATION OF ORIGIN OF SEGMENT ANATOMICAL COORDINATE SYSTEMS: LARGE MALE

Segment	X _H (mm)	Y _H (mm)	Z _{.H} (mm)
Head	-212	0	646
Neck	-300	0	531
Thorax	-237	0	77
Abdomen	-126	0	143
Pelvis	- 27	0	86
Upper Arms	-256	±217*	454
Lower Arms	52	±261	252
Upper legs	22	±215	- 22
Lower Legs	433	± 97	163
Feet	843	±134	- 80

*Positive sign on $\boldsymbol{Y}_{\boldsymbol{H}}$ for left side of body.

TABLE 7

ANATOMICAL AXES WITH RESPECT TO HIP POINT AXIS SYSTEM: SMALL FEMALE (Cosine Matrix Expressed in Degrees)

				
Segment		Х _Н	Y _H	z _H
Head	X YA ZA	3.7 90.0 93.7	90.0 0.0 90.0	86.3 90.0 3.7
Neck	X Y Z A	27.5 90.0 62.4	90.0 0.0 90.0	117.6 90.0 27.5
Thorax	X Y Z A	8.7 90.0 98.7	90.0 0.0 90.0	81.3 90.0 8.7
Abdomen	X YA ZA	24.7 90.0 114.7	90.0 0.0 90.0	65.3 90.0 24.7
Pelvis	X Y Z A	53.9 90.0 143.9	90.0 0.0 90.0	36.1 90.0 53.9
Upper Arm (L)	X Y Z A	51.3 90.4 141.3	99.7 12.8 98.2	40.4 77.2 52.5
Upper Arm (R)	X Y Z A	51.3 89.6 141.3	80.3 12.8 81.8	40.4 102.8 52.5
Lower Arm with Hand (L)	X Y Z A	148.2 76.2 118.0	78.0 13.8 83.4	61.1 90.0 151.1
Lower Arm with Hand (R)	X Y Z A	148.2 103.8 118.0	102.0 13.8 96.6	61.1 90.0 151.1
Upper Leg (L)	X Y Z A	105.3 79.8 161.5	92.8 11.7 78.6	15.5 84.4 104.4
Upper Leg (R)	X Y Z A	105.3 100.2 161.5	87.2 11.7 101.4	15.5 95.6 104.4

TABLE 7
ANATOMICAL AXES WITH RESPECT TO HIP POINT AXIS SYSTEM:
SMALL FEMALE (Cosine Matrix Expressed in Degrees, Continued)

Segment		Х _Н	Y _H	z _H
Lower Leg (L)	X Y Z A	50.4 109.9 133.7	65.7 24.7 93.9	49.3 103.9 44.0
Lower Leg (R)	X Y Z A	50.4 70.1 133.7	114.3 24.7 86.1	49.3 76.1 44.0
Foot (L)	X YA ZA	59.5 94.4 149.1	80.3 9.6 89.3	32.3 98.7 59.1
Foot (R)	X YA ZA	59.5 85.6 149.1	99.7 9.6 90.7	32.3 81.3 59.1

TABLE 8

ANATOMICAL AXES WITH RESPECT TO HIP POINT AXIS SYSTEM: LARGE MALE (Cosine Matrix Expressed in Degrees)

Segment		X _H	Y _H	z _H
Head	X Y A Z A	2.7 90.0 92.7	90.0 0.0 90.0	87.3 90.0 2.7
Neck	X Y A Z A	24.2 90.0 65.8	90.0 0.0 90.0	114.2 90.0 24.2
Thorax	X Y Z Z	7.9 90.0 97.9	90.0 0.0 90.0	82.1 90.0 7.9
Abdomen	X Y Z A	30.7 90.0 120.7	90.0 0.0 90.0	59.3 90.0 30.7
Pelvis	X Y Z A	64.9 90.0 154.9	90.0 0.0 90.0	25.1 90.0 64.9
Upper Arm (L)	X Y Z A	57.3 84.5 146.7	112.4 23.9 98.1	41.4 66.8 58.0
Upper Arm (R)	X Y Z A	57.3 95.5 146.7	67.6 23.9 81.9	41.4 113.2 58.0
Lower Arm with Hand (L)	X Y Z A	117.3 66.8 142.8	69.3 25.4 76.0	35.4 99.8 123.6
Lower Arm with Hand (R)	X Y Z A	117.3 113.2 142.8	110.7 25.4 104.0	35.4 80.2 123.6
Upper Leg (L)	X Y Z A	114.3 85.7 155.3	82.1 8.0 88.9	25.7 96.7 114.7
Upper Leg (R)	X Y Z A	114.3 94.3 155.3	97.9 8.0 91.1	25.7 83.3 114.7

TABLE 8

ANATOMICAL AXES WITH RESPECT TO HIP POINT AXIS SYSTEM:

LARGE MALE (Cosine Matrix Expressed in Degrees, Continued)

Segment		Х _Н	Y _H	z _H
Lower Leg (L)	X Y Z A	47.7 104.2 134.2	65.4 25.1 85.3	52.3 110.2 44.6
Lower Leg (R)	X Y Z A	47.7 75.8 134.2	114.6 25.1 94.7	52.3 69.8 44.6
Foot (L)	X Y Z A	57.8 92.3 147.7	79.0 11.8 85.8	34.4 101.5 58.1
Foot (R)	X Y A Z A	57.8 87.7 147.7	101.0 11.8 94.2	34.4 78.5 58.1

TABLE 9

ANATOMICAL AXES WITH RESPECT TO HIP POINT AXIS SYSTEM: SMALL FEMALE (Cosine Matrix)

Segment		Х _Н	YH	z _H
Head	X Y A Z A	.998 .000 0649	0.000 1.000 0.000	.0649 .000 .998
Neck	X Y A Z A	.887 .000 .463	0.000 1.000 0.000	463 .000 .887
Thorax	X YA ZA	.989 .000 151	0.000 1.000 0.000	.151 .000 .989
Abdomen	X Y Z A	.909 .000 418	0.000 1.000 0.000	.418 .000 .909
Pelvis	X Y Z A	.589 .000 808	0.000 1.000 0.000	.808 .000 .589
Upper Arm (L)	X Y Z A	.625 006 780	-0.169 0.975 -0.143	.762 .222 .609
Upper Arm (R)	X Y Z A	.625 .0062 780	0.169 0.975 0.143	.762 222 .609
Lower Arm with Hand (L)	X Y Z A	850 .238 470	0.208 0.971 0.115	.484 000 875
Lower Arm with Hand (R)	X Y Z A	850 238 470	-0.208 0.971 -0.115	.484 .000 875
Upper Leg (L)	X Y Z A	264 .178 948	-0.048 0.979 0.197	.963 .098 250
Upper Leg (R)	X Y Z A	264 178 948	0.048 0.979 -0.197	.963 098 250

TABLE 9
ANATOMICAL AXES WITH RESPECT TO HIP POINT AXIS SYSTEM:
SMALL FEMALE (Cosine Matrix, Continued)

Segment		x _H	YH	z _H
Lower Leg (L)	X	.637	0.412	.652
	Y A	341	0.909	241
	Z A	691	-0.069	.719
Lower Leg (R)	X	.637	-0.412	.652
	Y A	.341	0.909	.241
	Z A	691	0.069	.719
Foot (L)	X	.508	0.169	.845
	Y A	076	0.986	152
	Z A	858	0.013	.514
Foot (R)	X	.508	-0.169	.845
	Y A	.076	0.986	.152
	Z A	858	-0.013	.514

TABLE 10

ANATOMICAL AXES WITH RESPECT TO HIP POINT AXIS SYSTEM: LARGE MALE (Cosine Matrix)

Segment		Х _Н	Y _H	z _H
Head	X	.999	0.000	.0476
	Y A	.000	1.000	.000
	Z A	0476	0.000	.999
Neck	X	.912	0.000	410
	Y A	.000	1.000	.000
	Z A	.410	0.000	.912
Thorax	X	.991	0.000	.137
	Y A	.000	1.000	.000
	Z A	137	0.000	.991
Abdomen	X	.860	0.000	.511
	YA	.000	1.000	.000
	ZA	511	0.000	.860
Pelvis	X	.424	0.000	.906
	YA	.000	1.000	.000
	ZA	906	0.000	.424
Upper Arm (L)	X Y Z A	.540 .096 836	-0.380 0.914 -0.141	.750 .394 .530
Upper Arm (R)	X Y Z A	.540 096 836	0.380 0.914 0.141	.750 394 .530
Lower Arm with Hand (L)	X Y Z A	459 .394 797	0.353 0.903 0.243	.815 170 554
Lower Arm with Hand (R)	X Y Z Z	459 394 797	-0.353 0.903 -0.242	.815 .170 554
Upper Leg (L)	X	412	0.137	.901
	Y A	.074	0.990	117
	Z A	908	0.019	418
Upper Leg (R)	X	412	-0.137	.901
	YA	074	0.990	.117
	ZA	908	-0.019	418

TABLE 10
ANATOMICAL AXES WITH RESPECT TO HIP POINT AXIS SYSTEM:
LARGE MALE (Cosine Matrix, Continued)

Segment		Х _Н	YH	z _H
Lower Leg (L)	X Y Z A	.673 246 697	0.416 0.906 0.082	.611 346 .712
Lower Leg (R)	X A Y A Z A	.673 .246 697	-0.416 0.906 -0.082	.611 .346 .712
Foot (L)	X Y Z A	.532 040 846	0.190 0.979 0.073	.825 200 .529
Foot (R)	X A Y A Z A	.532 .040 846	-0.190 0.979 -0.073	.825 .200 .529

TABLE 11

COORDINATES OF SURFACE POINTS ON CLAY FORM: SMALL FEMALE

Line	Selected Point	x _H	YH	z _H
BODY CENTERLINE	Crotch	69 67 63 59 53 45 38 28 16 2 - 15 - 27 - 37 - 52 - 59 - 66 - 73	00000000000000000	25 47 63 76 89 102 113 125 134 140 157 172 188 203 219 236 253 274
	Suprasternale Back of Chin (neck) Under Chin, Front Front of Chin, Low Lower Lip (mid) Top Lip (mid)	- 79 - 86 - 96 - 106 - 116 - 126 - 136 - 145 - 152 - 152 - 150 - 103 - 91 - 87 - 85	0000000000000000	293 312 332 348 360 370 383 392 416 433 445 496 506
	Root of Nose Tip of Nose Nasion	- 89 - 73 - 89 - 90 - 93 - 102 - 112 - 130 - 147 - 175	0 0 0 0 0 0 0	518 531 578 593 610 629 642 654 661 667

TABLE 11
COORDINATES OF SURFACE POINTS ON CLAY FORM:
SMALL FEMALE (Continued)

Line	Selected Point	X _H	YH	z _H
Centerline (Continued)	Top of Head	^H -185 -200 -225 -249 -266 -273 -272 -268	1 H O O O O O O O	667 666 658 643 618 595 575 553
	Edge of Seatback	-255 -240 -235 -235 -236 -243 -247 -253 -259 -272	0 0 0 0 0 0 0 0	527 507 488 467 449 432 412 392 372 363
BACK OF SHOULDER TO BELOW BREAST	Rear of Shoulder Top of Shoulder	-264 -254 -241 -233 -226 -192	75 80 84 85 86 84	373 392 405 417 418 407
	Clavicle	-172 -164 -147 -125 -107 - 87 - 70 - 55	80 77 74 73 76 79 81 82	393 388 378 361 341 318 294 274
	Tip of Breast Base of Breast	- 41 - 39 - 39 - 42 - 46 - 53	83 85 83 81 78 75	257 250 232 217 208 204

TABLE 11
COORDINATES OF SURFACE POINTS ON CLAY FORM:
SMALL FEMALE (Continued)

Line	Selected Point	Х _Н	YH	z _H	
TOP OF SHOULDER TO HAND	Top of Shoulder Crook of Elbow	- 188 - 165 - 145 - 123 - 103 - 88 - 67 - 45 - 24 5 20 32 47 63 82 95	150 153 157 160 164 168 173 176 178 181 178 175 172 170 167	400 394 384 366 345 325 309 272 248 269 284 301 322 347 368	
	Wrist	107 114	157 153	388 403	
	At Hand	172 132	148 140	423 454	
TOP OF HEAD TO LATERAL SHOULDER	Front of Ear Bottom of Ear, Front Jaw Behind Ear, Down Neck Back of Neck	-185 -184 -182 -181 -180 -179 -174 -169 -165 -163 -194 -199 -206 -212 -214 -215 -209	0 19 41 57 68 73 70 66 3 54 48 50 105 131	667 6656 6432 598 579 5519 450 450 413 404	
	Lateral Shoulder	-202 -186	156 179	396 382	

TABLE 11
COORDINATES OF SURFACE POINTS ON CLAY FORM:
SMALL FEMALE (Continued)

Line	Selected Point	ХН	YH	z _H
SIDE OF ARM TO WRIST	Shoulder Lateral Humeral Epicondyle (bend of elbow) Ulnar Styloid	-169 -147 -128 -105 - 83 - 55 - 28 - 55 - 44 - 64 - 83 - 97 - 110 - 129 - 146	193 199 201 203 204 208 212 212 214 212 208 202 193 187 183	358 336 316 295 272 252 232 207 226 245 266 291 321 348 382 403
UNDERSIDE OF ARM	Anterior Scye (close) Low Point on Elbow Ulnar Styloid	-165 -147 -124 -102 - 81 - 64 - 44 56 77 91 103 111 119 130 139	184 162 165 168 168 170 172 176 181 186 183 179 176 173 170 169 166	272 255 239 224 213 202 188 174 177 199 225 253 289 311 327 356 370
FLANK	Posterior Scye (close)	-191 -186 -171 -189 -145 -128 -112 - 98 - 81	159 164 149 141 135 130 130 135 142 150	285 260 225 191 164 132 100 77 55

TABLE 11
COORDINATES OF SURFACE POINTS ON CLAY FORM:
SMALL FEMALE (Continued)

Line	Selected Point	хн	YH	z _H
Flank (<u>Continued</u>)	Near Seat	- 61 - 40 5	162 177 188	32 7 - 15
INSIDE ARM	Scye Humeral Condyle Wrist Thumb Knuckle	-104 - 88 - 59 - 29 3 27 52 73 91 111 123	131 136 139 142 150 145 146 146 144 140 135	357 285 262 237 213 225 255 295 333 374 394 434
OUTSIDE OF LEG	Max. Circ. Pt. Upper Thigh Lateral Femoral Epicondyle Max. Calf Circ. Pt. Min. Ankle Circ. Pt. Lateral Malleolus Metatarsal Phalangeal V	25 62 102 113 142 175 208 275 307 368 275 307 368 457 5548 5786 6454 6454 6457	188 186 181 180 174 165 157 141 138 121 125 138 137 132 119 119 128 139 156 163	-11 - 4 - 5 - 14 - 24 - 30 - 39 - 47 - 52 - 57 - 61 - 87 - 110 - 136 - 186 - 197 - 210 - 229 - 194 - 156 - 131

TABLE 11
COORDINATES OF SURFACE POINTS ON CLAY FORM:
SMALL FEMALE (Continued)

Line	Selected Point	Х _Н	Y _H	ZH
UNDERSIDE OF LEG	Seat-Thigh Juncture Knee Pit	305 328 344 368 381 398 422 445 469 502 537 567 576	73 71 76 75 78 79 80 82 81 82 85 86	 - 11 - 15 - 40 - 64 - 92 -114 -128 -153 -180 -205 -215
TOP OF LEG	Thigh Abdominal Point Top of Knee Patella Toe II Toe III Toe IV Toe V	32 61 96 127 213 245 277 298 367 387 408 450 585 6485 585 6632 685 713 728 717 708	109 106 102 927 84 83 81 790 81 837 89 91 105 105 105 105 105 105 105 105 105 10	61 65 72 80 98 105 112 113 133 53 22 - 8 - 56 - 98 -143 -123 -103 - 77 - 66 - 74 - 86 - 99 - 155

TABLE 11
COORDINATES OF SURFACE POINTS ON CLAY FORM:
SMALL FEMALE (Continued)

Line	Selected Point	X _H	YH	z _H
INSIDE LEG	Crotch	76	12	- 3
		107	14	4
		147	12	13
		182	19	23
		207	27	32
		242	35	49
		285	35	60
		321	31	69
	Medial Femoral Epicondyle	350	33	74
	Tibiale	373	38	56
		388	42	35
		422	45	- 10
	Max. Calf Circ. Pt.	446	48	- 33
		483	52	- 70
		508	61	- 96
	Ankle	535	64	-124
		575	66	-156
	Sphyrion	592	61	-178
	Arch	626	71	-213
		635	72	-165
	Metatarsal Phalangeal I	682	78	-138

TABLE 12

COORDINATES OF SURFACE POINTS ON CLAY FORM: LARGE MALE

Line	Selected Point	Х _Н	Yн	z _H
BODY CENTERLINE	Crotch	77	0	77
		82	0	122
		79	0	144
		74	0	158
		67	0	167
		58	0	172
		56	0	187
		40	0	211
		11	0	244
		- 29	0	281
		- 57	o	303
		- 74	0	341
		- 96	0	376
		-116	0	412
		-142	0	437
		-163	0	459
		-175	0	469
		-176	0	
		l l	0	497
	Throat	-173		515
	Inroat	-162	0	532
	Under Chin	-134	0	539
	Under Chin	-115	0	547
	Front of Chin	-108	0	554
		-108	0	564
	Lin Bassan	-113	0	573
	Lip, Bottom	-108	0	586
	Mid Lip	-110	0	592
	Top Lip	-106	0	597
		-110	0	599
	Back of Nose	-110	0	614
	Tip of Nose	- 93	0	624
		- 99	0	647
	Nasion/Glabella	-111	0	670
		-110	0	681
		-110	0	701
		-119	0	725
	Top of Forehead	-129	0	744
		-142	0	758
		-178	0	774
		-206	0	778
		-238 -278	0	775
		-278	0	757
		-299	0	731
		-301	0	731
		-310	0	701

TABLE 12
COORDINATES OF SURFACE POINT ON CLAY FORM:
LARGE MALE (Continued)

Line	Selected Point	x _H	YH	z _H
Body Centerline (Continued)	Neck Top of Seat	-307 -291 -291 -304 -319 -332 -336 -341	0 0 0 0 0	654 608 565 520 479 429 385 374
SHOULDER TO HAND	Wrist	-335 -325 -297 -265 -225 -187 -143 -113 -58 -60 -18 21 42 79 137 185 236 298 306	125 150 166 178 186 195 205 213 217 217 217 216 223 226 231 218 205 190 173 153 128	386 431 462 489 482 456 405 3798 3127 362 456 456 456 456 456 456 456 456 456 456
TOP OF HEAD TO LATERAL SHOULDER	Top of Head Front of Ear End Line on Jaw Start of Line on Neck Neck and Shoulder Junction	-207 -202 -201 -199 -198 -197 -222 -237 -250 -252 -235 -226 -202	0 43 63 79 78 73 66 63 75 117 160 187 230	778 767 749 667 618 580 576 517 501 493 485 465

TABLE 12
COORDINATES OF SURFACE POINT ON CLAY FORM:
LARGE MALE (Continued)

		,		
Line	Selected Point	x _H	YH	z _H
Top of Head to Lateral Shoulder (<u>Continued</u>)		-189 -188 -185	244 252 252	445 415 382
SIDE OF ARM TO WRIST	Lateral Humeral Condyle Radiale Closest to Ulnar Styloid	-185 -128 -66 -22 25 43 72 122 186 217 245	253 255 258 261 266 267 268 252 225 211 200	382 345 311 291 267 271 285 315 351 371 386
UNDERSIDE OF ARM	Scye Low Pt. Elbow	-241 -186 -147 -107 - 53 - 8 29 89	224 215 216 208 216 216 206 214 196	328 308 291 264 246 229 221 237 270
	Wrist Crease	226 257 272 308 331 348	181 177 168 166 169 169	342 370 393 401 427 448
SIDE FROM POSTERIOR SCYE TO SEAT	Posterior Scye	-240 -196 -174	218 203 192	326 267 237
	"Flat-Tire" Crease Thigh-Abdominal Junction	-154 -128 -110 - 93 - 81 - 53 - 29	183 183 191 198 187 209 223	214 187 166 133 67 39
	(Last Point Measured)	- 10 + 2	219 218	- 19 - 27

TABLE 12
COORDINATES OF SURFACE POINT ON CLAY FORM:
LARGE MALE (Continued)

Line	Selected Point	XH	YH	z _H
OUTSIDE OF LEG		- 72	215	- 9
		+ 9	226	21
		53	226	38
		120	229	63
		217	226	96
		283	221	119
		343	215	139
		398	210	158
	Approx. 0.5 cm in front of	417	206	160
	Lateral Femoral Epicondyle			
		442	200	133
		477	201	89
		513	203	44
	Max. Calf Circ. Point	532	201	18
		589	172	- 50
		663	137	-129
		693	131	-161
	Approx. 0.5 cm behind and	705	134	-175
	below Malleolus	718	129	-189
	Lowest Points on	734	128	-222
	Leg and Foot	744	129	-220 -214
		751	135	-190
		773 800	163	-159
	Matatawaal Dhalangaal V	832	181	-105
	Metatarsal Phalangeal V	852	185	- 76
		052	105	70
UNDERSIDE OF LEG	Base of Heel	695	88	-239
		692	89	-213
		682	95	-199
		643	102	-154
		568	120	-102
		503	133	- 60
		454	140	- 5
	Knee Pit	411	148	+ 81
		360	140	48
	(Closest Pt. to Seat)	307	132	8

TABLE 12
COORDINATES OF SURFACE POINT ON CLAY FORM:
LARGE MALE (Continued)

Line	Selected Point	Х _Н	YH	Z _H
TOEBOARD POINTS		929 928 765 766	227 -227 -226 227	18 19 -238 -239
TOP OF LEG	Patella Top of Knee Nearest to Thigh-Abdom. Jct.	907 857 857 857 780 750 739 705 645 599 573 522 459 404 356 249 174 120 97 54	131 123 117 111 110 108 113 121 128 141 151 161 164 168 160 157 156 149 148 144 138 136	- 15 - 36 - 65 - 95 - 107 - 107 - 95 - 72 - 43 7 52 118 169 202 225 226 219 188 164 143 125 108
TOE TIPS	Toe I Toe II Toe III Toe IV Toe V	897 887 888 882 874	131 149 162 173 184	- 8 - 15 - 25 - 37 - 52

TABLE 12
COORDINATES OF SURFACE POINT ON CLAY FORM:
LARGE MALE (Continued)

		T	T	
Line	Selected Point	ХН	YH	Z _H
INSIDE OF LEG	Crotch Closest to Med. Fem. Epicon.	146 182 226 254 270 348 404	9 16 37 55 64 89 96 99	8 26 47 61 73 131 168
	Closest to Tibiale	484 511 593 624 667 703	91 85 86 83 79 69	83 45 - 34 - 65 -101 -129
	Closest to Sphyrion Near Arch Closest to Metatarsal Phal. I	722 753 798 854	64 69 77 90	-137 -141 -128 - 68
INSIDE ARM	Anterior Scye Closest to Med. Hum. Epicon.	-115 - 83 - 63 - 27 9	167 159 157 167 183 191	421 362 327 301 258 238
	Closest to Stylion Closest to Wrist Crease	70 100 149 201 242 251	181 174 166 154 141 138	262 287 323 369 412 419
		262 283	128	431 446

TABLE 13
ESTIMATED SEGMENT MASS AND VOLUME:
SMALL FEMALE

Segment	Predicted Volume (cm ³)	Predicted Mass (gm)
Head Neck Thorax Abdomen Pelvis Right Upper Arm Left Upper Arm Right Lower Arm with Hand Left Lower Arm with Hand Right Upper Leg Left Upper Leg Right Lower Leg Left Lower Leg Left Lower Leg Right Foot Left Foot	3,697 601 12,983 1,610 6,976 1,124 1,124 1,138 1,138 5,914 5,914 2,360 2,360 638 638	3,697 601 12,983 (11,944) * 1,610 6,976 1,124 1,124 1,138 1,138 5,914 5,914 2,360 2,360 638 638
TOTAL	48,215	48,215 (47,176)*

^{*}The number in parenthesis is based on a density=0.92. This yields a total body weight less than I percent different from the actual value obtained by the subject population.

TABLE 14
ESTIMATED SEGMENT MASS AND VOLUME:
LARGE MALE

Segment	Predicted Volume (cm ³)	Scaled Yolume (cm ³)	Estimated Mass (gm)
Head	4,753	4,511	4,511
Neck	1,231	1,168	1,168
Thorax	34,160	32,418	32,418
Abdomen	3,108	2,949	2,949
Pelvis	16,900	16,038	16,038
Right Upper Arm	2,431	2,307	2,307
Left Upper Arm	2,431	2,307	2,307
Right Lower Arm with Hand	2,556	2,426	2,426
Left Lower Arm with Hand	2,556	2,426	2,426
Right Upper Leg	11,950	11,341	11,341
Left Upper Leg	11,950	11,341	11,341
Right Lower Leg	5,331	5,059	5,059
Left Lower Leg	5,331	5,059	5,059
Right Foot	1,638	1,554	1,554
Left Foot	1,638	1,554	1,554
TOTAL	107,964	102,458	102,458*

 $^{{\}rm *This}$ mass corresponds to a weight of 225.8 lb.

TABLE 15

LOCATION OF ESTIMATED SEGMENT CENTERS OF GRAVITY
WITH RESPECT TO WHOLE-BODY COORDINATE SYSTEM:
SMALL FEMALE

Segment	X _H (mm)	Y _H (mm)	Z _H (mm)
Head Neck Thorax Abdomen Pelvis Upper Arms Lower Arms with Hands Upper Legs Lower Legs Feet	-184 -172 -147 - 82 - 76 - 91 97 147 444	0 0 0 0 ±163* ±176 ±104 ± 82 ±101	578 460 238 107 25 280 306 - 4 - 56 -178

*Positive sign on $\boldsymbol{Y}_{\boldsymbol{H}}$ refers to left side of the body.

TABLE 16

LOCATION OF ESTIMATED SEGMENT CENTERS OF GRAVITY
WITH RESPECT TO WHOLE-BODY COORDINATE SYSTEM:
LARGE MALE

Segment	X _H (mm)	Y _H (mm)	Z _H (mm)
Head Neck Thorax Abdomen Pelvis Upper Arms Lower Arms with Hands Upper Legs Lower Legs Feet	-205 -217 -198 -118 - 73 - 94 183 203 514 805	0 0 0 0 ±205* ±182 ±140 ±136 ±119	678 557 292 120 13 356 347 80 26

*Positive sign on $\boldsymbol{Y}_{\boldsymbol{H}}$ refers to left side of body.

TABLE 17

LOCATION OF ESTIMATED SEGMENT CENTERS OF GRAVITY
WITH RESPECT TO SEGMENT COORDINATE SYSTEMS:
SMALL FEMALE

Segment	X _A (mm)	Y (mm)	Z _A (mm)
Head	- 2	0	33
Neck	52	0	44
Thorax	59	0	146
Abdomen	5	0	- 22
Pelvis	-76	0	20
Upper Arm (R)	115	30	-147
Upper Arm (L)	115	-30	-147
Lower Arm with Hand (R)	11	-14	-135
Lower Arm with Hand (L)	11	14	-135
Upper Leg (R)	-16	60	-143
Upper Leg (L)	-16	-60	-143
Lower Leg (R)	-13	-48	-131
Lower Leg (L)	-13	48	-131
Foot (R)	-68	3	9
Foot (L)	-68	- 3	9

TABLE 18

LOCATION OF ESTIMATED SEGMENT CENTERS OF GRAVITY
WITH RESPECT TO SEGMENT COORDINATE SYSTEMS:
LARGE MALE

Segment	X _A (mm)	Y _A (mm)	Z _A (mm)
Head	8.6	0.0	31.3
Neck	65.3	0.0	57.4
Thorax	68.3	0.0	207.5
Abdomen	- 4.7	0.0	- 24.2
Pelvis	-85.6	0.0	10.9
Upper Arm (R)	19.1	34.2	-185.6
Upper Arm (L)	19.1	-34.2	-185.6
Lower Arm with Hand (R)	-10.7	36.3	-176.5
Lower Arm with Hand (L)	-10.7	-36.3	-176.5
Upper Leg (R)	7.3	72.8	-208.6
Upper Leg (L)	7.3	-72.8	-208.6
Lower Leg (R)	-12.9	-62.7	-150.6
Lower Leg (L)	-12.9	62.7	-150.6
Foot (R)	-82.1	- 0.6	- 6.2
Foot (L)	-82.1	0.6	- 6.2

TABLE 19

ANTHROPOMETRIC VARIABLES USED IN MOMENT OF INERTIA REGRESSION EQUATIONS: SMALL FEMALE

Segment	Moment	Anthropometric Variables
Head	I X I Y I Z	Stature, weight Head circumference Head circumference, head breadth, stature
Neck	X Y Z	Stature, neck circumference, neck breadth Stature, neck circumference, neck length Neck circumference, stature, neck length
Thorax	I X I Y I Z	Weight, thorax length, bust circumference Weight, thorax length, bust circumference Bust circum., 10th rib breadth, thorax length
Abdomen	X Y Z	Stature, weight Stature, weight Stature, weight
Pelvis	I X I Y Z	Weight, bispinous breadth Stature, weight Weight, stature, suprailiac skinfold
Upper Arms	x Y Z	Weight, acromion-radiale length, biceps circumference (relaxed) Weight, acromion-radiale length, biceps circumference (relaxed) Stature, weight
Lower Arms (with hands)	'x 'y 'z	Elbow circumference, forearm-hand length, wrist circumference, hand breadth Elbow circumference, forearm-hand length, wrist circumference, hand breadth Forearm circumference, elbow circumference, wrist circumference, forearm breadth
Upper Legs	'x 'y 'z	Weight, thigh length, buttock circumference mid-thigh circumference Weight, thigh length, mid-thigh circumference Buttock circum., mid-thigh circum., stature
Lower Legs	X Y Z	Calf depth, calf length, knee circumference Calf depth, calf length, knee circumference Calf circum., knee circum., knee breadth
Feet	I X I Y Z	Stature, weight Foot length, sphyrion height, weight, ankle circum Foot length, weight, sphyrion height, stature

TABLE 20

ANTHROPOMETRIC VARIABLES USED IN MOMENT OF INERTIA REGRESSION EQUATIONS: LARGE MALE

Segment	Moment	Anthropometric Variables
Head	I X I Y I Z	Head circumference, head breadth Head circumference Head circumference, head length
Neck	I X I Y I Z	Neck breadth, weight, neck length Neck circumference, weight, neck breadth Neck circumference, neck breadth, weight
Thorax	I X I Y I Z	Stature, weight Stature, weight Weight, chest circumference (seated)
Abdomen	X Y X	Waist circum., abdomen length, suprailiac skinfold Circum. at R10, abdomen length, suprailiac skinfold Waist circum., abdomen length, suprailiac skinfold
Pelvis	I X I Y I Z	Buttock circumference, suprailiac skinfold Stature, weight Stature, weight
Upper Arms	l X l Y	Weight, biceps circum., acromion-radiale length Weight, triceps skinfold, axilla arm depth, biceps circum., acromion-radiale length Biceps circumference, axilla arm circumference, acromion-radiale length
Forearms Plus Hands	X I Y I Z	Forearm-hand length, wrist circum., hand breadth Forearm-hand length, wrist circum., hand breadth Elbow circumference, mid-forearm circumference, weight, hand breadth
Upper Legs	I X I Y I Z	Weight, stature, mid-thigh circum., thigh length Weight, mid-thigh circum., stature, thigh length Weight, mid-thigh circum., upper thigh circum.
Lower Legs	I X I Y I Z	Stature, calf depth, ankle circum., calf length Stature, calf depth, ankle circum., calf length Calf circum., weight, calf length, calf depth
Feet	IX IY IZ	Stature, weight Foot length, sphyrion height, ankle circum., weight Foot length, ankle circum., sphyrion height, weight

TABLE 21
ESTIMATED SEGMENT INERTIAL PROPERTIES:
SMALL FEMALE

Segment	Ι _χ (gm cm ²)	l _γ (gm cm ²)	I _Z (gm cm ²)
Head Neck Thorax Abdomen Pelvis Upper Arms (each) Lower Arms with Hands (each) Upper Legs (each) Lower Legs (each) Feet (each)	146,150	172,919	131,715
	6,084	9,510	10,295
	1,542,806	1,161,238	1,208,626
	143,484	101,463	205,715
	326,244	282,872	574,158
	49,980	51,135	8,168
	141,515	129,402	8,342
	731,416	700,953	153,857
	261,414	261,922	23,135
	3,441	18,428	16,614

TABLE 22
ESTIMATED SEGMENT INERTIAL PROPERTIES:
LARGE MALE

Segment	Predicted (gm cm ²)			Scaled (gm cm ²)		
	l X	l _Y	l _Z	l X	l _Y	l Z
Head Neck Thorax Abdomen Pelvis Up. Arm (L) Up. Arm (R) Low. Arm & Hand (L) Low. Arm & Hand (R) Up. Leg (L) Up. Leg (R) Low. Leg (L)	229,900 . 22,200 7,480,000 267,000 1,750,000 182,000 421,000 421,000	267,700 24,860 5,570,000 168,000 1,580,000 190,000 407,000 407,000 2,035,000 2,035,000	171,700 32,460 4,990,000 489,000 1,990,000 52,400 52,400 28,500 28,500	225,900 21,800 7,351,000 262,000 1,720,000 179,000 414,000 414,000 1,926,000 1,926,000	263,100 24,400 5,474,000 165,000 1,553,000 187,000 400,000 400,000 2,000,000 2,000,000	168,700 31,900 4,904,000 481,000 1,956,000 51,500 51,500 28,000
Low. Leg (R) Foot (L) Foot (R)	846,000 10,600 10,600	848,500 76,400	95,450 79,000 79,000	831,000 10,400	834,000 75,100	93,800

TABLE 23

PRINCIPAL AXES OF INERTIA WITH RESPECT TO ANATOMICAL AXES: SMALL FEMALE (Cosine Matrix Expressed in Degrees)

Segment		XA	YA	ZA
Head	X _P	42	90	48
	YP	90.0	0.0	90.0
	Z _P	132	90.0	42
Neck	X _P	8.6	90.0	81.4
	Y _P	90.0	0.0	90.0
	Z _P	98.6	90.0	8.6
Thorax	X _P	19.1	90.0	70.9
	Y _P	90.0	0.0	90.0
	Z _P	109.1	90.0	19.1
Abdomen	X _P	0.0	90.0	90.0
	Y _P	90.0	0.0	90.0
	Z _P	90.0	90.0	0.0
Pelvis	X _P	2.7	90.0	92.7
	Y _P	90.0	0.0	90.0
	Z _P	87.3	90.0	2.7
Upper Arm (L)	X _P	27	116.6	84.1
	Y _P	63.4	27.7	97.3
	Z _P	92.5	82.9	8.6
Upper Arm (R)	X _P	27	63.4	84.1
	Y _P	116.6	27.7	82.9
	Z _P	92.5	97.3	8.6
Lower Arm with Hand (L)	X _P	17	74.4	95.4
	Y _P	105.6	17.3	82.8
	Z _P	82.6	97.2	9.7
Lower Arm with Hand (R)	X _P	17	105.6	95.4
	Y _P	74.4	17.3	97.2
	Z _P	82.6	82.8	9.7
Upper Leg (L)	X _P	15.2	77.3	81.7
	Y _P	102.7	12.8	88.8
	Z _P	98.3	91.2	8.4
Upper Leg (R)	X _P	15.2	102.7	81.7
	Y _P	77.3	12.8	91.2
	Z _P	98.3	88.8	8.4

TABLE 23
PRINCIPAL AXES OF INERTIA WITH RESPECT TO ANATOMICAL AXES:
SMALL FEMALE (Cosine Matrix Expressed in Degrees, Continued)

Segment		X _A	YA	ZA
Lower Leg (L)	X _P	0.0	90.0	90.0
	Y _P	90.0	0.0	90.0
	Z _P	90.0	90.0	0.0
Lower Leg (R)	X _P	0.0	90.0	90.0
	Y _P	90.0	0.0	90.0
	Z _P	90.0	90.0	0.0
Foot (L)	X _P	6.3	90.3	96.3
	Y _P	91.5	16.5	106.4
	Z _P	83.7	73.5	17.6
Foot (R)	X _P	6.3	89.7	96.3
	Y _P	88.4	16.5	73.6
	Z _P	83.7	106.5	17.6

TABLE 24

PRINCIPAL AXES OF INERTIA WITH RESPECT TO ANATOMICAL AXES: LARGE MALE (Cosine Matrix Expressed in Degrees)

	<u> </u>	<u> </u>		
Segment		XA	YA	z _A
Head	X _P	36	90	54
	Y _P	90.0	0.0	90.0
	Z _P	126	90.0	36
Neck	X _P	11	90.0	79
	Y _P	90.0	0.0	90.0
	Z _P	101	90.0	11
Thorax	X _P	14.5	90.0	75.5
	Y _P	90.0	0.0	90.0
	Z _P	104.5	90.0	14.5
Abdomen	X _P	2.6	90.0	92.2
	Y _P	90.0	0.0	90.0
	Z _P	87.8	90.0	2.6
Pelvis	X _P	8.4	90.0	81.6
	Y _P	90.0	0.0	90.0
	Z _P	98.4	90.0	8.4
Upper Arm (L)	X _P	33.9	56.1	90.0
	Y _P	123.9	33.9	90.0
	Z _P	90.0	90.0	0.0
Upper Arm (R)	X _P	33.9	123.9	90.0
	Y _P	56.1	33.9	90.0
	Z _P	90.0	90.0	0.0
Lower Arm with Hand (L)	X _P	19.5	70.5	90.0
	Y _P	109.5	19.5	90.0
	Z _P	90.0	90.0	1
Lower Arm with Hand (R)	Х _Р	19.5	109.5	90.0
	ҮР	70.5	19.5	90.0
	Z _Р	90.0	90.0	1
Upper Leg (L)	Х _Р	9.8	80.2	90.0
	ҮР	99.8	9.8	90.0
	Х _Р	90.0	90.0	0.0
Upper Leg (R)	X _P	9.8	99.8	90.0
	Y _P	80.2	9.8	90.0
	Z _P	90.0	90.0	0.0

TABLE 24
PRINCIPAL AXES OF INERTIA WITH RESPECT TO ANATOMICAL AXES:
LARGE MALE (Cosine Matrix Expressed in Degrees, <u>Continued</u>)

Segment		X _A	YA	z _A
Calf (L)	X _P	24	114	90
	Y _P	66	24	92
	Z _P	90	88	1
Calf (R)	X _P	24	66	90
	Y _P	114	24	88
	Z _P	90	92	1
Foot (L)	X _P	10	94	81
	Y _P	86	7	95
	Z _P	99	85	10
Foot (R)	X _P	10	86	81
	Y _P	94	7	85
	Z _P	99	95	10

TABLE 25

PRINCIPAL AXES OF INERTIA WITH RESPECT TO ANATOMICAL AXES: SMALL FEMALE (Cosine Matrix)

Segment		X _A	YA	z _A
Head	X _P	0.743	0.000	0.669
	Y _P	0.000	1.000	0.000
	Z _P	-0.669	0.000	0.743
Neck	X _P	0.989	0.000	0.150
	Y _P	0.000	1.000	0.000
	Z _P	-0.150	0.000	0.989
Thorax	X _P	0.945	0.000	0.327
	Y _P	0.000	1.000	0.000
	Z _P	-0.327	0.000	0.945
Abdomen	X _P	1.000	0.000	0.000
	Y _P	0.000	1.000	0.000
	Z _P	0.000	0.000	1.000
Pelvis	X _P	0.999	0.000	-0.047
	Y _P	0.000	1.000	0.000
	Z _P	0.047	0.000	0.999
Upper Arm (L)	X _P	0.891	-0.448	0.103
	Y _P	0.448	0.885	-0.127
	Z _P	-0.044	0.124	0.989
Upper Arm (R)	X _P	0.891	0.448	0.103
	Y _P	-0.448	0.885	0.124
	Z _P	-0.044	-0.127	0.989
Lower Arm with Hand (L)	X _P	0.956	0.269	-0.094
	Y _P	-0.269	0.955	0.125
	Z _P	0.129	-0.125	0.986
Lower Arm with Hand (R)	X _P	0.956	-0.269	-0.094
	Y _P	0.269	0.955	-0.125
	Z _P	0.129	0.125	0.986
Upper Leg (L)	X _P	0.965	0.220	0.14 ¹
	Y _P	-0.220	0.975	0.021
	Z _P	-0.144	-0.021	0.989
Upper Leg (R)	X _P	0.965	-0.220	0.144
	Y _P	0.220	0.975	-0.021
	Z _P	-0.144	0.021	0.989

TABLE 25
PRINCIPAL AXES OF INERTIA WITH RESPECT TO ANATOMICAL AXES:
SMALL FEMALE (Cosine Matrix, Continued)

Segment		X _A	YA	z _A
Lower Leg (L)	X _P	1.000	0.000	0.000
	Y _P	0.000	1.000	0.000
	Z _P	0.000	0.000	1.000
Lower Leg (R)	X _P	1.000	0.000	0.000
	Y _P	0.000	1.000	0.000
	Z _P	0.000	0.000	1.000
Foot (L)	X _P	0.994	-0.005	-0.110
	Y _P	-0.027	0.959	-0.282
	Z _P	0.110	0.284	0.953
Foot (R)	X _P	0.994	0.005	-0.110
	Y _P	0.027	0.959	0.282
	Z _P	0.110	-0.284	0.953

TABLE 26

PRINCIPAL AXES OF INERTIA WITH RESPECT TO ANATOMICAL AXES: LARGE MALE (Cosine Matrix)

Segment		X _A	YA	z _A
Head	X _P	.809	0.000	0.588
	Y _P	.000	1.000	0.000
	Z _P	588	0.000	0.809
Neck	X _P	.981	0.000	0.192
	Y _P	.000	1.000	0.000
	Z _P	192	0.000	0.981
Thorax	X _P	.968	0.000	0.250
	Y _P	.000	1.000	0.000
	Z _P	250	0.000	0.968
Abdomen	X _P	.999	0.000	-0.038
	Y _P	.000	1.000	0.000
	Z _P	.038	0.000	0.999
Pelvis	X _P	.989	0.000	0.146
	Y _P	.000	1.000	0.000
	Z _P	146	0.000	0.989
Upper Arm (L)	X _P	.830	0.558	0.000
	Y _P	558	0.830	0.000
	Z _P	.000	0.000	1.000
Upper Arm (R)	X _P	.830	-0.558	0.000
	Y _P	558	0.830	0.000
	Z _P	.000	0.000	1.000
Lower Arm with Hand (L)	X _P	.943	0.334	0.000
	Y _P	334	0.943	0.000
	Z _P	.000	0.000	1.000
Lower Arm with Hand (R)	X _P	.943	-0.334	0.000
	Y _P	.334	0.943	0.000
	Z _P	.000	0.000	1.000
Upper Leg (L)	X _P	.985	0.170	0.000
	Y _P	170	0.985	0.000
	Z _P	.000	0.000	1.000
Upper Leg (R)	X _P	.985	-0.170	0.000
	Y _P	.170	0.985	0.000
	Z _P	.000	0.000	1.000

TABLE 26
PRINCIPAL AXES OF INERTIA WITH RESPECT TO ANATOMICAL AXES:
LARGE MALE (Cosine Matrix, Continued)

Segment		X _A	YA	z _A
Calf (L)	X _P	.913	-0.407	0.000
	Y _P	.407	0.913	-0.0349
	Z _P	.000	0.0349	1.000
Calf (R)	X _P	.913	0.407	0.000
	YP	407	0.913	0.0349
	Z _P	.000	-0.0349	1.000
Foot (L)	X P	.985	-0.0698	0.156
	Y P	.0698	0.992	-0.0872
	Z P	156	0.0872	0.985
Foot (R)	X _P	.985	0.0698	0.156
	Y _P	0698	0.992	0.0872
	Z _P	156	-0.0872	0.985

TABLE 27

PRINCIPAL AXES OF INERTIA WITH RESPECT TO HIP POINT AXIS SYSTEM: SMALL FEMALE (Cosine Matrix Expressed in Degrees)

		· · · · · · · · · · · · · · · · · · ·		
Segment		Х _Н	YH	z _H
Head	X _P	45.7	90.0	44.3
	Y _P	90.0	0.0	90.0
	Z _P	135.7	90.0	45.7
Neck	X _P	18.7	90.0	109.0
	Y _P	90.0	0.0	90.0
	Z _P	71.0	90.0	18.7
Thorax	X _P	28	90.0	62
	Y _P	90.0	0.0	90.0
	Z _P	118	90.0	28
Abdomen	X _P	24.7	90.0	65.3
	Y _P	90.0	0.0	90.0
	Z _P	114.7	90.0	24.7
Pelvis	X _P	51.2	90.0	38.7
	Y _P	90.0	0.0	90.0
	Z _P	141.3	90.0	51.2
Upper Arm (L)	X _P	61	127	50
	Y _P	68	36	63
	Z _P	143	91	53
Upper Arm (R)	X _P	61	53	50
	Y _P	112	36	117
	Z _P	143	89	53
Lower Arm with Hand (L)	X _P	134.7	63.3	57
	Y _P	66.6	27.6	103.9
	Z _P	127.1	88.9	143.1
Lower Arm with Hand (R)	X _P	134.7	116.7	57
	Y _P	113.3	27.6	76.1
	Z _P	127.1	91.1	143.1
Upper Leg (L)	X _P	110.6	78.6	23.8
	Y _P	77.8	14.3	97.0
	Z _P	154.6	79.6	112.8
Upper Leg (R)	X _P	110.6	101.4	23.8
	Y _P	102.2	14.3	83.0
	Z _P	154.6	100.4	112.8

TABLE 27
PRINCIPAL AXES OF INERTIA WITH RESPECT TO HIP POINT AXIS SYSTEM:
SMALL FEMALE (Cosine Matrix Expressed in Degrees, Continued)

Segment		X _H	Y _H	z _H
Lower Leg (L)	X _P	50.4	65.7	49.3
	Y _P	109.9	24.7	103.9
	Z _P	133.7	93.9	44
Lower Leg (R)	X _P	50.4	114.3	49.3
	Y _P	70.1	24.7	76.1
	Z _P	133.7	86.1	44
Foot (L)	X _P	53.6	66.4	45.4
	Y _P	96.8	25.4	114.5
	Z _P	142.8	80.6	54.5
Foot (R)	X _P	53.6	113.6	45.4
	Y _P	83.2	25.4	65.5
	Z _P	142.8	99.4	54.5

TABLE 28

PRINCIPAL AXES OF INERTIA WITH RESPECT TO HIP POINT AXIS SYSTEM: LARGE MALE (Cosine Matrix Expressed in Degrees)

Segment		Х _Н	Y _H	z _H
Head	X _P	38.7	90.0	51.3
	Y _P	90.0	0.0	90.0
	Z _P	128.7	90.0	38.7
Neck	X _P	13.2	90.0	103.1
	Y _P	90.0	0.0	90.0
	Z _P	76.9	90.0	13.2
Thorax	X _P	22.3	90.0	67.6
	Y _P	90.0	0.0	90.0
	Z _P	112.4	90.0	22.3
Abdomen	X _P	28.5	90.0	61.5
	Y _P	90.0	0.0	90.0
	Z _P	118.5	90.0	28.5
Pelvis	X _P	73.3	90.0	16.7
	Y _P	90.0	0.0	90.0
	Z _P	163.3	90.0	73.3
Upper Arm (L)	X _P	59.9	78.8	32.6
	Y _P	102.8	13.9	95.2
	Z _P	146.7	98.1	58.0
Upper Arm (R)	X _P	59.9	101.2	32.6
	Y _P	77.2	13.9	84.8
	Z _P	146.7	81.9	58.0
Lower Arm with Hand (L)	X _P	107.5	50.6	44.6
	Y _P	58.3	42.8	115.6
	Z _P	142.8	75.9	123.6
Lower Arm with Hand (R)	X _P	107.5	129.4	44.6
	Y _P	121.7	42.8	64.4
	Z _P	142.8	104.1	123.6
Upper Leg (L)	X _P	113.2	72.3	29.8
	Y _P	81.8	17.9	105.6
	Z _P	155.2	88.9	114.7
Upper Leg (R)	X _P	113.2	107.7	29.8
	Y _P	98.2	17.9	74.4
	Z _P	155.2	91.1	114.7

TABLE 28
PRINCIPAL AXES OF INERTIA WITH RESPECT TO HIP POINT AXIS SYSTEM:
LARGE MALE (Cosine Matrix Expressed in Degrees, Continued)

Segment		х _н	YH	z _H
Lower Leg (L)	X _P Y _P Z _P	44.4 85.8 134.9	89.4 6.5 83.5	45.7 95.3 45.6
Lower Leg (R)	X _P Y _P Z _P	44.4 94.2 134.9	90.6 6.5 96.5	45.7 84.7 45.6
Foot (L)	X _P Y _P Z _P	66.7 85.9 156.9	82.5 12.0 82.7	24.6 100.8 68.0
Foot (R)	X _P Y _P Z _P	66.7 94.1 156.9	97.5 12.0 97.3	24.6 79.2 68.0

TABLE 29

PRINCIPAL AXES OF INERTIA WITH RESPECT TO HIP POINT AXIS SYSTEM: SMALL FEMALE (Cosine Matrix)

Segment		Хн	YH	z _H
Head	X _P	.968	0.000	.716
	Y _P	.000	1.000	.000
	Z _P	716	0.000	.698
Neck	X _P	.947	0.000	325
	Y _P	.000	1.000	.000
	Z _P	.325	0.000	.947
Thorax	X _P	.885	0.000	.466
	Y _P	.000	1.000	.000
	Z _P	466	0.000	.885
Abdomen	X _P	.909	0.000	.418
	Y _P	.000	1.000	.000
	Z _P	418	0.000	.909
Pelvis	X _P	.626	0.000	.780
	Y _P	.000	1.000	.000
	Z _P	780	0.000	.626
Upper Arm (L)	X _P	.48	-0.60	.64
	Y _P	.37	0.81	.46
	Z _P	80	-0.01	.60
Upper Arm (R)	X _P	.48	0.60	.64
	Y _P	37	0.81	46
	Z _P	80	0.01	.60
Lower Arm with Hand (L)	X _P	704	0.449	.545
	Y _P	.397	0.886	240
	Z _P	603	0.019	800
Lower Arm with Hand (R)	X _P	704	-0.449	.545
	Y _P	397	0.886	.240
	Z _P	603	-0.019	800
Upper Leg (L)	X _P	352	0.197	.915
	Y _P	.212	0.969	122
	Z _P	903	0.181	388
Upper Leg (R)	X _P	352	-0.197	.915
	Y _P	212	0.969	.122
	Z _P	903	-0.181	388

TABLE 29
PRINCIPAL AXES OF INERTIA WITH RESPECT TO HIP POINT AXIS SYSTEM:
SMALL FEMALE (Cosine Matrix, Continued)

Segment		x _H	YH	z _H
Lower Leg (L)	X _P	.637	0.412	.652
	Y _P	341	0.909	241
	Z _P	691	-0.069	.719
Lower Leg (R)	X _P	.637	-0.412	.652
	Y _P	.341	0.909	.241
	Z _P	691	0.069	.719
Foot (L)	X _P	.593	0.400	.702
	Y _P	119	0.903	415
	Z _P	797	0.163	.581
Foot (R)	X _P	.593	-0.400	.702
	Y _P	.119	0.903	.415
	Z _P	797	-0.163	.581

TABLE 30

PRINCIPAL AXES OF INERTIA WITH RESPECT TO HIP POINT AXIS SYSTEM: LARGE MALE (Cosine Matrix)

Segment		x _H	Y _H	Z _H
Head	X _P	.780	0.000	.626
	Y _P	.000	1.000	.000
	Z _P	626	0.000	.780
Neck	X _P	.973	0.000	227
	Y _P	.000	1.000	.000
	Z _P	.227	0.000	.973
Thorax	X _P	.925	0.000	.380
	Y _P	.000	1.000	.000
	Z _P	380	0.000	.925
Abdomen	X _P	.879	0.000	.478
	Y _P	.000	1.000	.000
	Z _P	478	0.000	.879
Pelvis	X _P	.287	0.000	.958
	Y _P	.000	1.000	.000
	Z _P	958	0.000	.287
Upper Arm (L)	X _P	.502	0.195	.842
	Y _P	222	0.971	091
	Z _P	836	-0.141	.530
Upper Arm (R)	X _P	.502	-0.195	.842
	Y _P	.222	0.971	.091
	Z _P	836	0.141	.530
Lower Arm with Hand (L)	X _P	301	0.634	.712
	Y _P	.525	0.734	433
	Z _P	797	0.243	554
Lower Arm with Hand (R)	X _P	301	-0.634	.712
	Y _P	525	0.734	.433
	Z _P	797	-0.243	554
Upper Leg (L)	X _P	393	0.303	.868
	Y _P	.143	0.952	268
	Z _P	908	0.019	418
Upper Leg (R)	X _P	393	-0.303	.868
	Y _P	143	0.952	.268
	Z _P	908	-0.019	418

TABLE 30
PRINCIPAL AXES OF INERTIA WITH RESPECT TO HIP POINT AXIS SYSTEM:
LARGE MALE (Cosine Matrix, Continued)

Segment		хн	Y _H	z _H
Lower Leg (L)	X _P	.715	0.011	.699
	Y _P	.074	0.994	092
	Z _P	706	0.114	.700
Lower Leg (R)	X _P	.715	-0.011	.699
	Y _P	074	0.994	.092
	Z _P	706	-0.114	.700
Foot (L)	X _P	.395	0.130	.909
	Y _P	.071	0.978	187
	Z _P	920	0.128	.375
Foot (R)	X _P	.395	-0.130	.909
	Y _P	071	0.978	.187
	Z _P	920	-0.128	.375

TABLE 31

LOCATION OF JOINT CENTERS: SMALL FEMALE

Joint	X _H (mm)	Y _H (mm)	Z _H (mm)
Head/Neck	-189	0	519
C7/T1	-183	0	429
T4/T5	-205	0	381
T8/T9	-196	0	273
T12/L1	-149	0	140
L2/L3	-121	0	102
L5/S1	- 80	0	46
Sternoclavicular	-146	± 17	389
Claviscapular	-211	±140	390
Glenohumeral	-174	±146	354
Elbow	20	±179	188
Wrist	134	±155	385
Hip	0	± 80	0
Knee	363	± 75	71
Ankle	593	± 86	-182

TABLE 32

LOCATION OF JOINT CENTERS: LARGE MALE

Joint	X _H (mm)	Y _H (mm)	Z _H (mm)
Head/Neck	-222	0	619
C7/T1	-216	0	506
T4/T5	-248	0	439
T8/T9	-246	0	320
T12/L1	-203	0	175
L2/L3	-159	0	122
L5/S1	- 93	0	42
Sternoclavicular	-171	± 25	462
Claviscapular	-261	±177	470
Glenohumeral	-217	±186	427
Elbow	36	±225	242
Wrist	264	±162	406
Hip	0	± 86	0
Knee	413	±153	166
Ankle	718	± 99	-152

TABLE 33

LOCATION OF JOINT CENTERS IN SEGMENT COORDINATES:
SMALL FEMALE

Joint	Sogmont.	Coordinates (mm)		
Joint	Segment	XA	YA	ZA
Head/Neck	Head	- 11	0	- 25
Head/Neck	Neck	9	0	88
C7/T1	Neck	56	0	11
C7/T1	Thorax	52	0	340
T4/T5	Thorax	23	0	296
Т8/Т9	Thorax	16	0	188
T12/L1	Thorax	42	0	49
L2/L3	Thorax	64	0	7
L2/L3	Abdomen	- 32	0	- 10
L5/S1	Abdomen	- 18	0	- 78
L5/S1	Pelvis	- 62	0	35
Sternoclavicular (L)	Thorax	82	17	295
Sternoclavicular (R)	Thorax	82	- 17	295
Claviscapular (L)	Thorax	18	140	306
Claviscapular (R)	Thorax	18	-140	306
Glenohumeral (L)	Thorax	50	146	265
Glenohumeral (R)	Thorax	50	-146	265
Glenohumeral (L)	Upper Arm (L)	7	- 29	- 35
Glenohumeral (R)	Upper Arm (R)	7	29	- 35
Elbow (L)	Upper Arm (L)	- 3	- 35	-292
Elbow (R)	Upper Arm (R)	- 3	35	-292
Elbow (L)	Lower Arm (L)	- 1	- 29	5
Elbow (R)	Lower Arm (R)	- 1	29	5
Wrist (L)	Lower Arm (L)	- 8	- 25	-224
Wrist (R)	Lower Arm (R)	- 8	25	-224
Hip (L)	Pelvis	- 52	80	- 56
Hip (R)	Pelvis	- 52	- 80	- 56
Hip (L)	Upper Leg (L)	27	-109	- 9
Hip (R)	Upper Leg (R)	27	109	- 9
Knee (L)	Upper Leg (L)	1 0	- 42	-372
Knee (R)	Upper Leg (R)	0	42	-372
Knee (L)	Lower Leg (L)	15	38	17
Knee (R)	Lower Leg (R)	15	- 38	17
Ankle (L)	Lower Leg (L)	1	31	-325
Ankle (R)	Lower Leg (R)	li	- 31	-325
Ankle (L)	Foot (L)	-104	- 12	58
Ankle (R)	Foot (R)	-104	12	58

TABLE 34

LOCATION OF JOINT CENTERS IN SEGMENT COORDINATES:

LARGE MALE

1.2.4	S	Cool	Coordinates (mm)		
Joint	Segment	XA	YA	ZA	
Head/Neck	Head	- 11	0	- 26	
Head/Neck	Neck	35	0	112	
C7/T1	Neck	87	0	12	
C7/T1	Thorax	80	0	422	
T4/T5	Thorax	39	0	360	
т8/т9	Thorax	24	0	242	
T12/L1	Thorax	47	0	92	
L2/L3	Thorax	83	0	31	
L2/L3	Abdomen	- 39	0	- '	
L5/S1	Abdomen	- 23	0	-104	
L5/S1	Pelvis	- 68	lo	41	
Sternoclavicular (L)	Thorax	118	25	37	
Sternoclavicular (R)	Thorax	118	- 25	372	
Claviscapular (L)	Thorax	78	177	386	
Claviscapular (R)	Thorax	78	-177	386	
Glenohumeral (L)	Thorax	68	186	348	
Glenohumeral (R)	Thorax	68	-186	348	
Glenohumeral (L)	Upper Arm (L)	13	- 35	- 4	
Glenohumeral (R)	Upper Arm (R)	13	35	- 4	
Elbow (L)	Upper Arm (L)	- 4	- 48	-358	
Elbow (R)	Upper Arm (R)	- 4	48	-358	
Elbow (L)	Lower Arm (L)	- 14	- 37	10	
Elbow (R)	Lower Arm (R)	- 14	37	10	
Wrist (L)	Lower Arm (L)	- 7	- 32	-278	
Wrist (R)	Lower Arm (R)	- 7	32	-278	
Hip (L)	Pelvis	- 66	86	- 6	
Hip (R)	Pelvis	- 66	- 86	- 6	
Hip (L)	Upper Leg (L)	11	-132] [
Hip (R)	Upper Leg (R)	1 11	132	1	
Knee (L)	Upper Leg (L)	0	- 54	-435	
Knee (R)	Upper Leg (R)	0	54	-435	
Knee (L)	Lower Leg (L)	12	55	2	
Knee (R)	Lower Leg (R)	12	- 55	2	
Ankle (L)	Lower Leg (K)	0	41	-423	
Ankle (R)	Lower Leg (R)	0	- 41	-423	
Ankle (L)	Foot (L)	-133	- 15	65	
Ankle (R)	Foot (R)	-133	15	65	

7.0 REFERENCES

- Dempster, W.T. (1955) <u>Space requirements of the seated operator</u>. Wright-Patterson AFB, Wright Air Development Center, WADC-TR-55-159.
- McConville, J.T.; Churchill, T.D.; Kaleps, I.; Clauser, C.E.; and Cuzzi, J. (1980) Anthropometric relationships of body and body segment moments of inertia. Wright-Patterson AFB, Aerospace Medical Research Laboratory, AMRL-TR-80-119.
- Reynolds, H.M.; Snow, C.C.; and Young, J.W. (1981) Spatial geometry of the human pelvis. Federal Aviation Administration, Memorandum Report No. AAC-119-81-5.
- Snyder, R.G.; Chaffin, D.B.; and Schutz, R.K. (1972) <u>Link system of the human torso</u>. Wright-Patterson AFB, Aerospace Medical Research Laboratory, AMRL-TR-71-88.
- Young, J.W.; Chandler, R.F.; Snow, C.C.; Robinette, K.M.; Zehner, G.F.; and Lofberg, M.S. (1983) Anthropometric and mass distribution characteristics of adult female body segments (Draft Report). Federal Aviation Administration, Civil Aeromedical Institute.

